

# SPECT、PET 影像定量處理分析

楊邦宏 博士

臺北榮總 核醫部暨迴旋加速中心

# 討論一

- 現在各醫院用在SPECT、PET定量檢查的軟體有哪些？
- 腦部
- 心臟
- 肺臟
- 腎臟
- 唾液腺
- 骨骼
- 其他

# 討論二

- 有無新的軟體工具提供參考，或是未來採購依據？



# Quantitative Nuclear Medicine imaging in TVGH

Bang-Hung Yang, PhD  
Department of Nuclear Medicine and National  
PET/Cyclotron Center,  
Taipei Veterans General Hospital

# 核醫影像品質影響因子

- 藥物
  - 吸收特性、藥物標誌比活度、注射劑量
- 儀器
  - 儀器品管、準直儀、廠牌
- 病患
  - 檢查前準備事項、移動、病兆區域大小
- 收集影像條件
  - 收集的角度、時間，Zoom，繞360、矩陣大小、COR、距離
- 影像重建法
  - AC、SC、FBP、OSEM、Filter



# What do we have now for clinical diagnosis?

- Neurology
  1. eZIS SW: ECDSPECT imaging analysis
  2. TRODAT-1 SW: TRODAT-1 SPECT imaging analysis
  3. Corex ID SW : FDG PET imaging analysis
- Cardiology
  1. EF analysis (first-pass)
  2. Heartsee for  $\text{NH}_3$  PET



# easy Z-score imaging system (eZIS)

- statistical analysis methods for automated diagnosis
- perfusion SPECT images
- regional cerebral blood flow (rCBF)



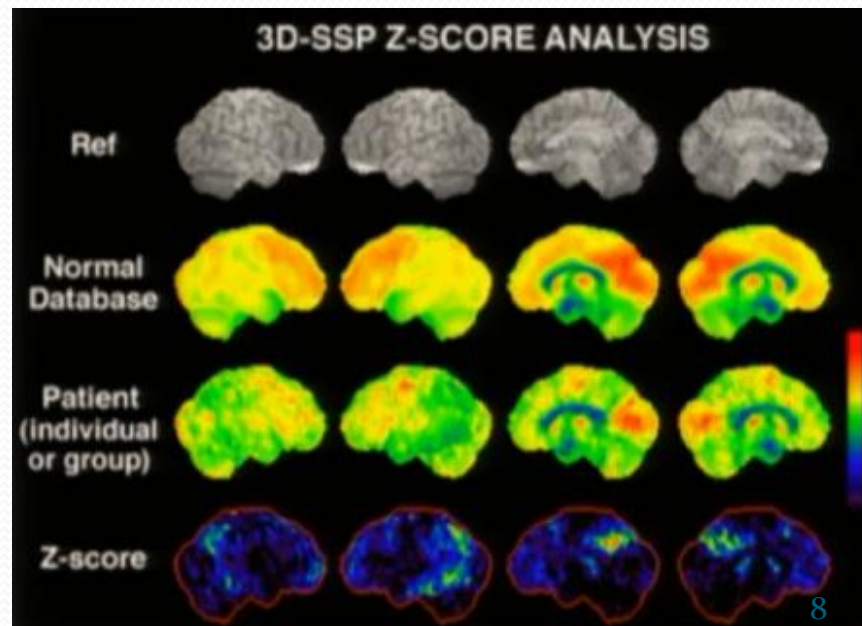
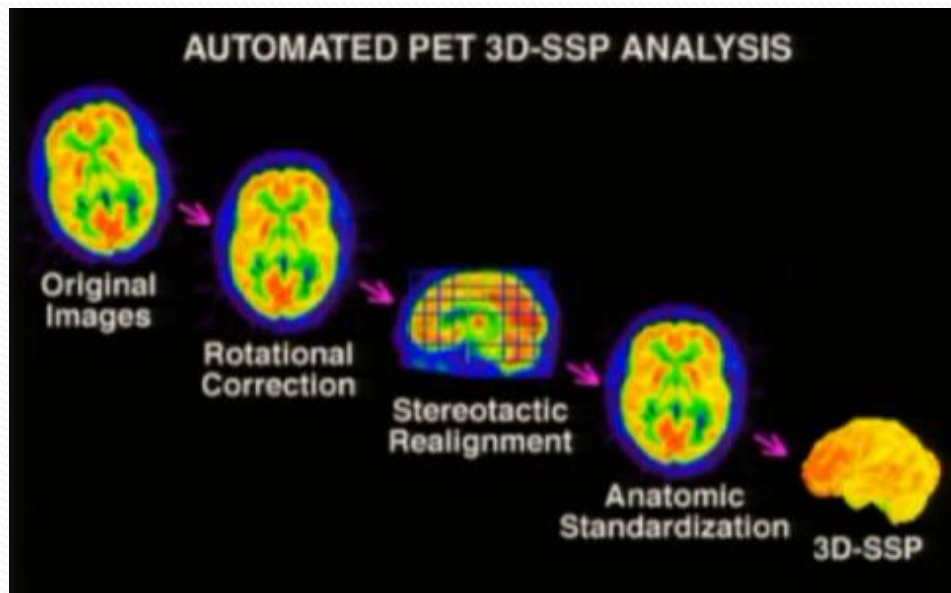
# A Diagnostic Approach in Alzheimer's Disease Using Three-Dimensional Stereotactic Surface Projections of Fluorine-18-FDG PET

Satoshi Minoshima, Kirk A. Frey, Robert A. Koeppe, Norman L. Foster and David E. Kuhl

*Division of Nuclear Medicine, Department of Internal Medicine, and Departments of Neurology and Radiology, University of Michigan, Ann Arbor, Michigan*

To improve the diagnostic performance of PET as an aid in evaluating patients suspected of having Alzheimer's disease, we developed a fully automated method which generates compre-

**F**or more than a decade, PET has been used to investigate functional alteration of the brain in patients with Alzheimer's disease (1-5). Various researchers have demonstrated metabolic and blood flow reductions in the pari-

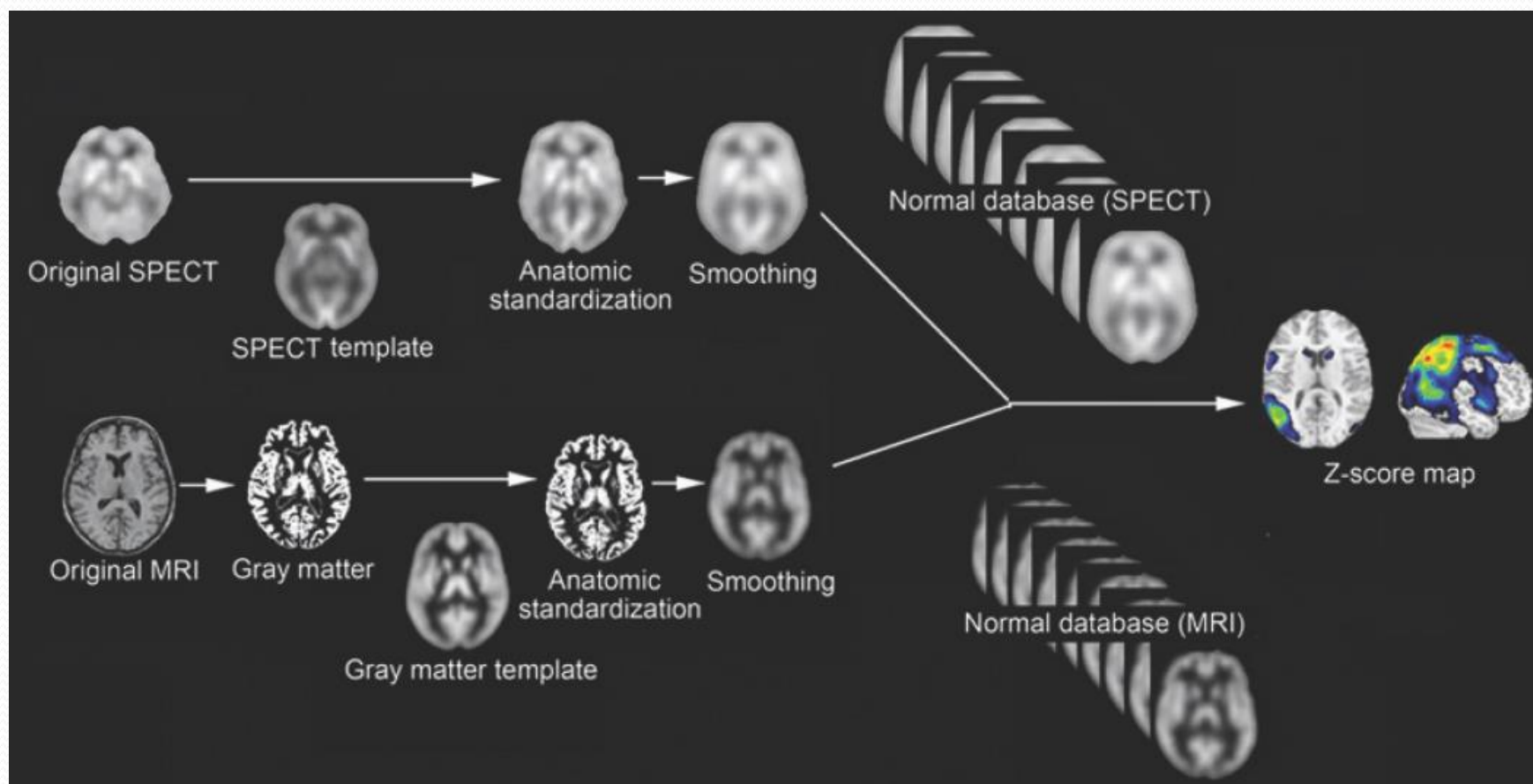






# easy Z-score imaging system (eZIS)

- developed by Prof. Hiroshi Matsuda, National Center of Neurology and Psychiatry, Japan (NCNP; 日本國立精神神經研究中心)





# Z-score

- Voxel normalization : global mean or cerebellar values
- $Z\text{-score} = ( [\text{control mean}] - [\text{individual value}] ) / (\text{control SD})$



# easy Z-score imaging system (eZIS)

<sup>99m</sup> Tc-ECD データベース名	年齢階層	性別	例数	SPECT 収集中心時刻(MST)*1	減弱補正(AC)の 有無(+/-)
ECD1-3yDB *2	1-3 歳 *1	男女混合	21 例		AC+
ECD3-5yDB *2	3-5 歳 *1		18 例		
ECD6-10yDB *2	6-10 歳		17 例		
ECD10-15yDB *2	10-15 歳		9 例		
ECD20-39yDB	20-39 歳		28 例		
ECD40-59yDB	40-59 歳		30 例		
ECD60-69yDB	60-69 歳		40 例		
ECD70y-DB	70 歳以上		40 例		
ECD60-69y の男 DB	60-69 歳		男性のみ		
ECD60-69y の女 DB	60-69 歳	女性のみ	22 例		
ECD70y-の男 DB	70 歳以上	男性のみ	20 例		
ECD70y-の女 DB	70 歳以上	女性のみ	20 例		



tes\ECD2\_SPM2.img

Original of patient: C:\Users\cbdoctor\Desktop\20160630\EARLY\_IRACSC001\_DS\_Result\\*\_EARLY\_IRACSC001\_DS.img

Patient: C:\Users\cbdoctor\Desktop\20160630\EARLY\_IRACSC001\_DS\_Result\\*\_EARLY\_IRACSC001\_DS.img

Result: C:\Users\cbdoctor\Desktop\20160630\EARLY\_IRACSC001\_DS\_Result\chg\_snt\*\_EARLY\_IRACSC001\_DS\_Z-GLOB.img

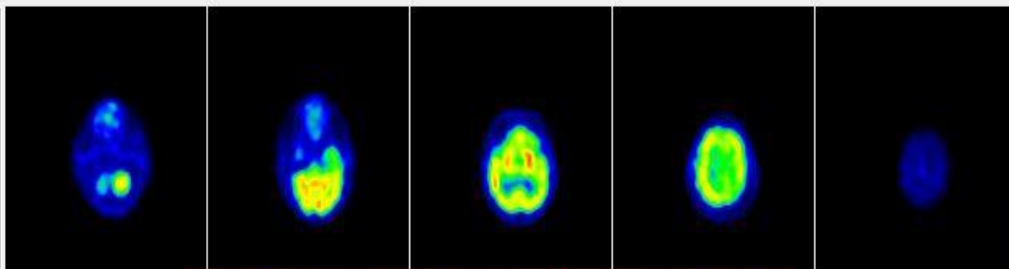
MRI: C:\e215y3\surface mri.img

### Original SPECT

- Start,End
- StepMode

Start  / 53

End  / 53



### CONTROL

Color Map:  Zoom:



MRI  / 0



Fusion:

### POSITION

X

Y

Z

Xbars crosshair spacing



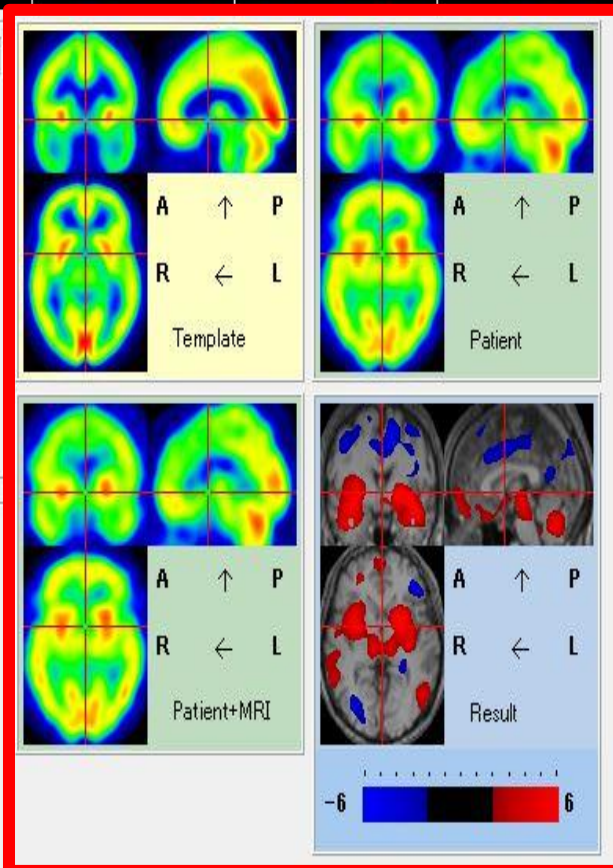
MNI: X=0, Y=0, Z=0

(Result=1.46, Spect=302.00, Template=27.40)

Talairach: X=0.0000, Y=0.0000, Z=0.0000

MNI

Talairach






# For Hyperperfusion



File Edit View Z-SCORE

MRI

Upper  
 lower  
 For QT




Fusion

%

Z-Score level

Upper  
 lower  
 Fix Color



Extent Threshold

n >=  Voxels

Overlay  White Background

Color Map(MRI):

Color Map(Z-Score):

Normal-Patient  Two Tail View  
 Patient-Normal

MEMO ID:

Name:

Date:

Age:

Gender:

**eZIS**  
Version 3.2.0.0

Specific VOI analysis

NDB(ecd80y-(female)db)REF(GLOBAL)TMPL(ECD2\_SPM2)(Setting1)

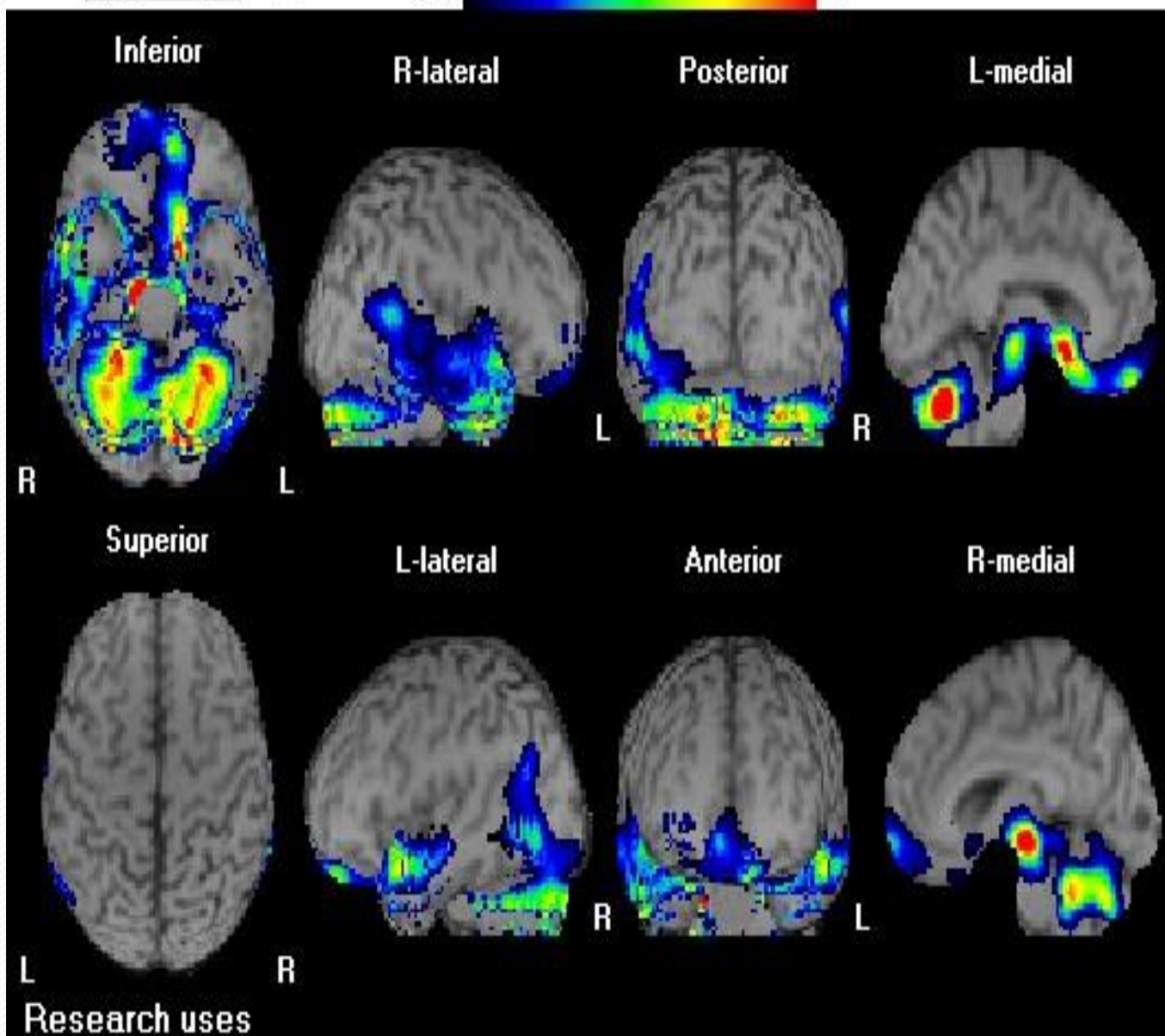
Report & QC

Save Settings

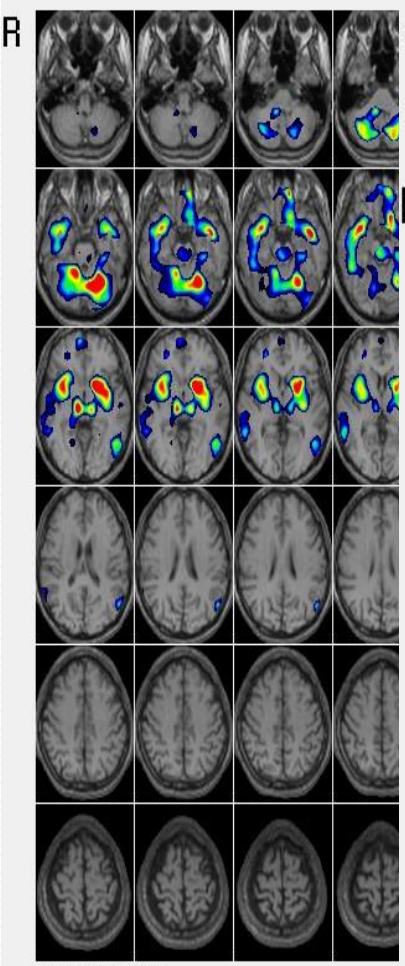


Zoom: x1.5

Label 2.0

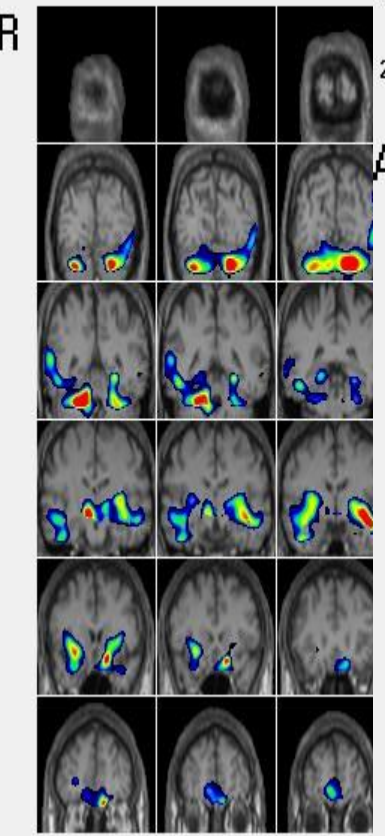


Rows 6 Start Slice 1 End Slice 68  
Columns 8  
 I->S  S->I  
Zoom: x1.0  
Redraw



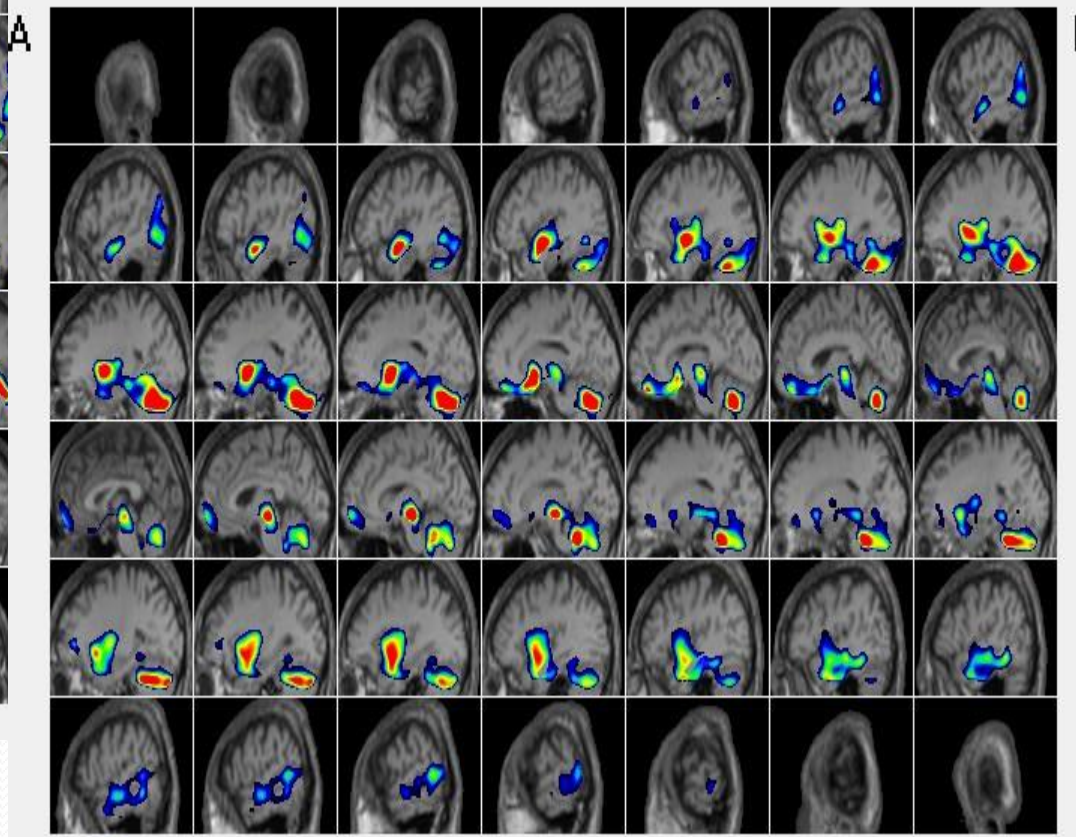
Research uses

Rows 6 Start Slice 1 End Slice 95  
Columns 7  
 P->A  A->P  
Zoom: x1.0  
Redraw



Research uses

Rows 6 Start Slice 1 End Slice 79  
Columns 7  
 L->R  R->L  
Zoom: x1.0  
Redraw



Research uses

P

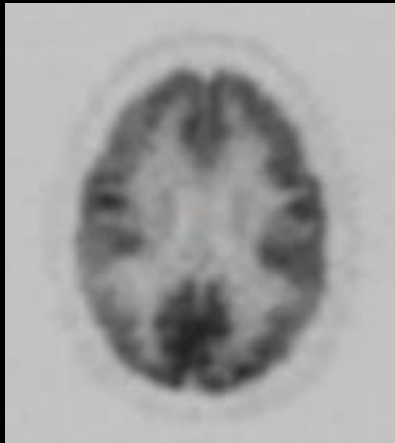




# For Early Alzheimer's Disease

# FDG-PET in 3 Major Dementias

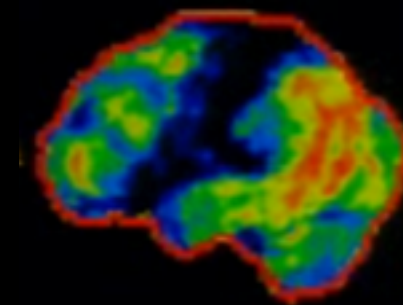
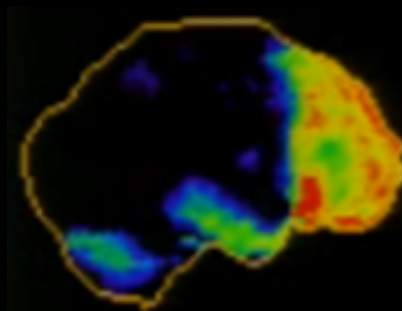
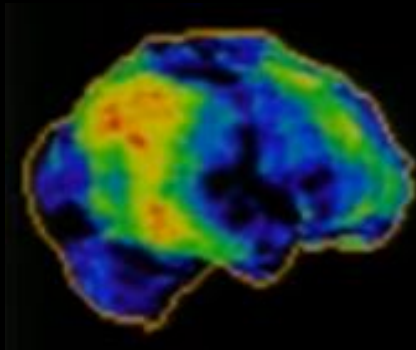
**AD**



**FTD**



**DLB**



File Edit View Z-SCORE specific VOI

MRI Fusion Z-Score level Extent Threshold

100 Upper 6 Upper n>= 300 Voxels

0 lower 2.0 lower 0 2000

For QT  Overlay  White Background

Color Map(MRI): Grayscale

Color Map(Z-Score): Scintipac-7000

Normal-Patient  Two Tail View  Patient-Normal

Specific VOI analysis

for early-stage Alzheimer's disease

MEMO ID: Name:

specific VOI analysis

### Specific VOI analysis result (for early-stage Alzheimer's disease)

1. Severity of Regional Cerebral Blood Flow (rCBF) Decrease in Specific VOI (Posterior Cingulate Gyrus, Precuneus, Parietal Lobule) (the average of positive z scores in specific VOI)	2.14	Description
2. Extent of Regional Cerebral Blood Flow (rCBF) Decrease in Specific VOI (Posterior Cingulate Gyrus, Precuneus, Parietal Lobule) (the ratio of the number of voxels showing $z >= 2$ in the specific VOI. to the number of voxels in the specific VOI)	44.72 %	Description
3. Ratio in the Extent of Regional Cerebral Blood Flow (rCBF) Decrease between Specific VOI (Posterior Cingulate Gyrus, Precuneus, Parietal Lobule) and the Whole Brain (when the rCBF decrease in the whole brain was determined to be 1)	2.82 times	Description

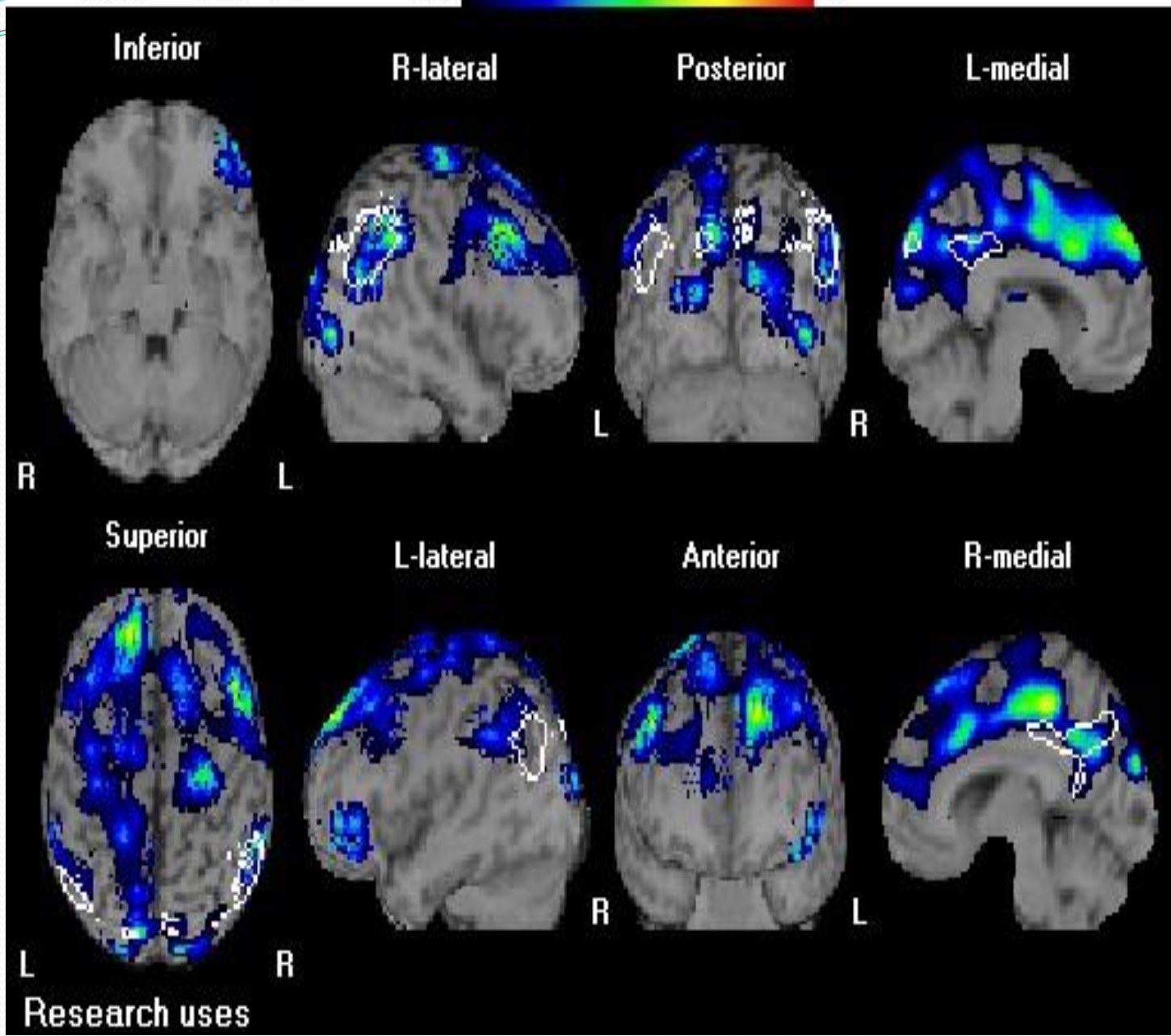
**However, the results of the analysis may differ under various conditions, such as a particular operating condition or subject bias.**

Research uses

Report output Save as csv Close


Zoom: x1.5

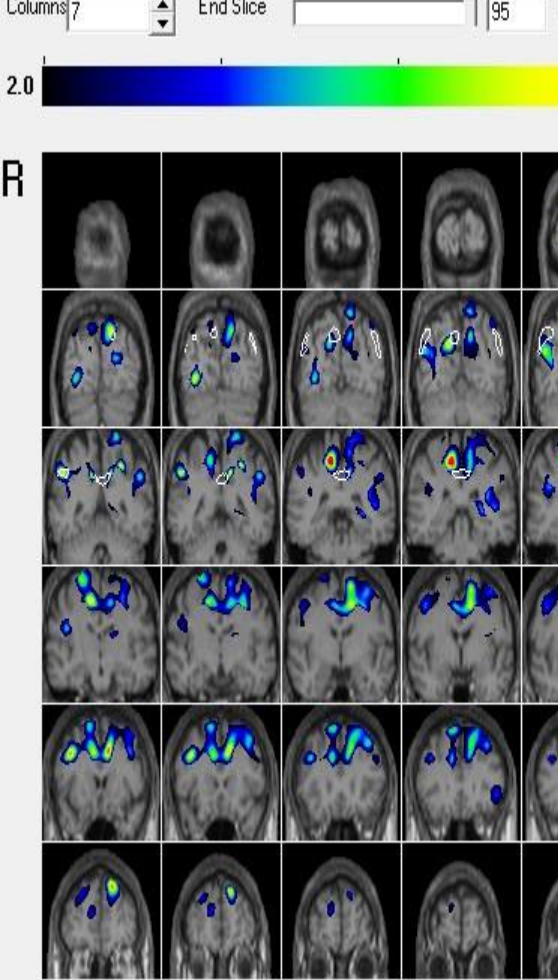
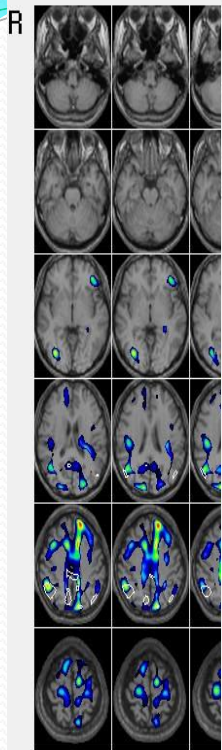
Label 2.0



Research uses

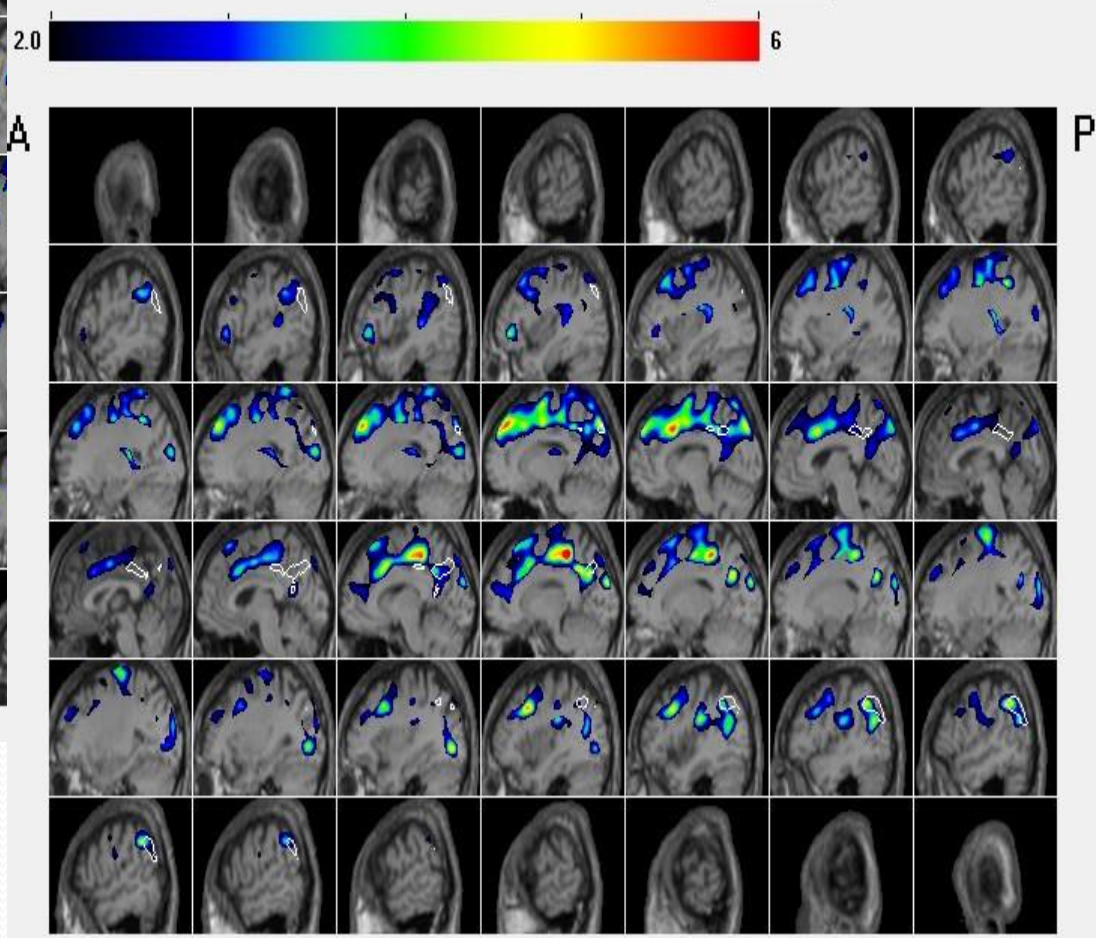
Rows: 6 Start Slice: 1 End Slice: 68 Zoom: x1.0  
Columns: 8  1->S  S->1 Redraw

2.0  Rows: 6 Start Slice: 1 End Slice: 95 Zoom: x1.0  
Columns: 7  P->A  A->P Redraw



Research uses

Rows: 6 Start Slice: 1 End Slice: 79 Zoom: x1.0  
Columns: 7  L->R  R->L Redraw



Research uses

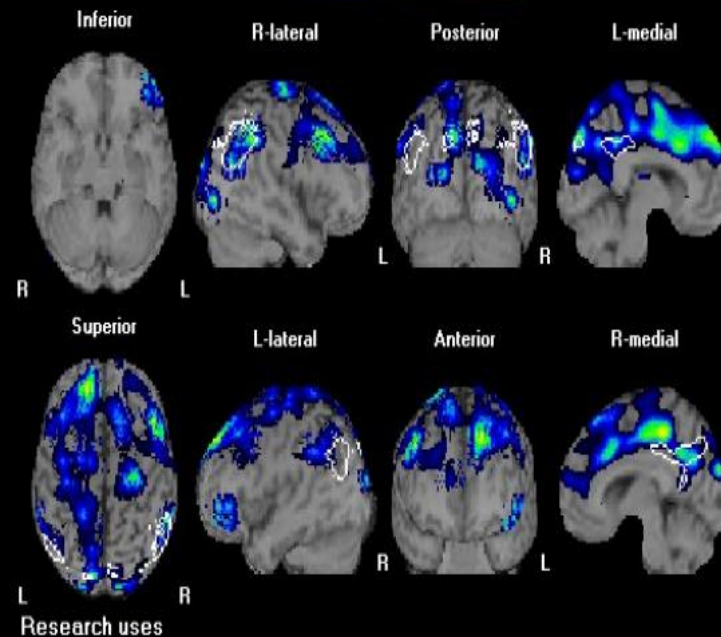
P



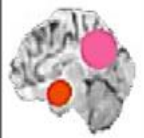

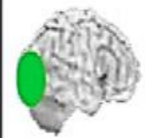
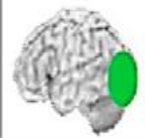




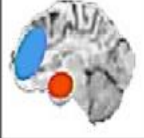
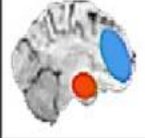
# Easy Z-score Imaging System (eZIS)

ID:

Name:

Zoom:   Label 2.0 



Alzheimer's Disease					<ul style="list-style-type: none"> <li><span style="color: yellow;">●</span> Parietal</li> <li><span style="color: orange;">●</span> Temporal</li> <li><span style="color: pink;">●</span> Posterior Cingulate</li> </ul>
Dementia with Lewy Bodies					<ul style="list-style-type: none"> <li><span style="color: green;">●</span> Occipital</li> </ul>
Frontotemporal Dementia					<ul style="list-style-type: none"> <li><span style="color: blue;">●</span> Frontal</li> <li><span style="color: orange;">●</span> Temporal</li> </ul>

# Regional Cerebral Blood Flow (rCBF) Decrease in Specific **VOI** (Posterior Cingulate Gyrus, Precuneus, Parietal Lobule)

**ID:**            **Name:**

## 1. Severity: 2.14

(the average of positive z scores in specific VOI)

## 2. Extent: 44.72%

(the percent rate of the coordinates with a Z value exceeding the threshold value of 2)

## 3. Ratio: 2.82

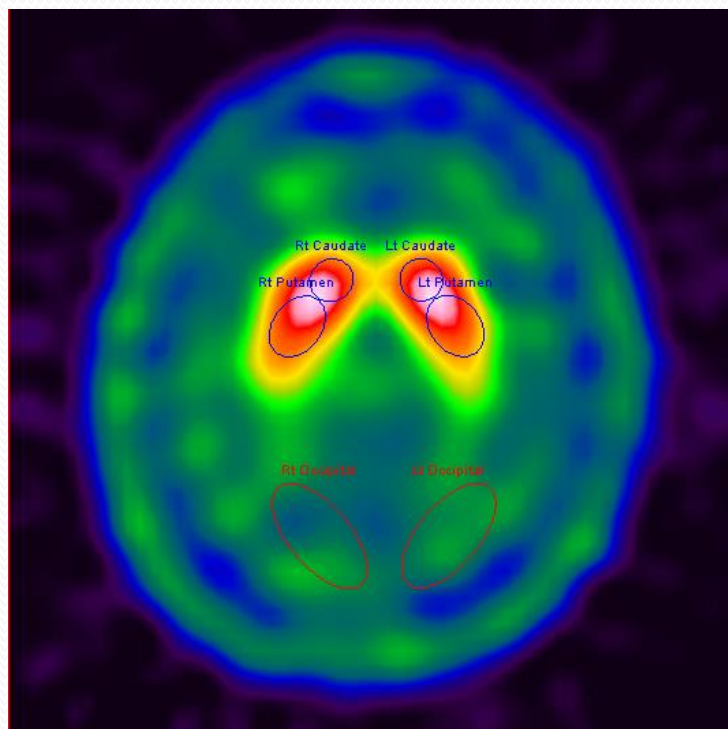
(the extent of a region showing significant rCBF reduction in the VOI to the extent of a region showing significant rCBF reduction in the whole brain)

Cut-off level for diagnosing Alzheimer's Disease

1. Severity: 1.19
2. Extent: 14.2%
3. Ratio: 2.22



# TRUDAT 1-1 SPECT images semi-quantitative analysis



- Specific uptake ratio (SUR)

$$SUR = \frac{target - background}{background}$$

- \*target : striatum, caudate or putamen
- \*background : occipital cortex, frontal cortex or cerebellum
- \* unit : counts/voxel

- Asymmetry

$$Asymmetry = \frac{|SUR_{right\ striatum} - SUR_{left\ striatum}| \times 2}{SUR_{right\ striatum} + SUR_{left\ striatum}} \times 100\%$$





# TRODAT Tool

Bang-Hung Yang & Tung-Hsin Wu

Department of Biomedical Imaging &  
Radiological Sciences  
National Yang-Ming University

Processing (single file di...)

Parameter Setting

Parameter Defaults

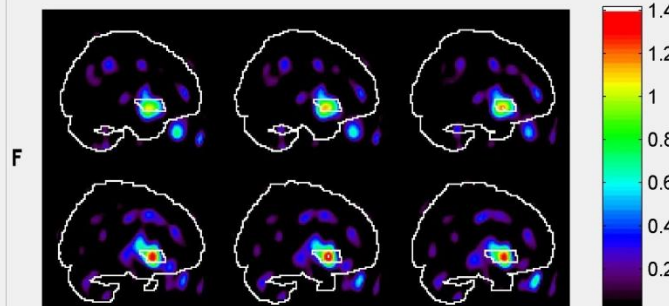
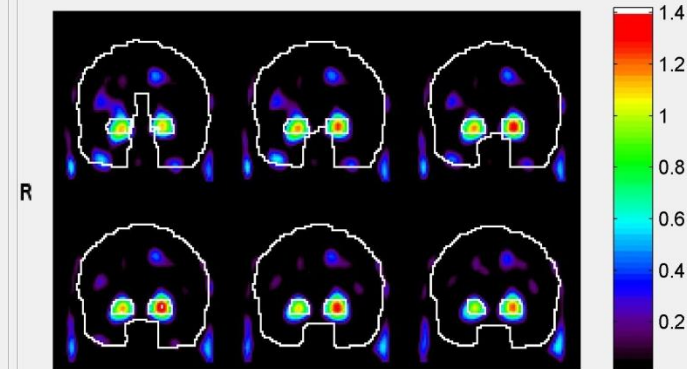
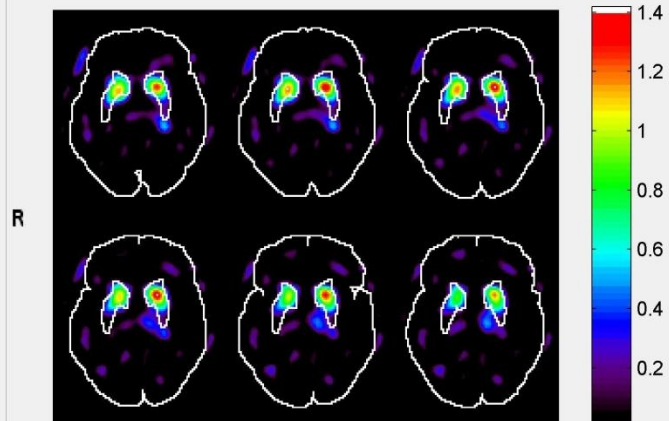
Save

Reset

Quit

colormap: PET

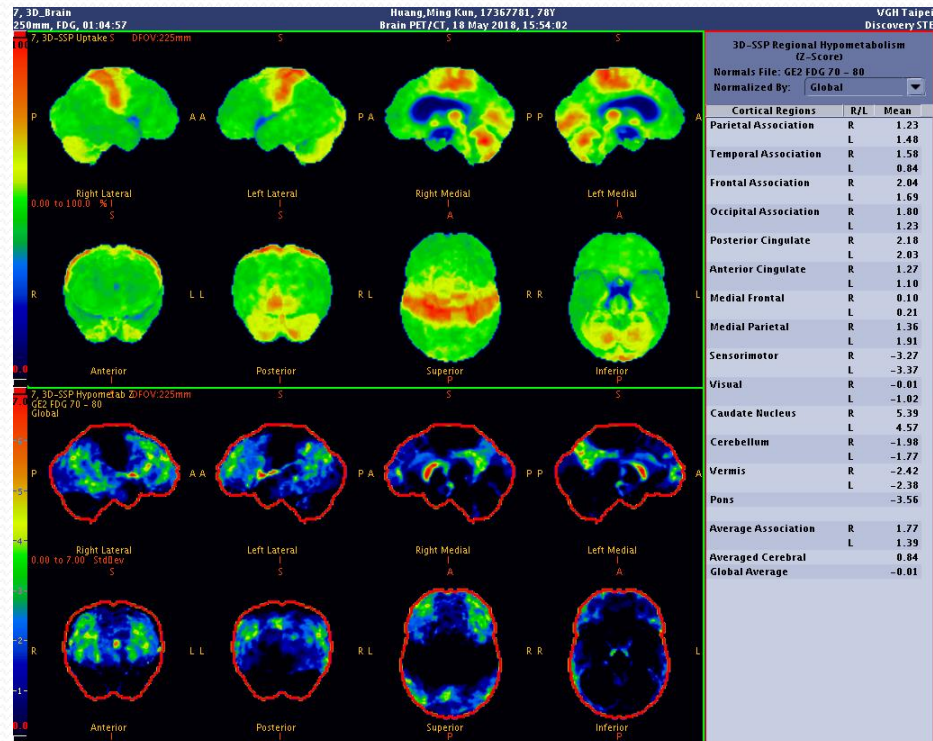
ROI

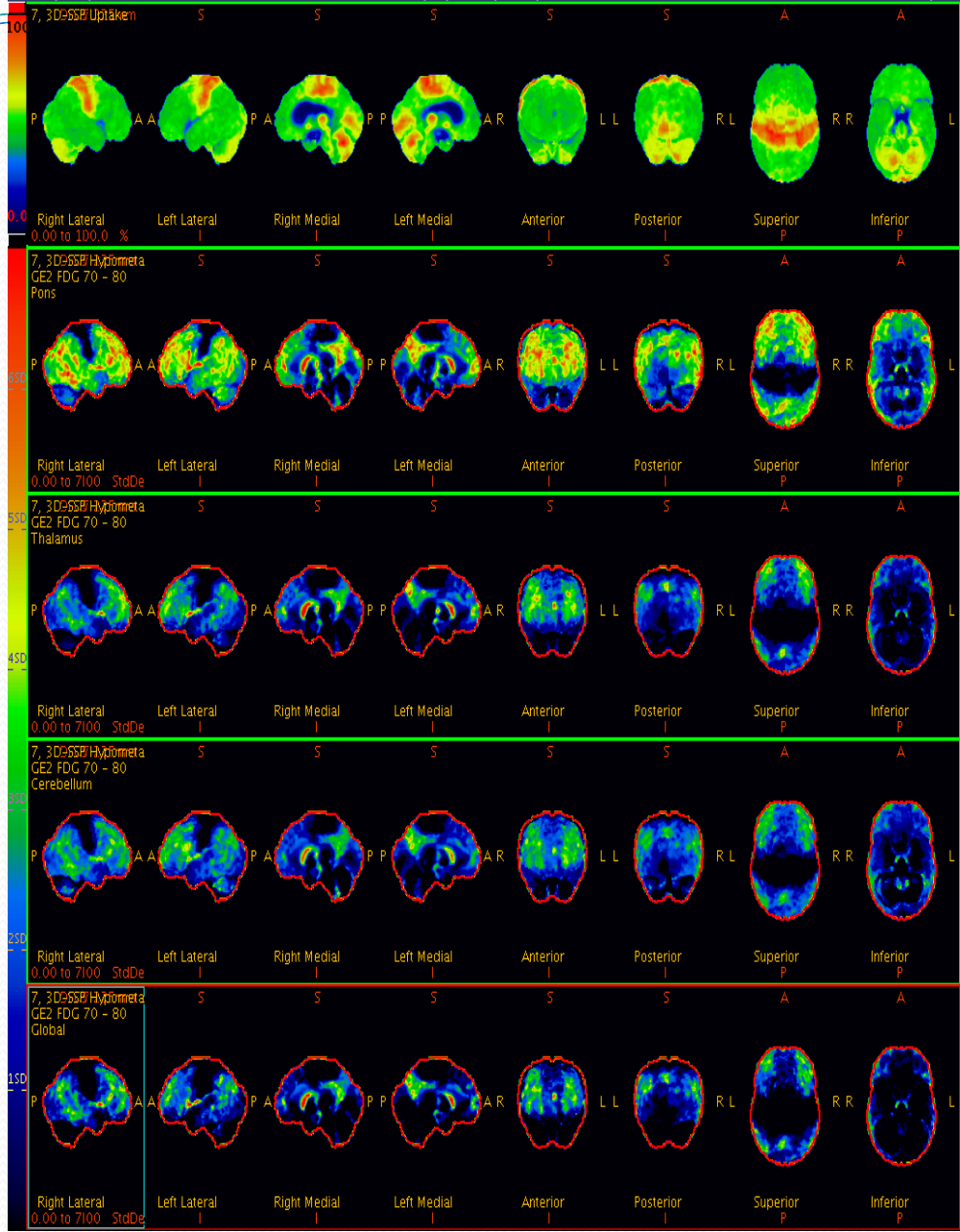


Tc-99m TRODAT

	SUR(R)	SUR(L)	Asymmetry	Global	
caudate	0.7830	0.7480	-0.0457		^
putamen	0.4156	0.6980	0.5071		v
striatum	0.5603	0.6809	0.1943		
	SUR(R)	SUR(L)	Asymmetry	Cerebellum	
caudate	1.2800	1.2353	-0.0355		^
putamen	0.8103	1.1713	0.3644		v
striatum	0.9953	1.1495	0.1438		
	SUR(R)	SUR(L)	Asymmetry	Occipital	
caudate	1.5114	1.4621	-0.0331		^
putamen	0.9940	1.3917	0.3334		v
striatum	1.1978	1.3676	0.1324		

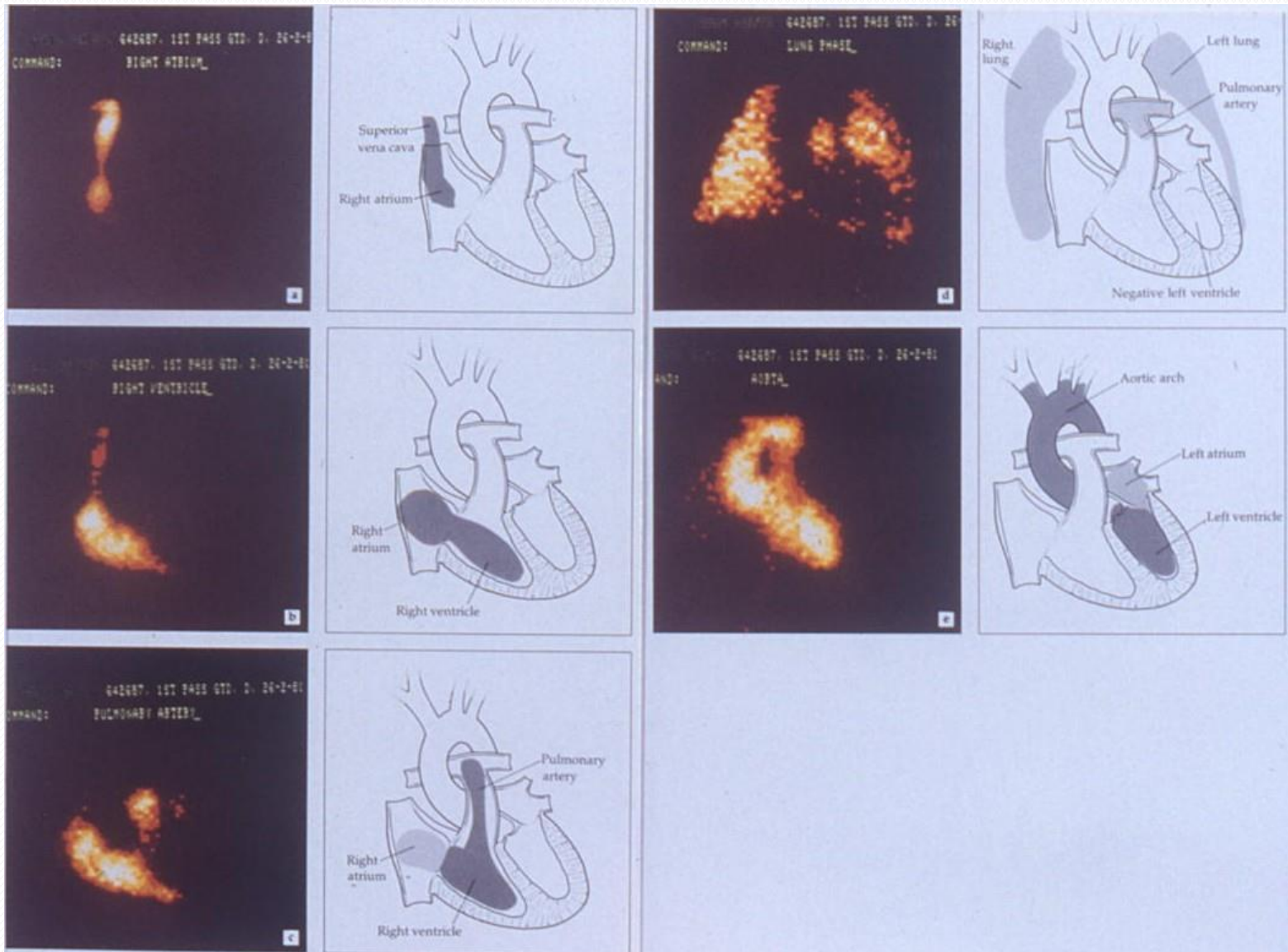
# Cortex ID

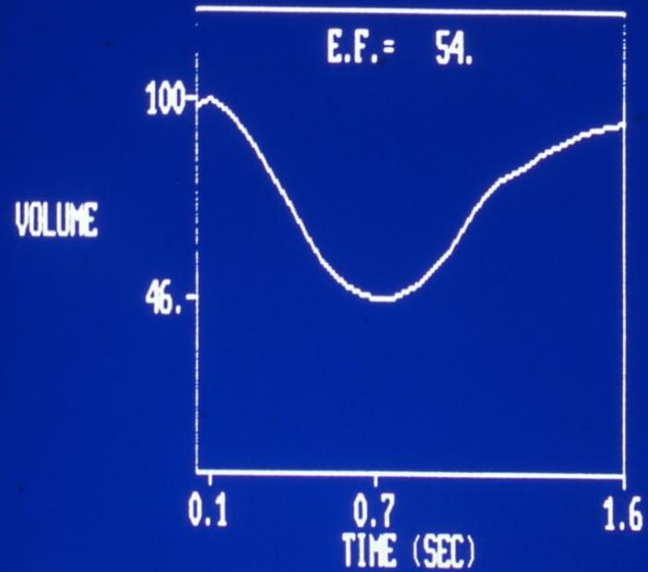




# Cardiology

# First pass analysis



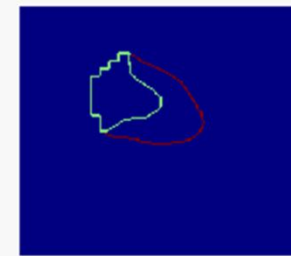


**Figure 4-12** Time-activity curve. Typical left ventricular time-activity curve. Maximum activity is assigned a value of 100, and activity for the remainder of the cycle is scaled relative to this. E.F. = ejection fraction.

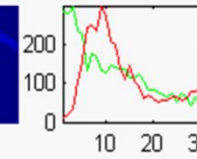
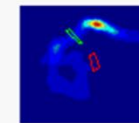
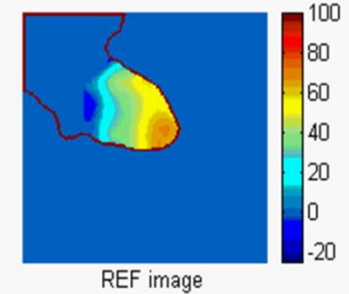
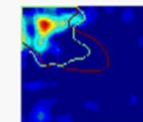
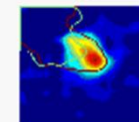
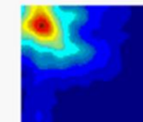
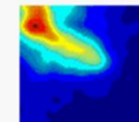
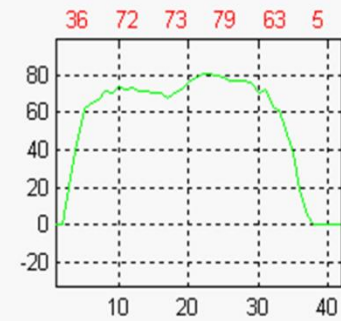
$$\text{Ejection fraction} = \frac{\text{ED} - \text{ES}}{\text{ED}}$$

A normal resting left ventricular ejection fraction is 50 percent or greater. With satisfactory exercise, the ejection fraction should rise at least 5 percentage points\* above its resting value.<sup>40,41</sup>

2005/06/27 S45097893 28209065

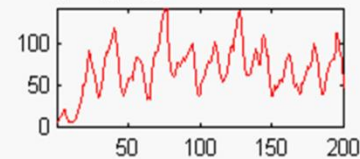
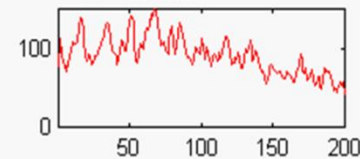
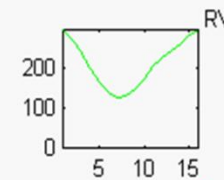
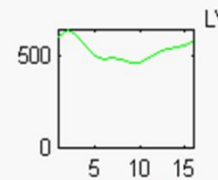
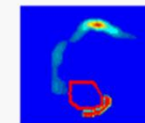
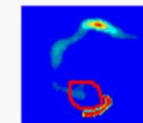
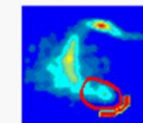
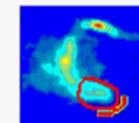


Global EF= 54%



SMTT= 8.43 sec  
 PMTT= 11.64 sec  
 LVEF= 41%  
 RVEF= 62%  
 L/R = 0.66

LVT= 11  
 RVT= 2  
 HR = 75



# Father of Flow Quantitation

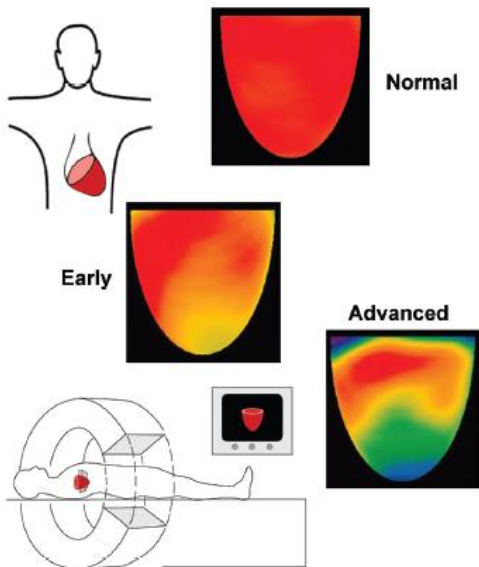


## K. Lance Gould, M.D.

- Professor, Division of Cardiovascular Medicine, Weatherhead PET Center for Preventing and Reversing Atherosclerosis
- The Martin Bucksbaum Distinguished University Chair, The University of Texas Medical School at Houston

42 years, > 100 million USD

# HeartSee



Find early or advanced coronary disease before a heart attack and prevent it. Positron Emission Tomography (PET) of early reduced blood flow in the heart. The only program with proven non-invasive imaging of early coronary disease.

510(K) No. K143664

## GoULD Guidelines for Preventing and Reversing Coronary Artery Disease



THE UNIVERSITY of TEXAS  
MEDICAL SCHOOL AT HOUSTON

*A part of The University of Texas Health Science Center at Houston*

<http://www.uth.tmc.edu/pet/>

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K. LANCE GOULD, M.D.

# Heal *Your* Heart

How You Can Prevent  
or Reverse Heart Disease

Copyrighted Material

amazon

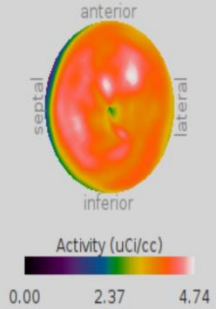


Patient Information



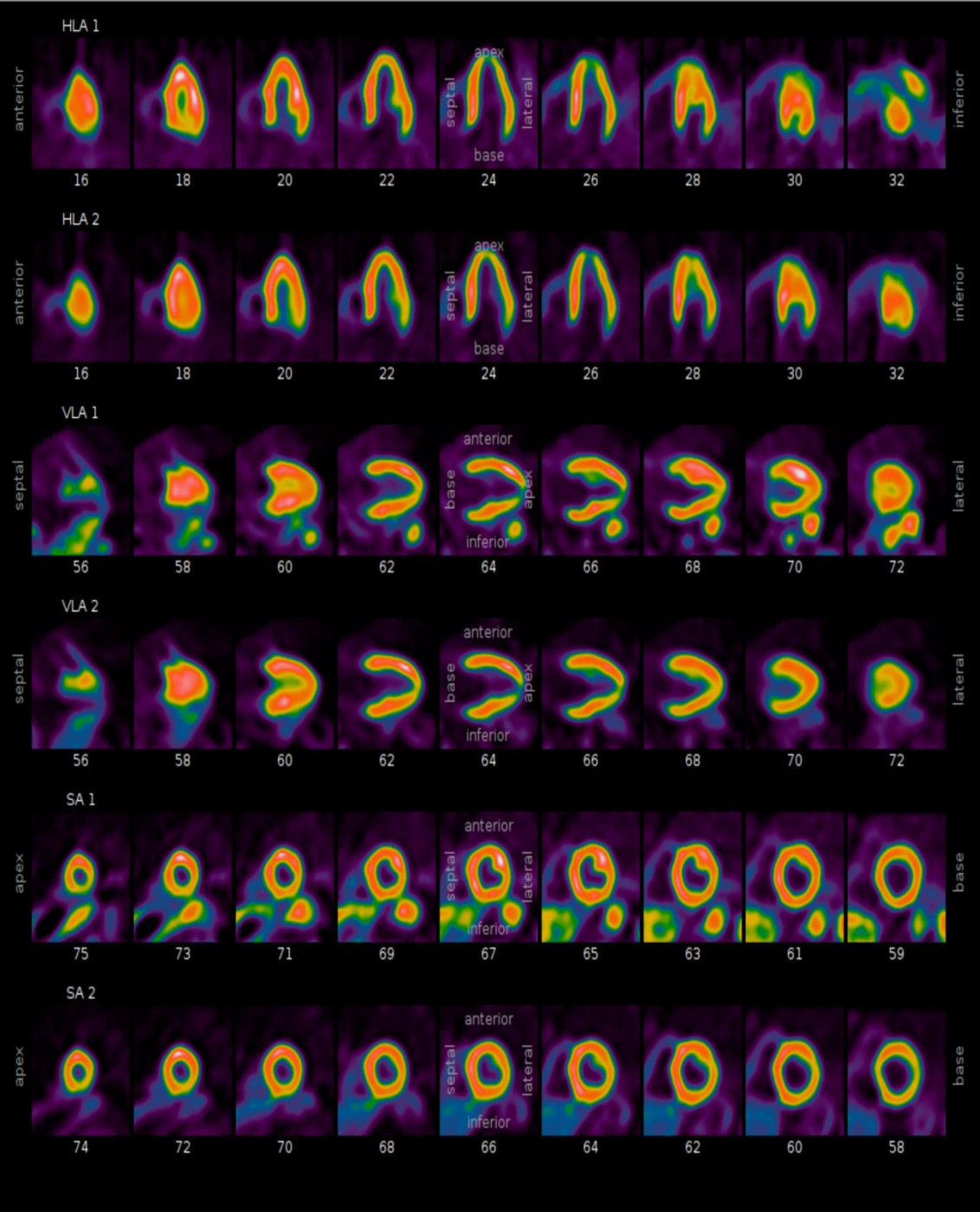
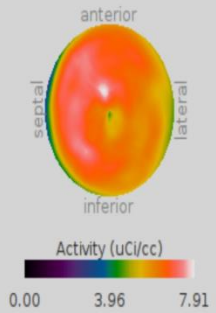
Dataset 1

File Name: **\_Sshift\_Rest\_9min\_L\_1**  
Study ID: **30668**  
Date: **May 03 2018**  
Isotope: **NH**  
State: **Rest**



Dataset 2

File Name: **\_Sshift\_Stress\_9min\_L\_1**  
Study ID: **30668**  
Date: **May 03 2018**  
Isotope: **NH**  
State: **Stress**

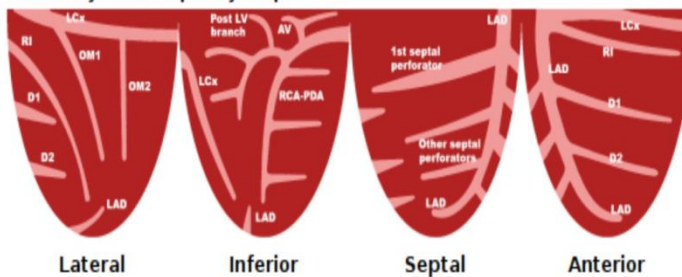


Partial Volume Corrections: Art=1 Myo=0.9

Rest Arterial=5.32 Stress Arterial=3.63

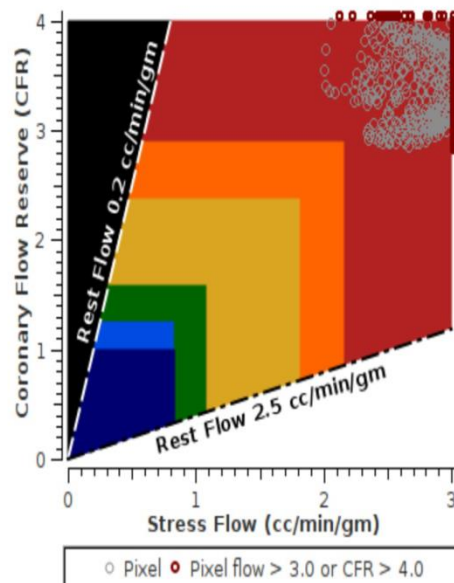
Rest Location=High Ascending Aorta Stress Location=High Ascending Aorta

Coronary Flow Capacity Map



- 100% Normal flow capacity comparable to healthy young volunteers.
- 0% No ischemia. Minimally reduced flow capacity.
- 0% No ischemia. Mildly reduced flow capacity.
- 0% Moderately reduced, sometimes angina or STΔ with dipyridamole stress.
- 0% Severely reduced, usually angina and STΔ with dipyridamole stress.

Plot of Flow Values for Capacity Map



Coronary Flow Capacity Color Scale

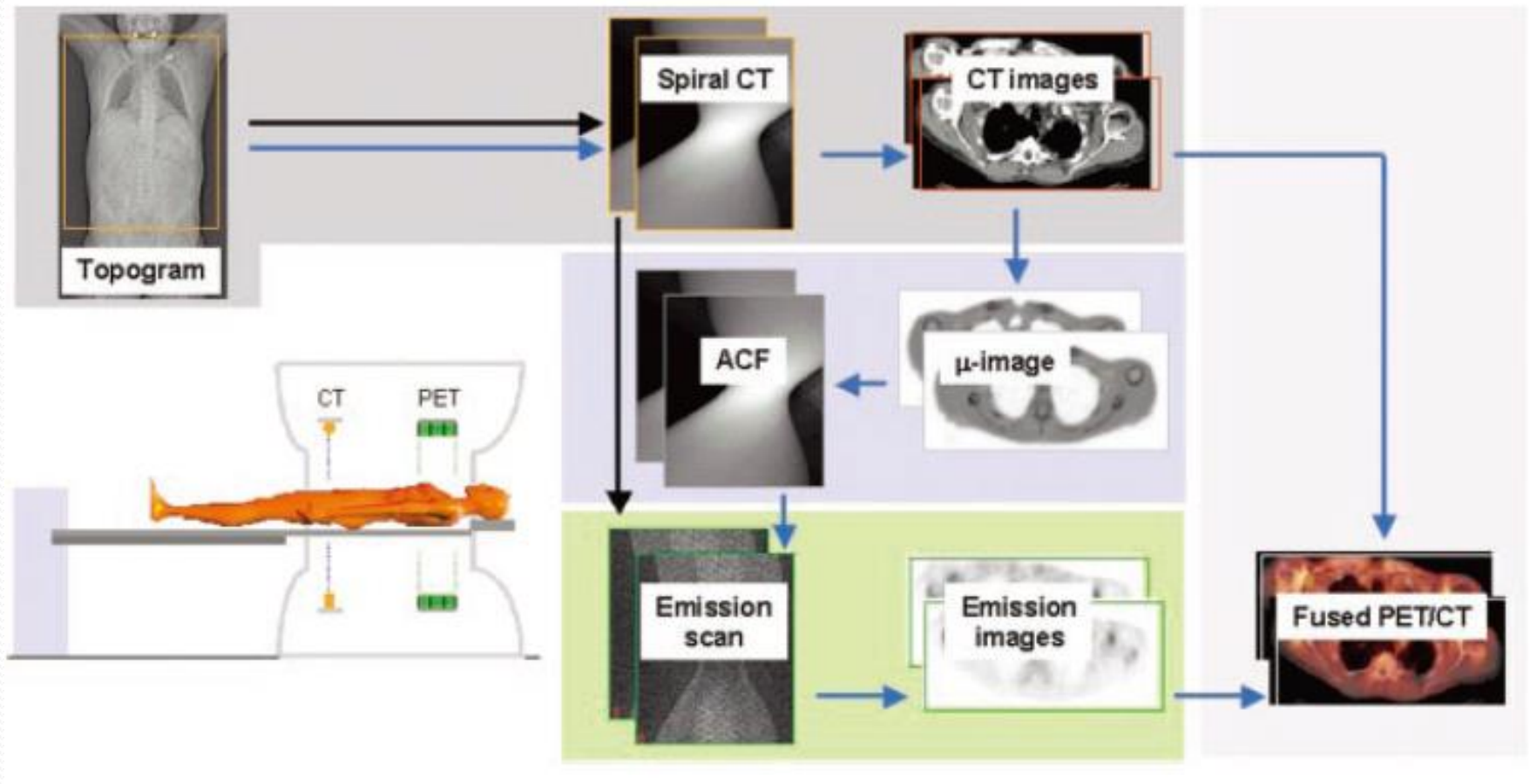
- Healthy young volunteers
- Minimally reduced (risk factors only)
- Mildly reduced (stable CAD)
- Moderately reduced (possible ischemia)
- Severely reduced (definite ischemia)
- Myocardial steal (definite ischemia)

# 核醫全身電腦斷層衰減校正之輻射劑量與假影介紹

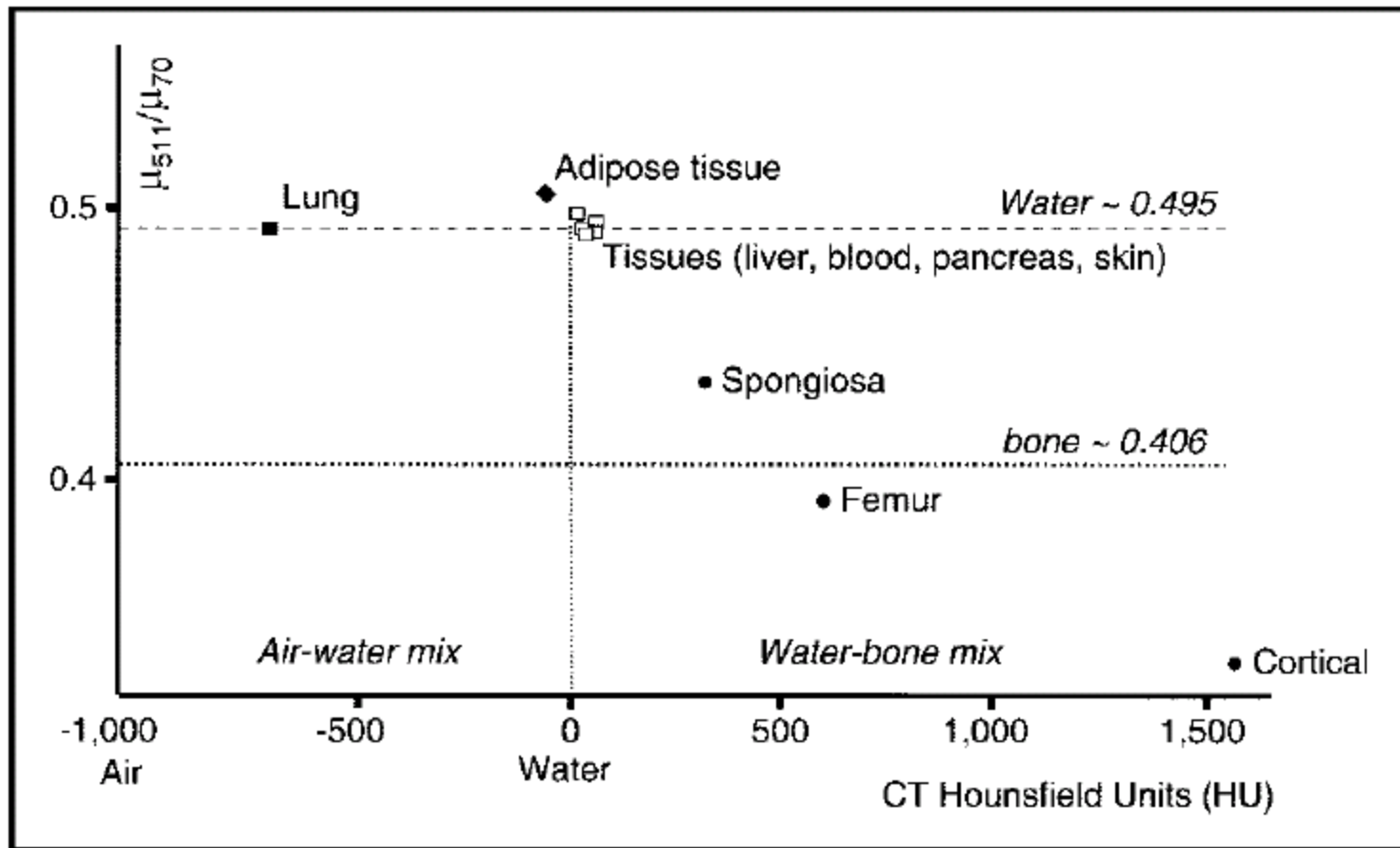
楊邦宏 博士

臺北榮總 核醫部暨迴旋加速中心

# Standard FDG-PET/CT imaging protocol

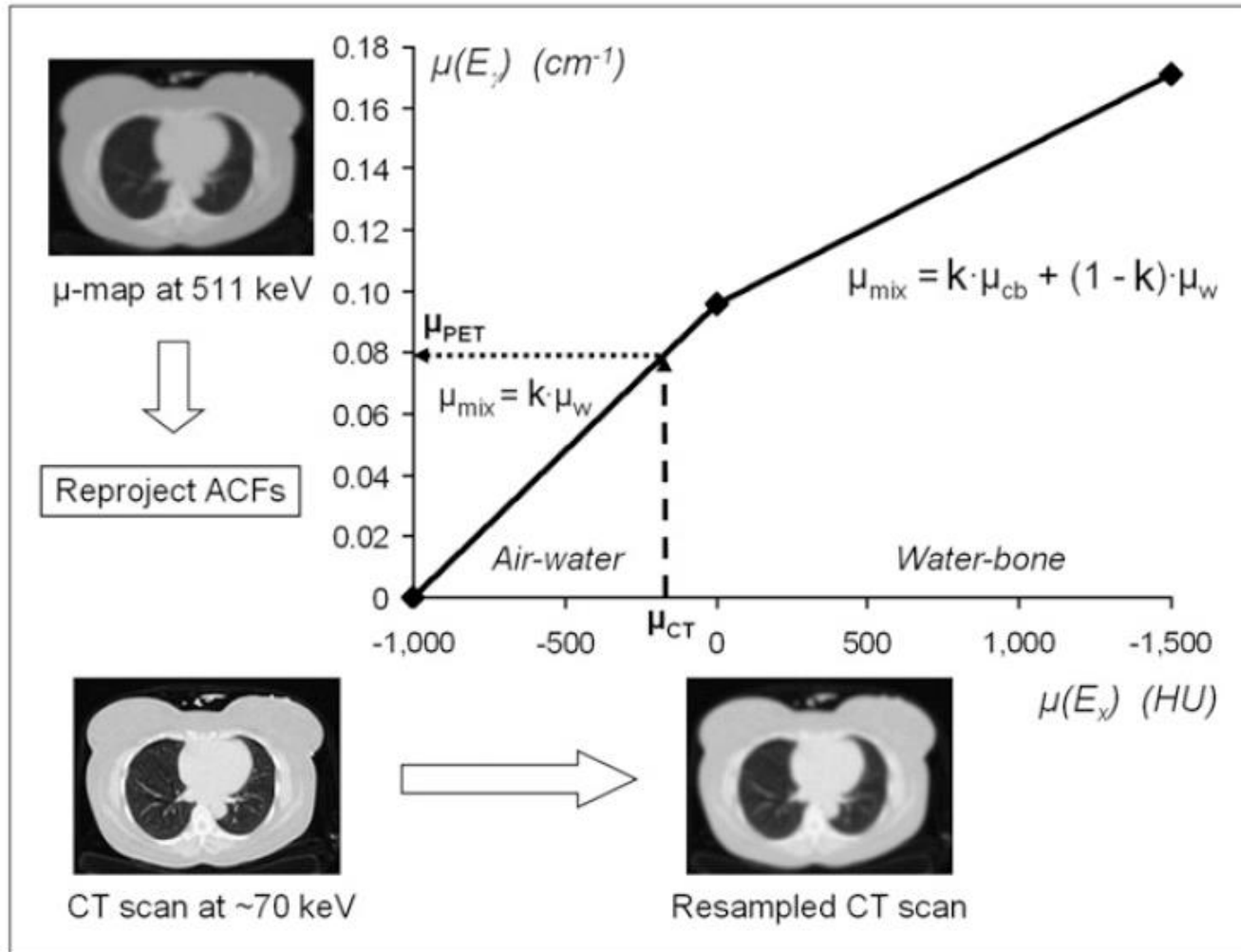


PET + CT → Attenuation Correction



**FIGURE 5.** Plot of ratio of  $\mu(511 \text{ keV})/\mu(70 \text{ keV})$  as function of CT Hounsfield unit (HU) for reference tissues, as given by International Commission on Radiological Protection in 1975 (25). Scaling factors used in algorithm of Kinahan et al. (26) for soft tissue (water) and bone are indicated by horizontal lines.

# CT-BASED ATTENUATION CORRECTION (CT-AC)



# 計畫目的

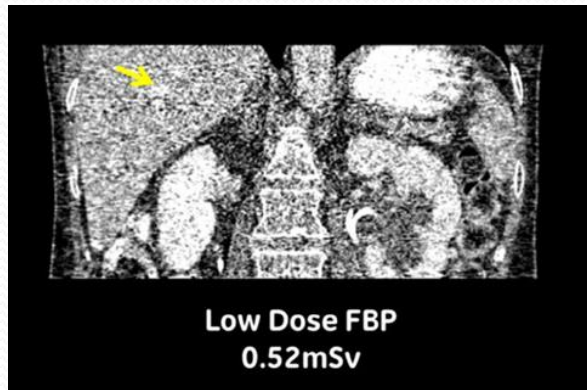
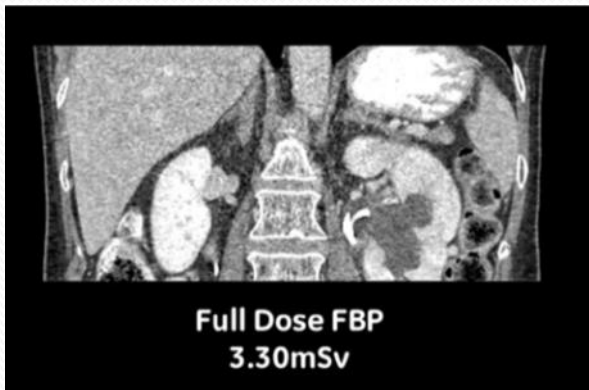
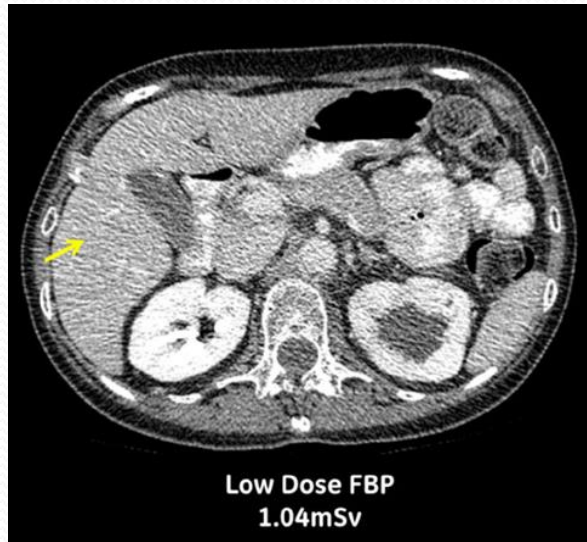
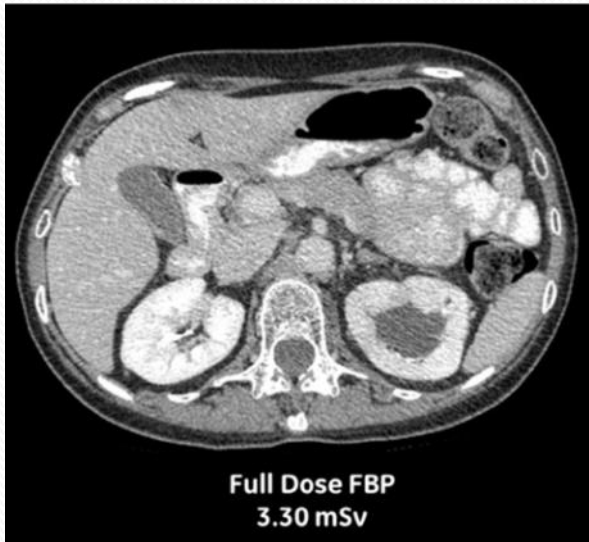
- 過去的PET/CT及SPECT/CT造影系統皆搭載濾波反投影影像重建法(filter back-projection reconstruction, FBP)來進行CT影像的重建，爾後提供PET或SPECT做影像衰減校正使用，主要原因為 FBP影像重建法對於龐大的CT影像資料處理速度既快速又簡便。
- 疊代影像重建法(iterative reconstruction, IR)為降低輻射劑量策略中最有效的方法之一，使得CT造影時可使用低劑量造影參數，達到更好的影像品質。因此，本計畫目的為建立核醫影像品質與低劑量造影參數之最佳化。



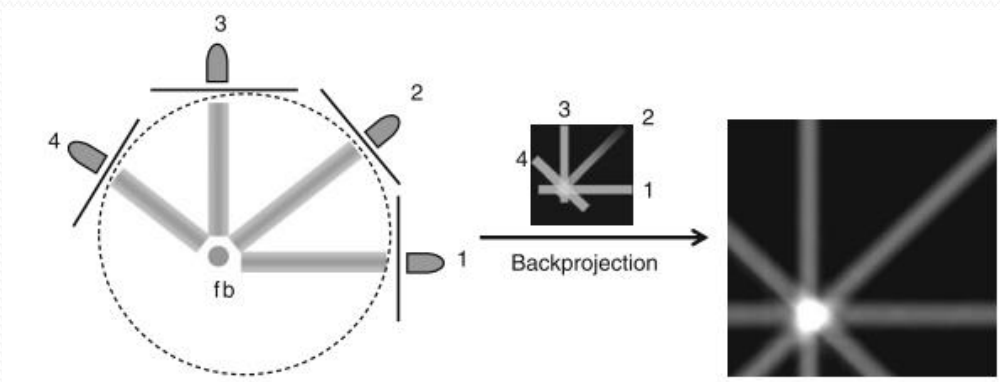


Benefits of ASiR-V\* Reconstruction  
for Reducing Patient Radiation Dose  
and Preserving Diagnostic Quality  
in CT Exams

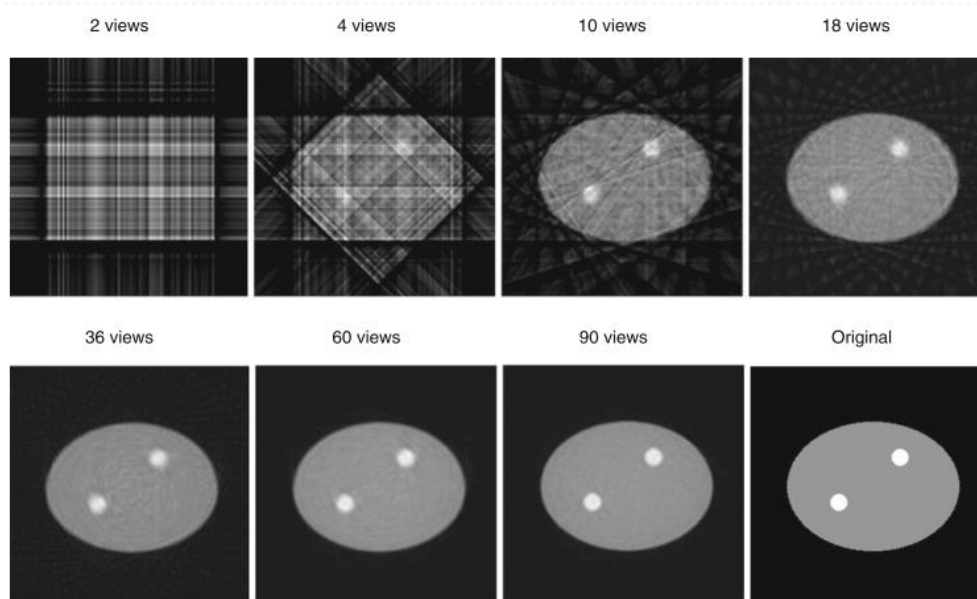
Authors: Jiahua Fan, Meghan Yue, and Roman Melnyk



# Filtered Back Projection (FBP)

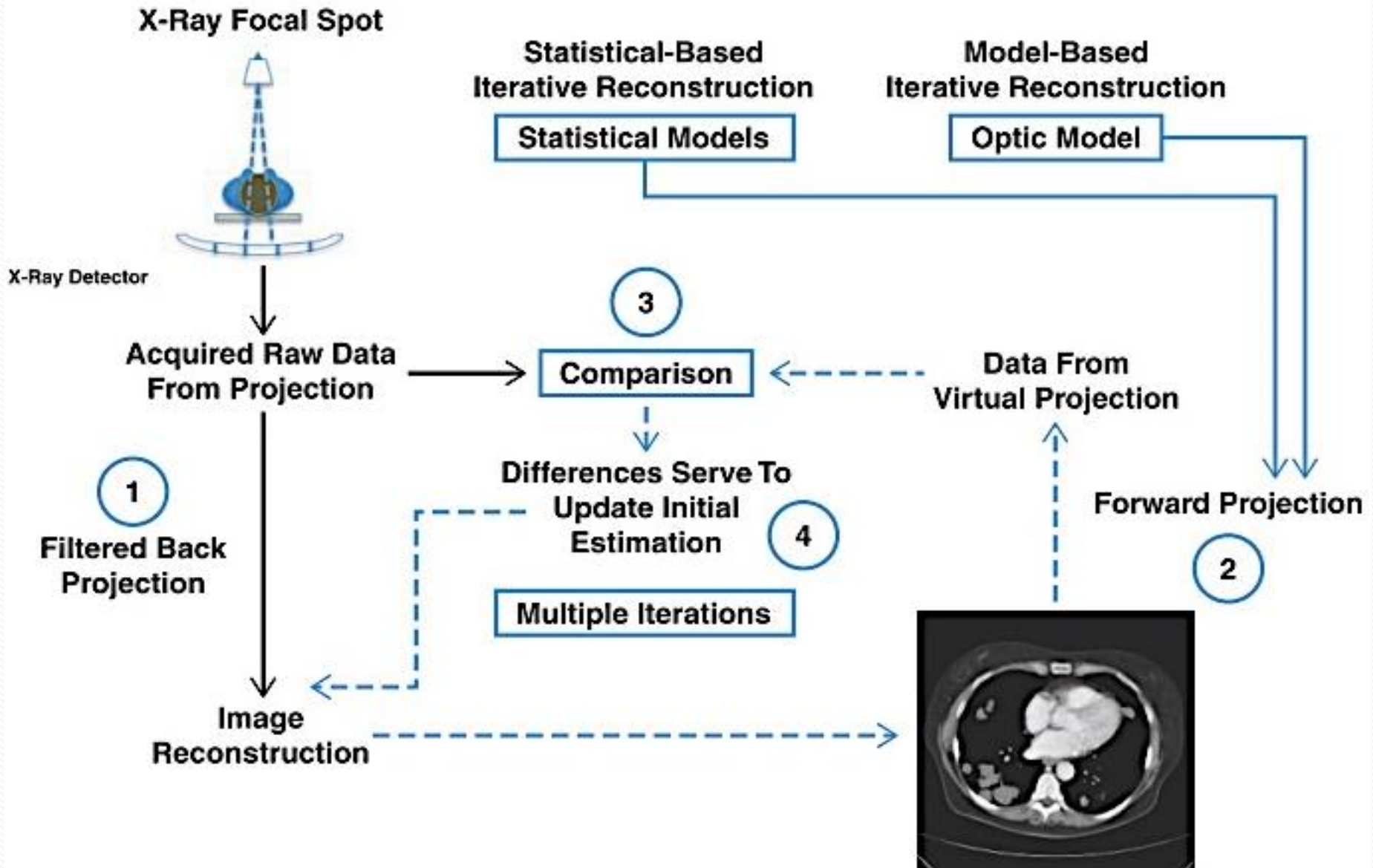


- Image reconstruction using simple backprojection.



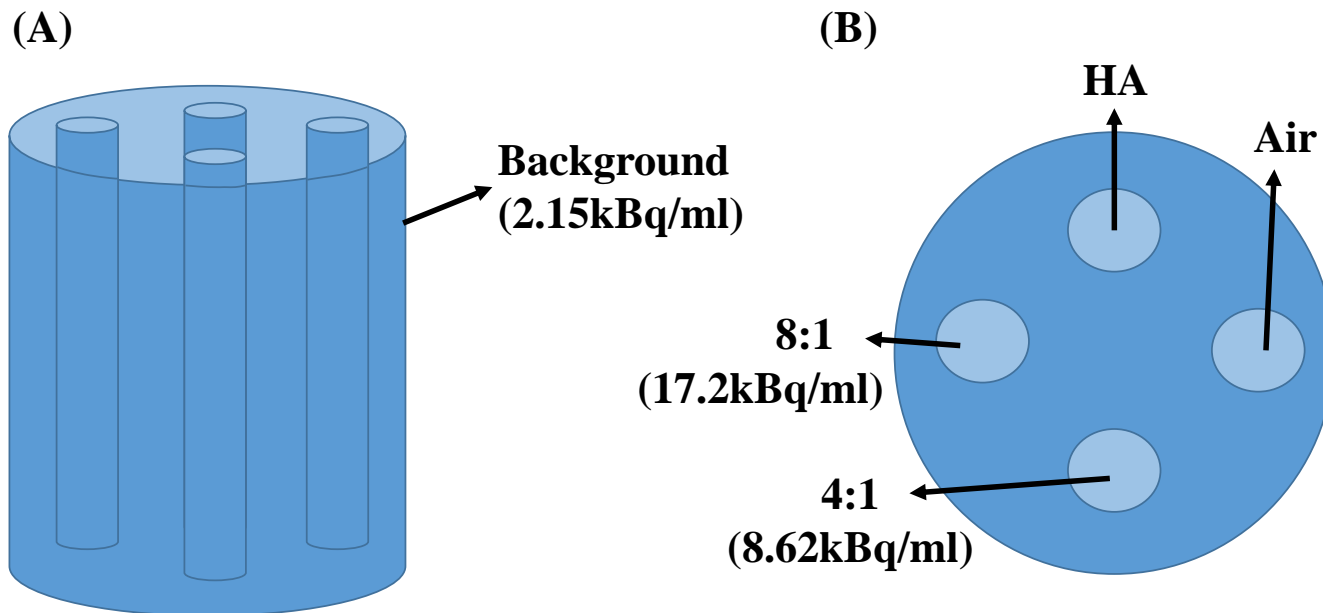
- Filtered backprojection (FBP) using different viewing angles.

# Iterative reconstruction

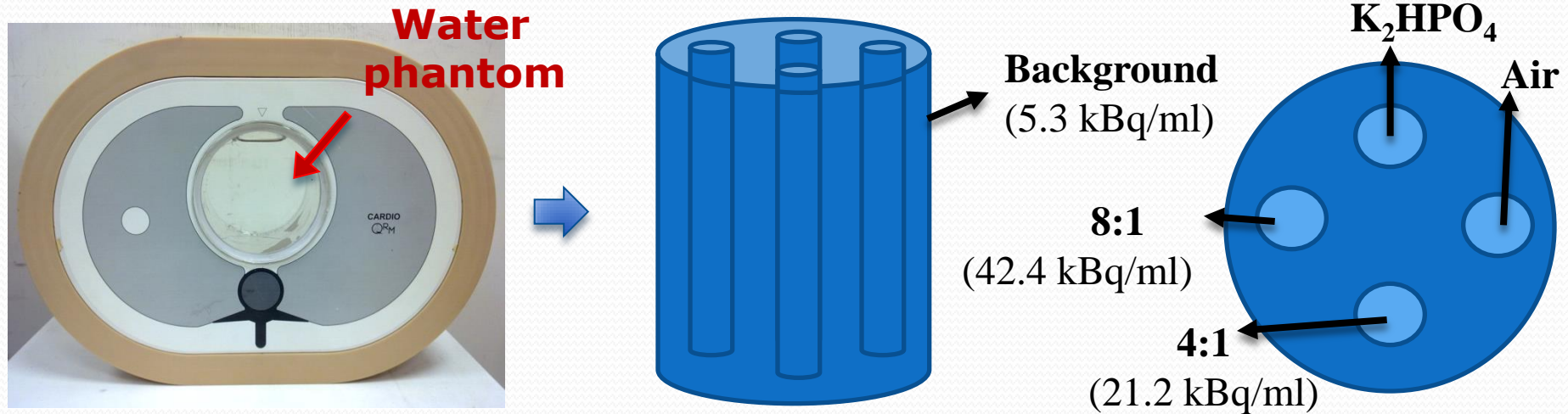


# PET/CT影像收集

使用水假體進行影像擷取，背景值(background)為 $^{18}\text{F}$ -FDG (Fludeoxyglucose)放射性同位素水溶液(圖2A)，水假體內將放置四支試管，分別為：a.空氣、b.鈣化物質(hydroxyapatite, HA;  $200\text{mg}/\text{cm}^3$ )用來模擬骨頭等效組織、c.與背景質濃度比4:1的放射性同位素水溶液、d.與背景質濃度比8:1的放射性同位素水溶液(圖2B)，目的在於模擬不同組織的密度及不同濃度的hot spot。

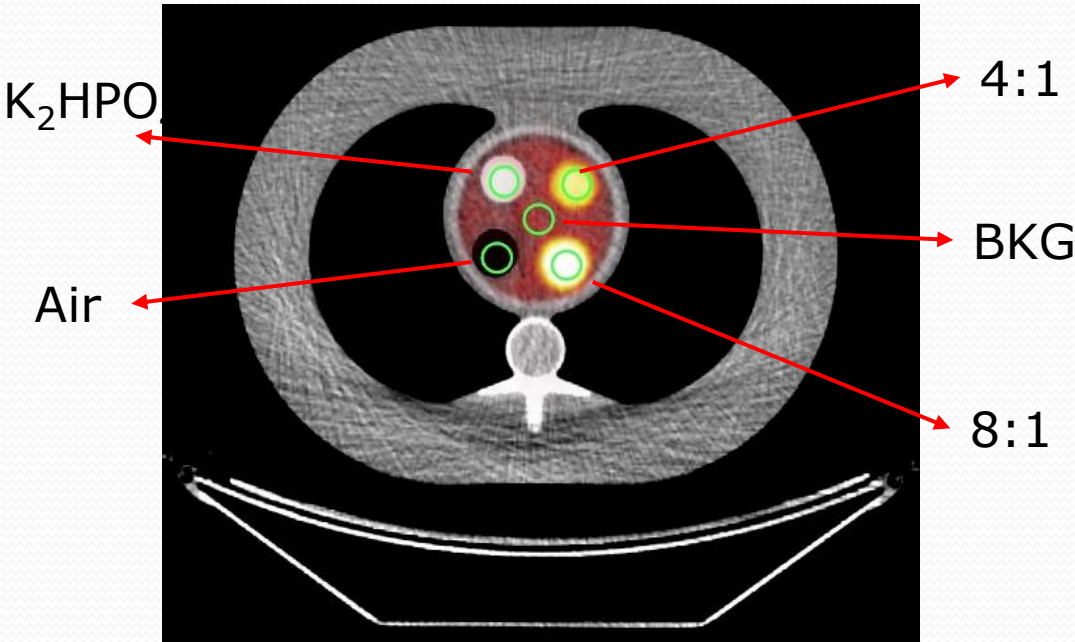


# Low-dose CTAC Evaluation



Description	Classification	Parameters
CT	kVp	120
	mA	120, 80, 60, 40, 20, 10
	Rotation time (s)	0.5
	Pitch	1.35
	Scan mode	spiral
	Reconstruction	FBP, ASiR 10%, ASiR 30%, ASiR 50%, ASiR 70%, ASiR 90%, ASiR 100%
PET	Emission time (min)	10
	Scan mode	3-D mode
	FOV	70

# PET Imaging Analysis



**OsiriX Imaging Software**  
Advanced Open-Source PACS Workstation  
DICOM Viewer

2D Viewer 3D Viewer ROI Plugins Recent Studies

Display DICOM Overlays  
 DICOM Meta-Data

**Convert from/to SUV**

Do nothing: don't convert values and don't display SUV  
 Convert all pixels to SUV  
 Display SUV for pixel under the mouse

Values stored in the DICOM file for this study:

Modifying this value WILL change the SUV values!

Patient's weight (Kg):

Injected Dose (MBq):



Corrected Dose (MBq):

Injection Time:

Acquisition Time:

Half-Life (min.):

**Warning**


 Following formula is used:
 

SUV (g/ml) = Pixel value (Bq/ml) \* Weight (kg) / Dose (Bq) \* 1000 (g/kg)

Dose is corrected by the half-life, in relation to the Acquisition Time and the Injection Time. Corrected dose = Dose \* exp (ln(2) / Half-life)

Depending on the constructor of the PET modality, the result can vary. Compare these SUV values with the values obtained directly on the PET modality, before using them.

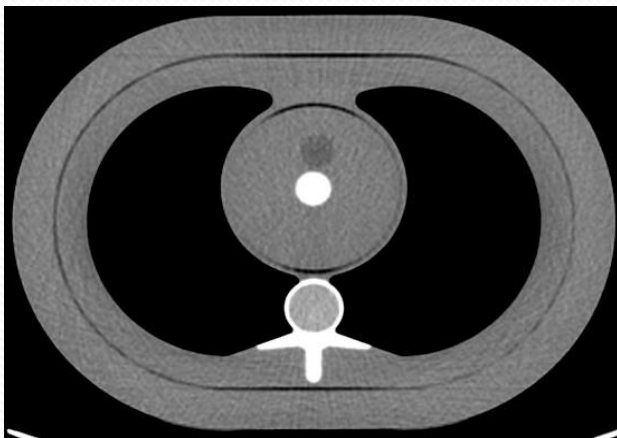
**DO NOT USE THESE VALUES FOR CLINICAL DECISIONS !**

- Standard Uptake Value, *SUV*

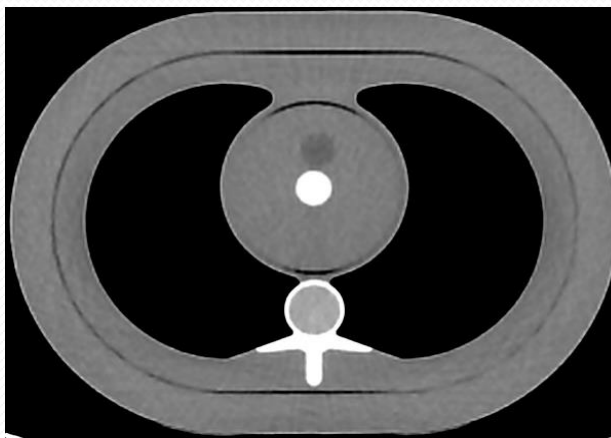
$$\frac{\text{Pixel Value} \left(\frac{\text{Bq}}{\text{ml}}\right) \times \text{Weight}(\text{kg})}{\text{Dose}(\text{Bq})} \times 1000 \left(\frac{\text{g}}{\text{kg}}\right)$$

- Statistic analysis : Independent t-test,

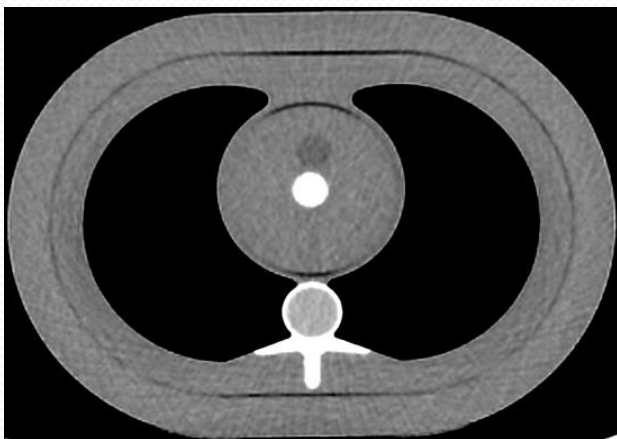
# CT images



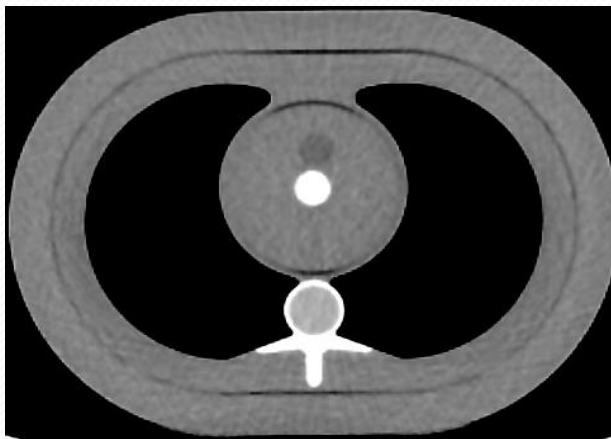
(A)  $CT_{FBP}(120mA)$



(B)  $CT_{ASiR100}(120mA)$



(C)  $CT_{ASiR70}(40mA)$



(D)  $CT_{ASiR100}(40mA)$

		CT parameter		
kVp	mA	s	Reconstruction methods	
120	10	0.5	FBP ASiR10% ASiR30% ASiR50%	ASiR70% ASiR90% ASiR100%
120	20	0.5	FBP ASiR10% ASiR30% ASiR50%	ASiR70% ASiR90% ASiR100%
120	40	0.5	FBP ASiR10% ASiR30% ASiR50%	ASiR70% ASiR90% ASiR100%
120	60	0.5	FBP ASiR10% ASiR30% ASiR50%	ASiR70% ASiR90% ASiR100%
120	80	0.5	FBP ASiR10% ASiR30% ASiR50%	ASiR70% ASiR90% ASiR100%
120	120	0.5	FBP ASiR10% ASiR30% ASiR50%	ASiR70% ASiR90% ASiR100%



## PET parameter

### PET-CTAC

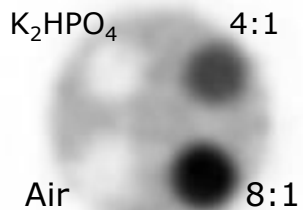
<p><math>PET_{FBP-10mA}</math>  <math>PET_{ASiR10-10mA}</math> <math>PET_{ASiR30-10mA}</math>  <math>PET_{ASiR50-10mA}</math></p>	<p><math>PET_{ASiR70-10mA}</math>, <math>PET_{ASiR90-10mA}</math>, <math>PET_{ASiR100-10mA}</math></p>
<p><math>PET_{FBP-20mA}</math>  <math>PET_{ASiR10-20mA}</math>  <math>PET_{ASiR30-20mA}</math>  <math>PET_{ASiR50-20mA}</math></p>	<p><math>PET_{ASiR70-20mA}</math>, <math>PET_{ASiR90-20mA}</math>, <math>PET_{ASiR100-20mA}</math></p>
<p><math>PET_{FBP-40mA}</math>  <math>PET_{ASiR10-40mA}</math>  <math>PET_{ASiR30-40mA}</math>  <math>PET_{ASiR50-40mA}</math></p>	<p><math>PET_{ASiR70-40mA}</math> <math>PET_{ASiR90-40mA}</math> <math>PET_{ASiR100-40mA}</math></p>
<p><math>PET_{FBP-60mA}</math>  <math>PET_{ASiR10-60mA}</math>  <math>PET_{ASiR30-60mA}</math>  <math>PET_{ASiR50-60mA}</math></p>	<p><math>PET_{ASiR70-60mA}</math>, <math>PET_{ASiR90-60mA}</math>, <math>PET_{ASiR100-60mA}</math></p>
<p><math>PET_{FBP-80mA}</math>  <math>PET_{ASiR10-80mA}</math>  <math>PET_{ASiR30-80mA}</math>  <math>PET_{ASiR50-80mA}</math></p>	<p><math>PET_{ASiR70-80mA}</math> <math>PET_{ASiR90-80mA}</math> <math>PET_{ASiR100-80mA}</math></p>
<p><math>PET_{FBP-120mA}</math>  <math>PET_{ASiR10-120mA}</math>  <math>PET_{ASiR30-120mA}</math>  <math>PET_{ASiR50-120mA}</math></p>	<p><math>PET_{ASiR70-120mA}</math>, <math>PET_{ASiR90-120mA}</math> <math>PET_{ASiR100-120mA}</math></p>

# 結果與討論

# Result (PET SUV)

PET<sub>FBP(120mA)</sub>

K<sub>2</sub>HPO<sub>4</sub> 4:1  
Air 8:1



PET<sub>FBP(80mA)</sub>



PET<sub>FBP(60mA)</sub>



PET<sub>FBP(40mA)</sub>



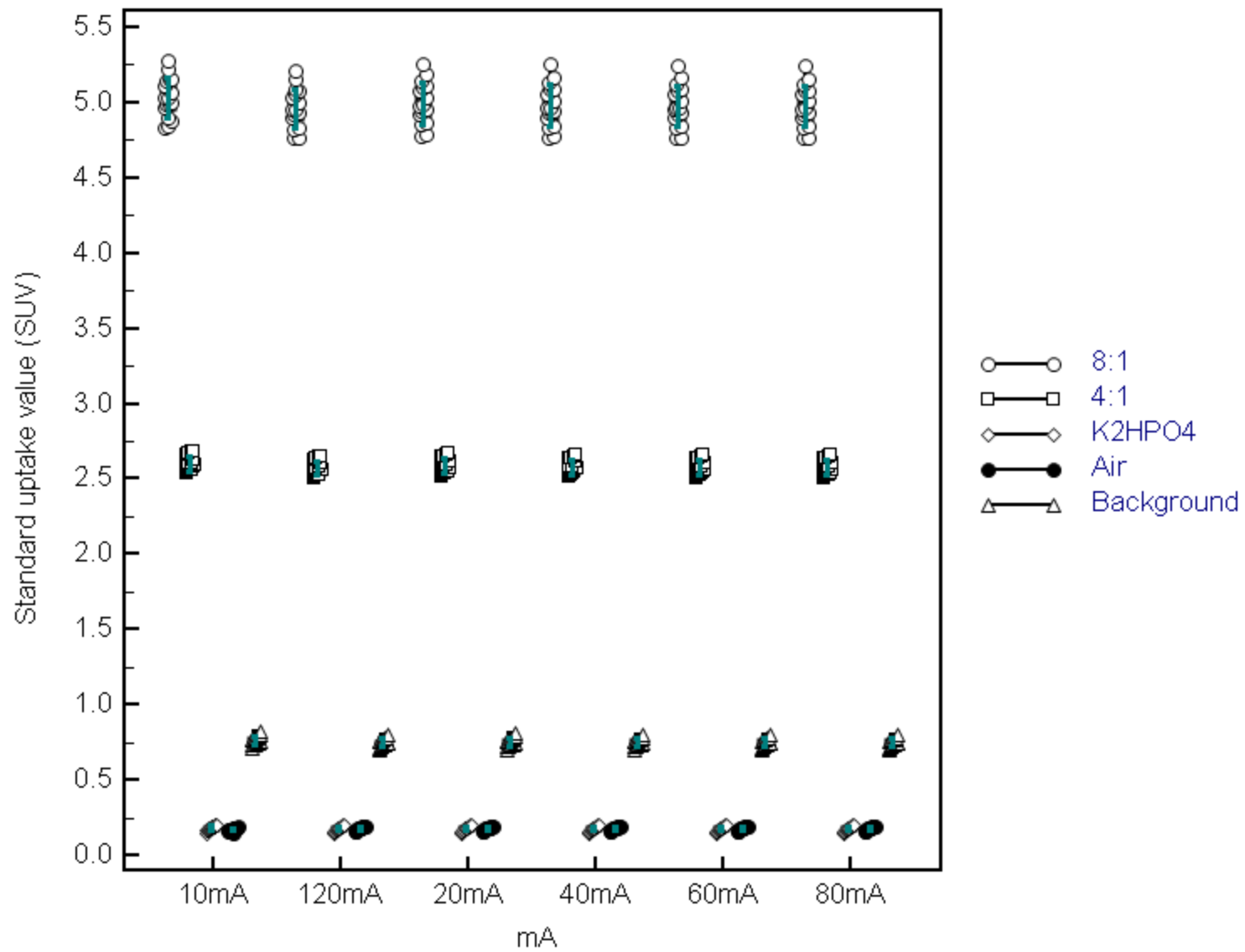
PET<sub>FBP(20mA)</sub>



PET<sub>FBP(10mA)</sub>

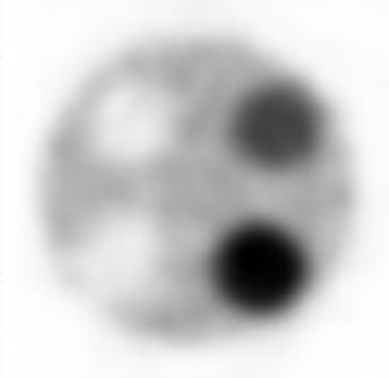


SUV	8:1		4:1		K <sub>2</sub> HPO <sub>4</sub>		Air		Background	
PET Classification	Mean±SD	R <sup>2</sup>	Mean±SD	R <sup>2</sup>	Mean±SD	R <sup>2</sup>	Mean±SD	R <sup>2</sup>	Mean±SD	R <sup>2</sup>
FBP(120mA)	4.96±0.69	1	2.57±0.32	1	0.18±0.06	1	0.18±0.06	1	0.75±0.05	1
FBP(80mA)	4.97±0.69	0.998	2.58±0.33	0.995	0.18±0.06	1	0.18±0.06	1	0.75±0.05	0.987
FBP(60mA)	4.98±0.69	0.997	2.58±0.33	0.991	0.18±0.06	1	0.18±0.06	1	0.75±0.05	0.991
FBP(40mA)	4.98±0.69	0.998	2.57±0.33	0.989	0.18±0.06	1	0.18±0.06	0.972	0.75±0.05	0.985
FBP(20mA)	4.99±0.69	0.998	2.59±0.33	0.995	0.18±0.06	0.985	0.18±0.06	0.947	0.75±0.05	0.985
FBP(10mA)	5.03±0.70	0.999	2.6±0.33	0.997	0.18±0.06	0.935	0.17±0.06	0.871	0.76±0.05	0.982

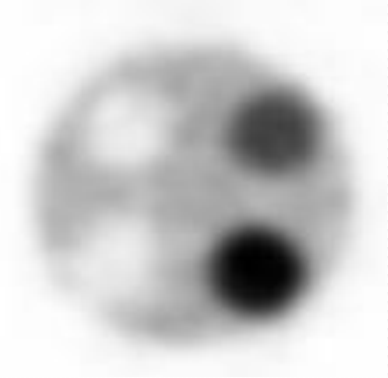


# FBP VS OSEM

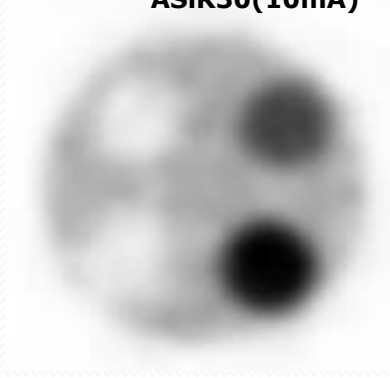
**PET** FBP(10mA)



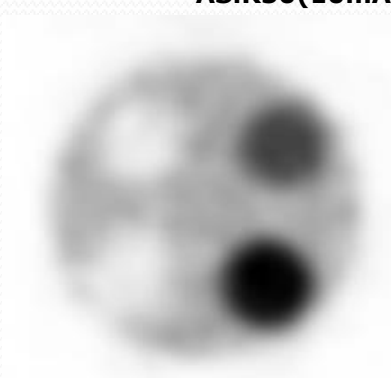
**PET** ASiR10(10mA)



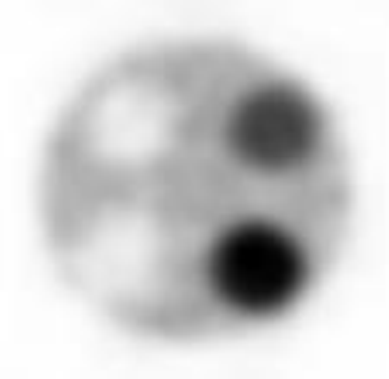
**PET** ASiR30(10mA)



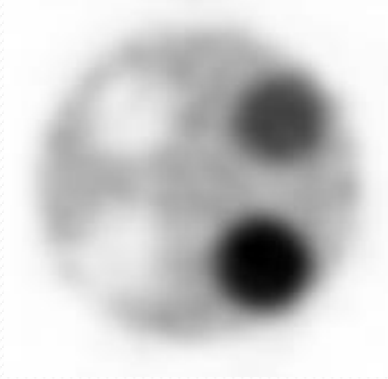
**PET** ASiR50(10mA)



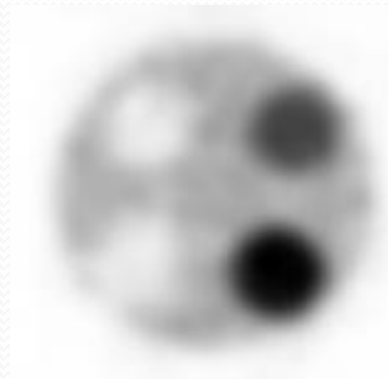
**PET** ASiR70(10mA)



**PET** ASiR90(10mA)

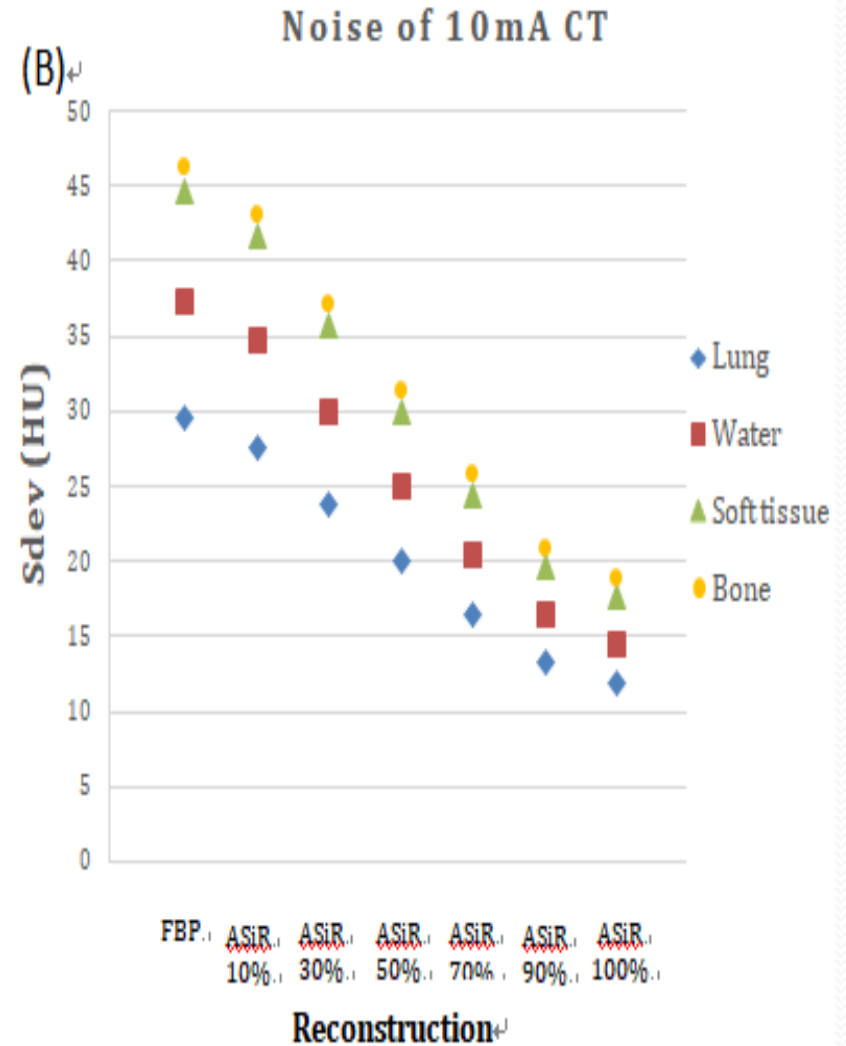
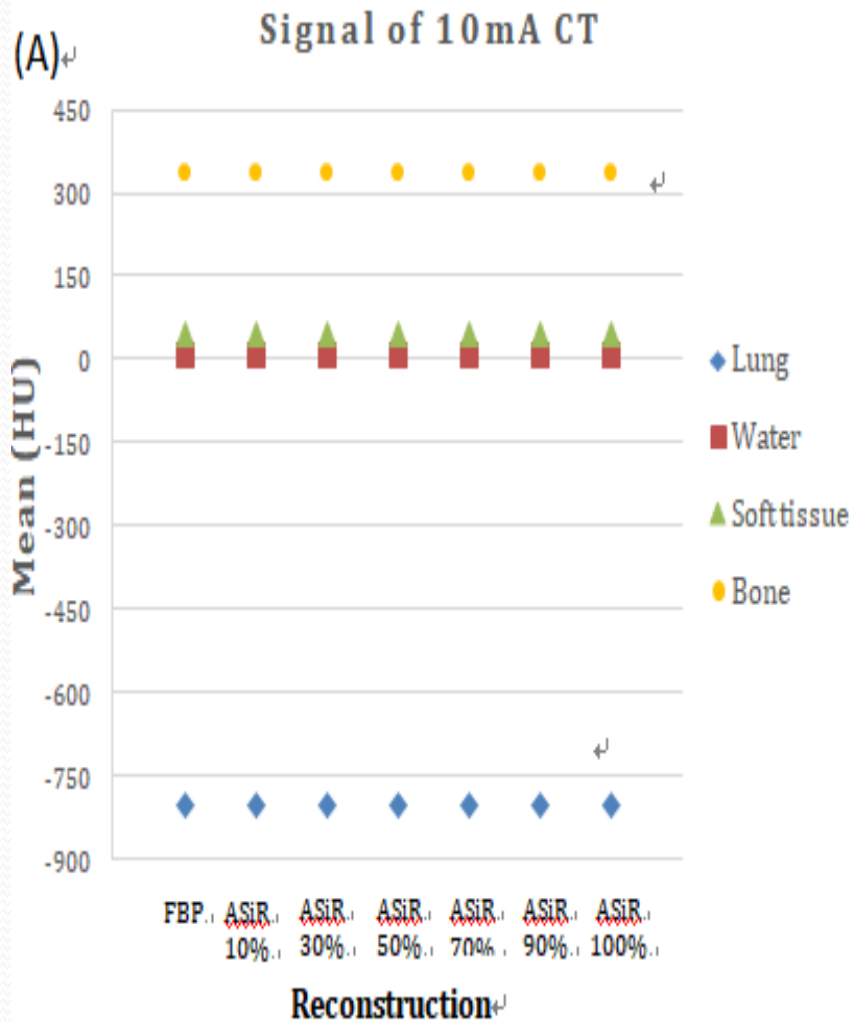


**PET** ASiR100(10mA)



SUV	8:1		4:1		K <sub>2</sub> HPO <sub>4</sub>		Air		Background	
PET Classification	Mean±SD	R <sup>2</sup>	Mean±SD	R <sup>2</sup>	Mean±SD	R <sup>2</sup>	Mean±SD	R <sup>2</sup>	Mean±SD	R <sup>2</sup>
FBP(10mA)	5.03±0.70	1	2.60±0.33	1	0.18±0.06	1	0.17±0.06	1	0.76±0.05	1
ASiR10 (10mA)	5.03±0.70	1	2.60±0.33	1	0.18±0.06	1	0.17±0.06	1	0.76±0.05	1
ASiR30 (10mA)	5.03±0.70	1	2.60±0.33	0.999	0.18±0.06	1	0.17±0.06	0.966	0.76±0.05	1
ASiR50 (10mA)	5.03±0.70	0.999	2.60±0.33	0.999	0.18±0.06	1	0.17±0.06	0.966	0.76±0.05	1
ASiR70 (10mA)	5.03±0.70	0.999	2.60±0.33	0.998	0.18±0.06	0.984	0.17±0.06	0.966	0.76±0.05	1
ASiR90 (10mA)	5.03±0.70	0.999	2.60±0.33	0.998	0.18±0.06	0.984	0.17±0.06	0.966	0.76±0.05	1
ASiR100 (10mA)	5.03±0.70	0.999	2.60±0.33	0.997	0.18±0.06	0.984	0.17±0.06	0.913	0.76±0.05	1

# FBP VS OSEM





# Radiation Dose Concerns

- From Image Wisely (web of ACR and RSNA)

Typical acquisition techniques used for whole-body FDG-PET-CT imaging

Study	Injected Activity	Effective Dose Estimate
PET <sup>6, 7</sup>	[5-15] mCi <sup>18</sup> F-FDG Injected (185-555 MBq)	3.5-10.5 mSv
CT for diagnostic purposes <sup>8</sup>	[110-200] mAs <sup>1</sup> CTDIvol = [8-14] mGy	11-20 mSv
CT for anatomic localization <sup>8</sup>	[30-60] mAs <sup>3</sup> CTDIvol = [2-4] mGy	3-6 mSv
CT for attenuation correction only <sup>8</sup>	[5-10] mAs <sup>4</sup> CTDIvol = [0.3-1.0] mGy	0.5-1.0 mSv

For ease of comparison, all CT studies presented are performed with 120 kVp, pitch 1.375, 40 mm collimation, 900 mm scan range, average tube current-time product.

# PET Diagnostic Accuracy: Improvement with In-Line PET-CT System: Initial Results

**TABLE 1**  
Differentiation of Classified Lesions

Classification	PET Alone	PET-10-mA CT	PET-40-mA CT	PET-80-mA CT	PET-120-mA CT
Tumor	137	135	135	137	137
Inflammation	40	50	56	55	55
Other lesion	44	54	57	59	59
Total ( <i>n</i> = 287)	221 (77)	239 (83)	248 (86)	251 (87)	251 (87)

Note.—Numbers in parentheses are percentages.

**TABLE 2**  
Analysis of Lesions Classified as Tumors

Lesion	PET Alone	PET-10-mA CT	PET-40-mA CT	PET-80-mA CT	PET-120-mA CT
Tumor	137	135	135	137	137
TP	123	133	133	135	135
FP	6	1	1	1	1
FN	8	1	1	1	1

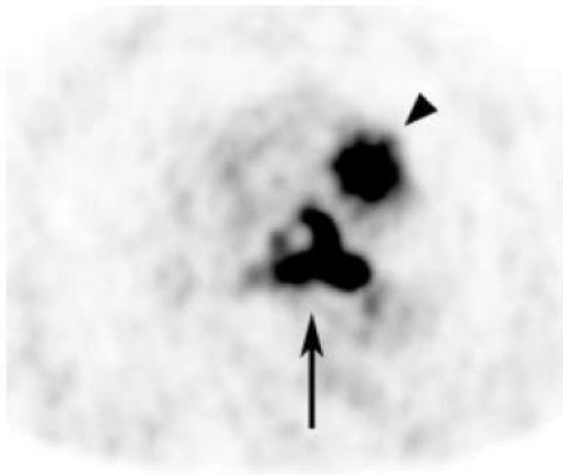
**TABLE 3****Analysis of Lesions Classified as Tumors Compared with Standard of Reference**

Result	PET Alone	PET-10- mA CT	PET-40- mA CT	PET-80- mA CT	PET-120- mA CT
TP	123	133	133	135	135
TN	84	109	112	115	115
FP	6	1	1	1	1
FN	13	5	5	3	3
Undecided	61 (21)	39 (14)	36 (13)	33 (12)	33 (12)
Sensitivity (%)	90	96	96	98	98
Specificity (%)	93	99	99	99	99
Accuracy (%)	91	97	97	98	98
Significance of differences*					
Between PET-CT and PET alone		<.01	<.05	<.05	<.05
Between PET-CT techniques		NS	NS	NS	NS

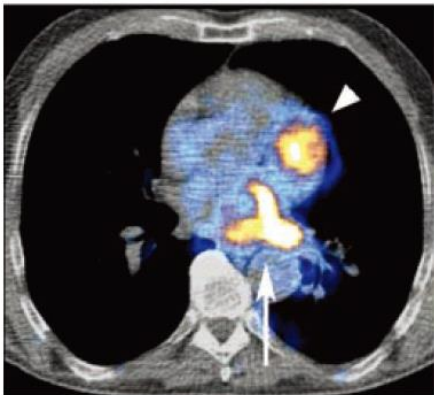
Note.—Numbers in parentheses are percentages of 287 lesions.

\* McNemar test ( $\chi^2$ ), step-by-step analysis. NS = not significant.

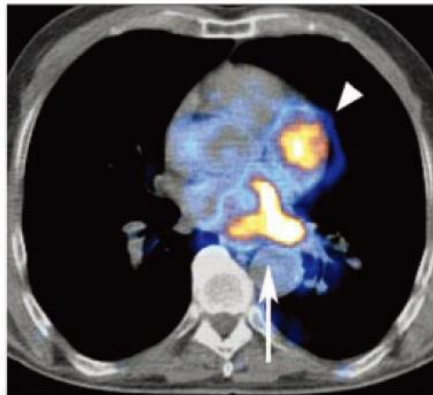
Left-sided intrapulmonary mass (sarcomatoid tumor) in a 76-year-old male patient. **(a) Transverse FDG PET image** shows pathologic uptake of FDG (arrow in a–e) in the infracarinal region and physiologic uptake of FDG (arrowhead in a–e) in the heart. **(b) Transverse PET–10-mA CT scan** at the same level as a shows the tumor to be in the left atrium. **(c) PET–40-mA CT, (d) PET–80-mA CT, and (e) PET–120-mA CT** images at the same level as a and b do not give additional information.



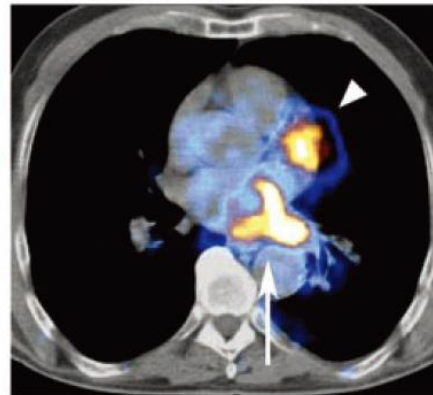
a.



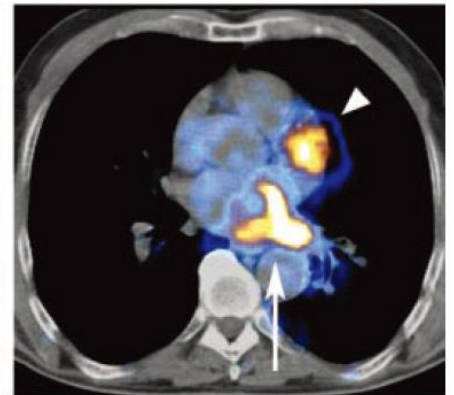
b.



c.



d.



e.

# 結語

- 透過上述的分析結果，可以得知低劑量CT造影條件對CT、PET、SPECT影像品質造成的影響並不是很大，甚至在低劑量影像之間是幾乎沒有影響；適當運用IR影像重建法可以有效改善低劑量影像之雜訊，提高影像品質，證明低劑量CT在核醫影像檢查具有臨床診斷價值，進一步達到降低病人醫療輻射曝露累積劑量的效果。

# Imaging Artifacts from CTAC

# Imaging Artifacts from CT

## 1. Metal Artifacts

假牙、金屬關節、對比劑、鋇劑、ECG墊片、人工血管等等

## 2. Motion Artifacts

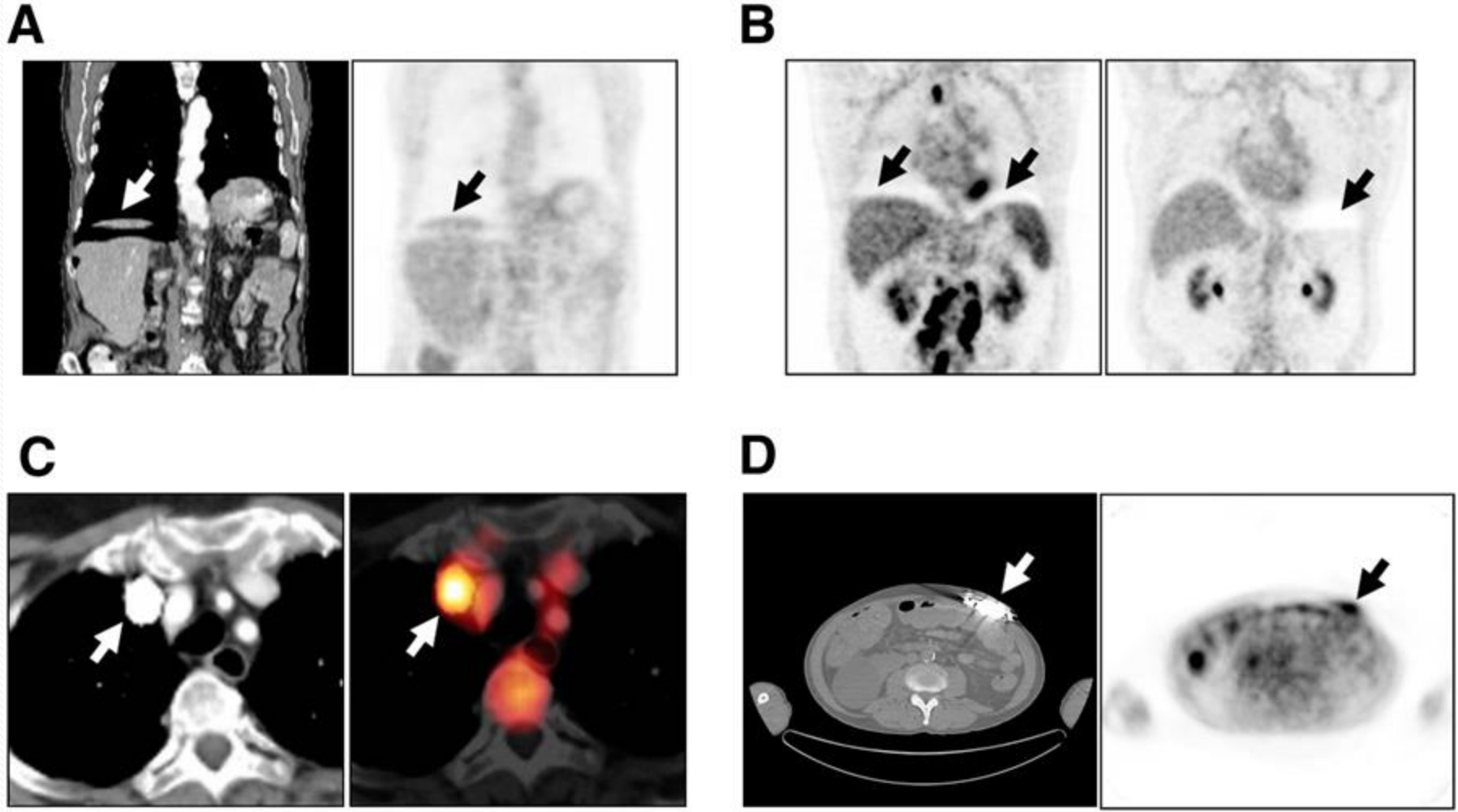
呼吸移動、躁動

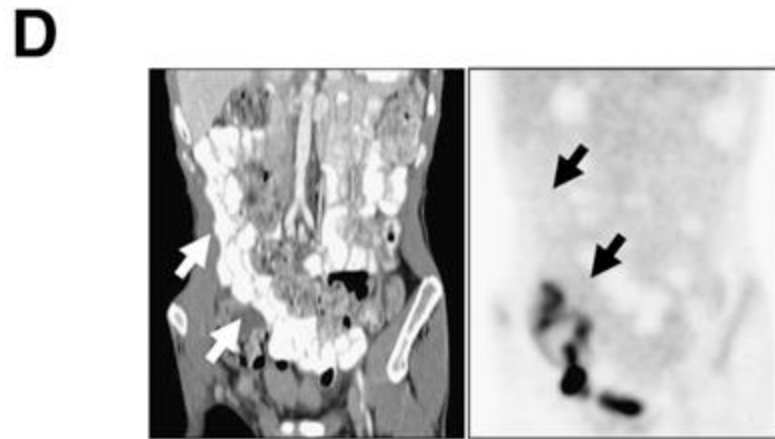
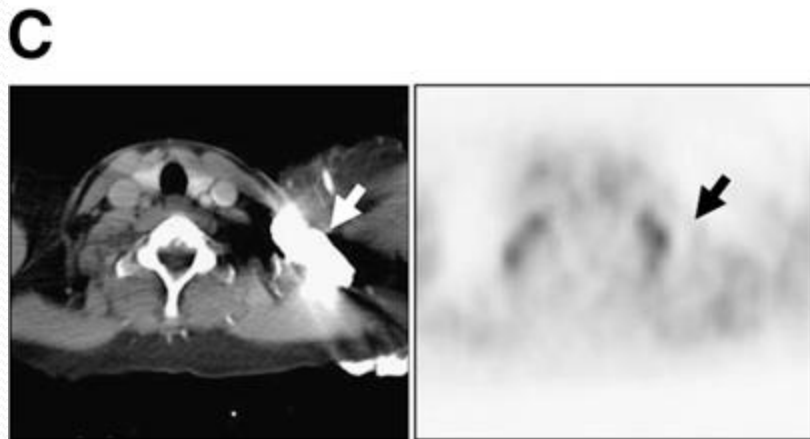
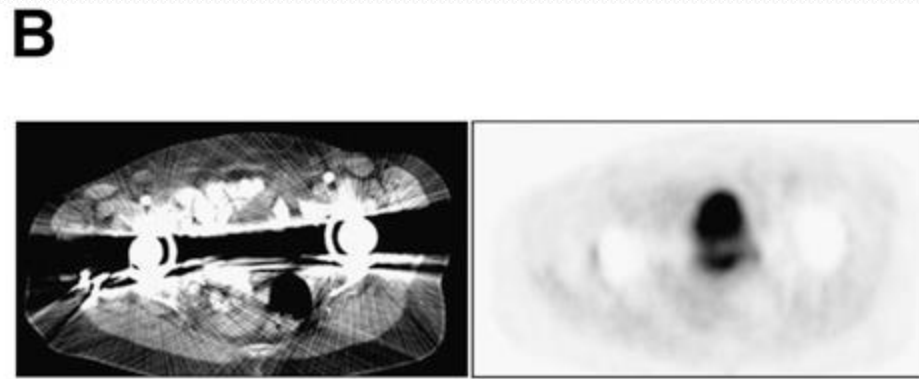
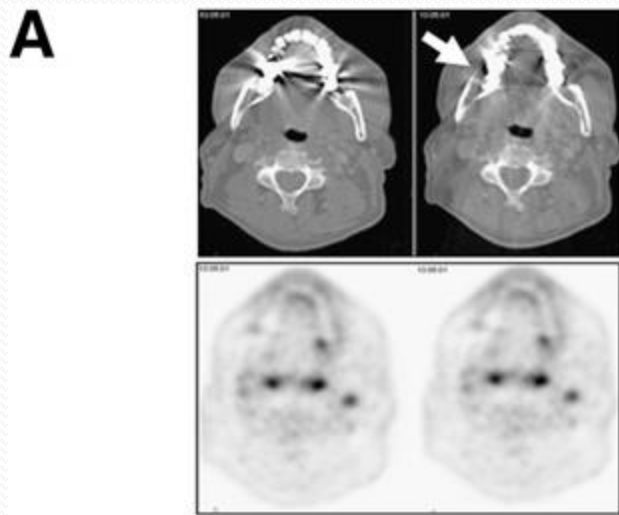
# 衣服有亮片 ( CT )



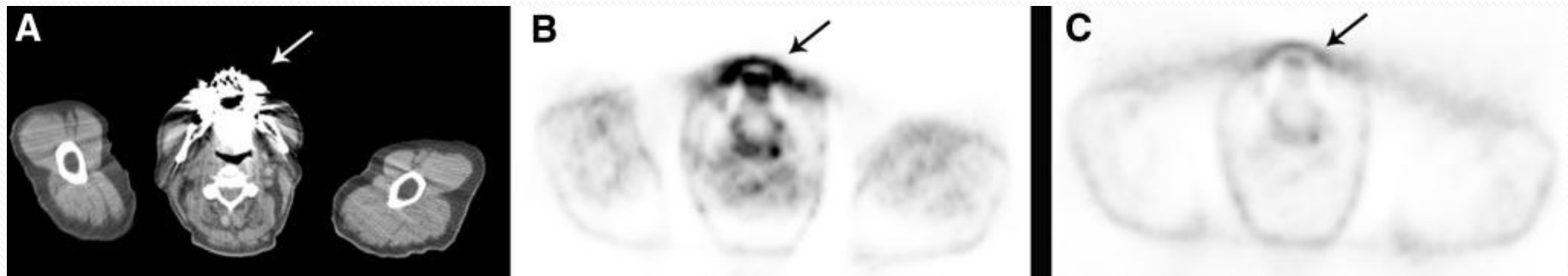


# Potential image artifacts generated from CT-AC





# Metal Artifacts



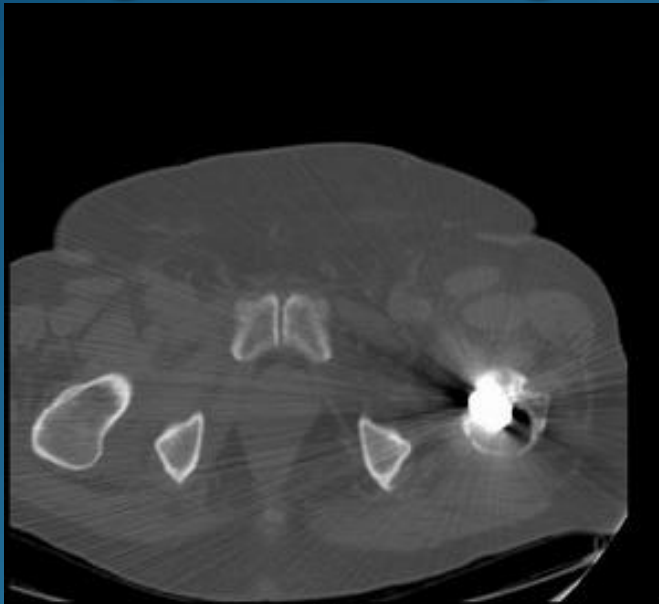
A:嘴巴有金屬而形成CT streaking artifacts

B:PET 影像因AC 的過度補償而形成嘴巴的uptake增高

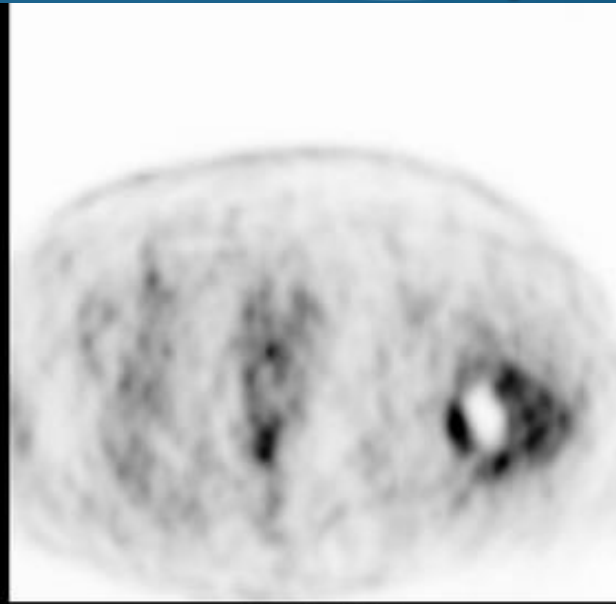
C:PET 影像無AC 的影像

# Hip Prosthesis

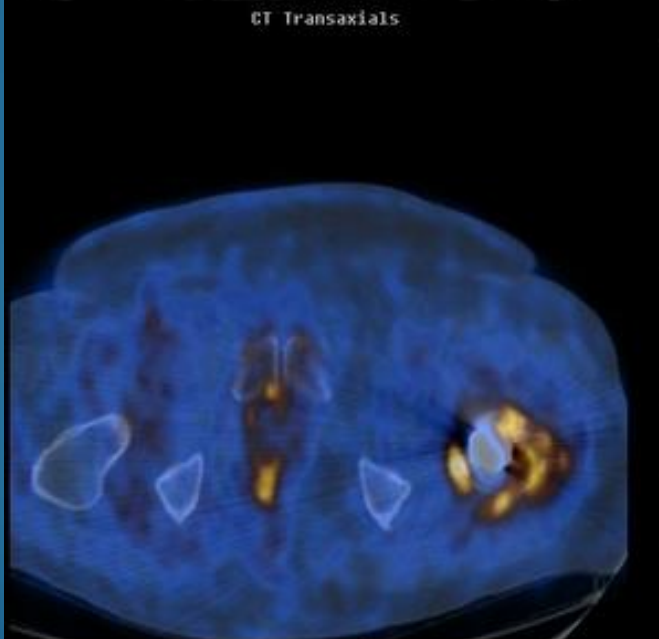
# Benign Pathological Variants: Hip Prosthesis



CT Transaxials



PET Transaxials



Fused Transaxials

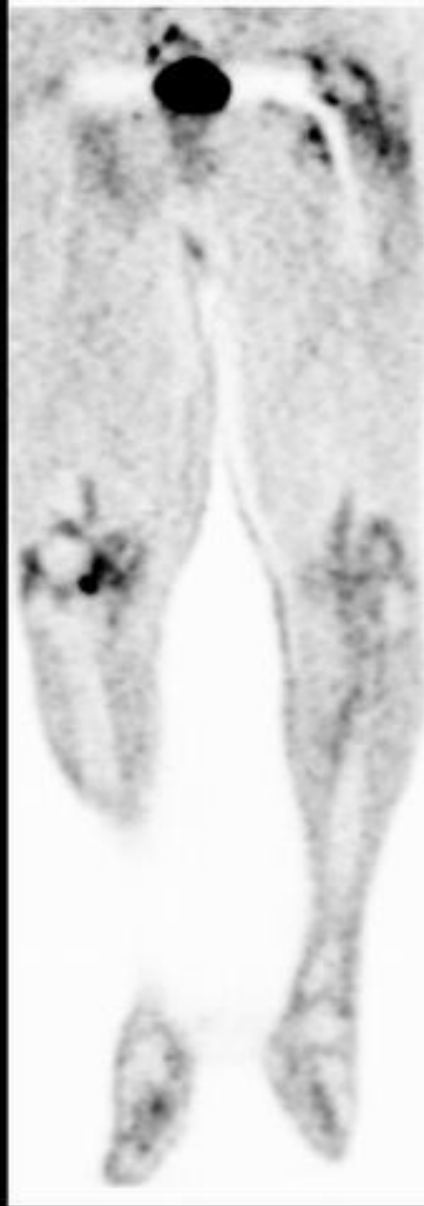


PET NACTransaxials

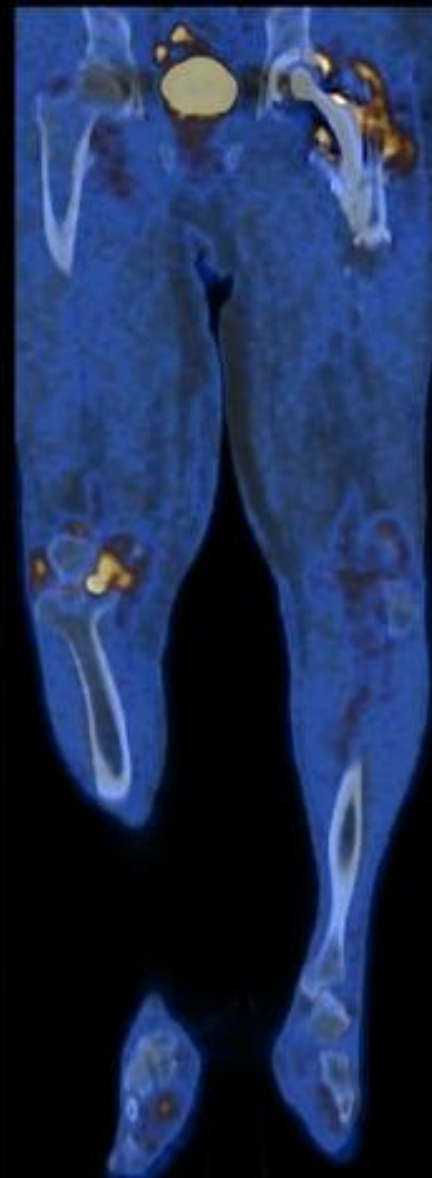
# Benign Pathological Variants: Hip Prosthesis



CT Coronals



PET Coronals



Fused Coronals

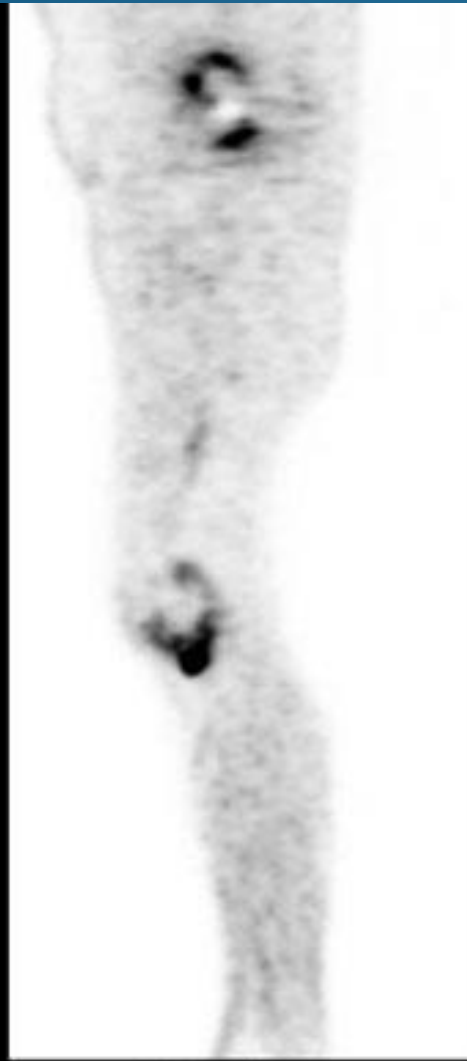


PET MIP Coronals

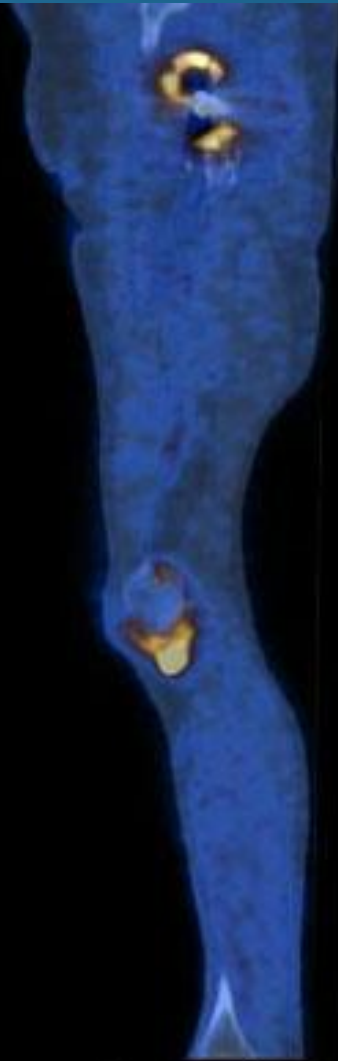
# Benign Pathological Variants: Hip Prosthesis



CT Sagittals



PET Sagittals

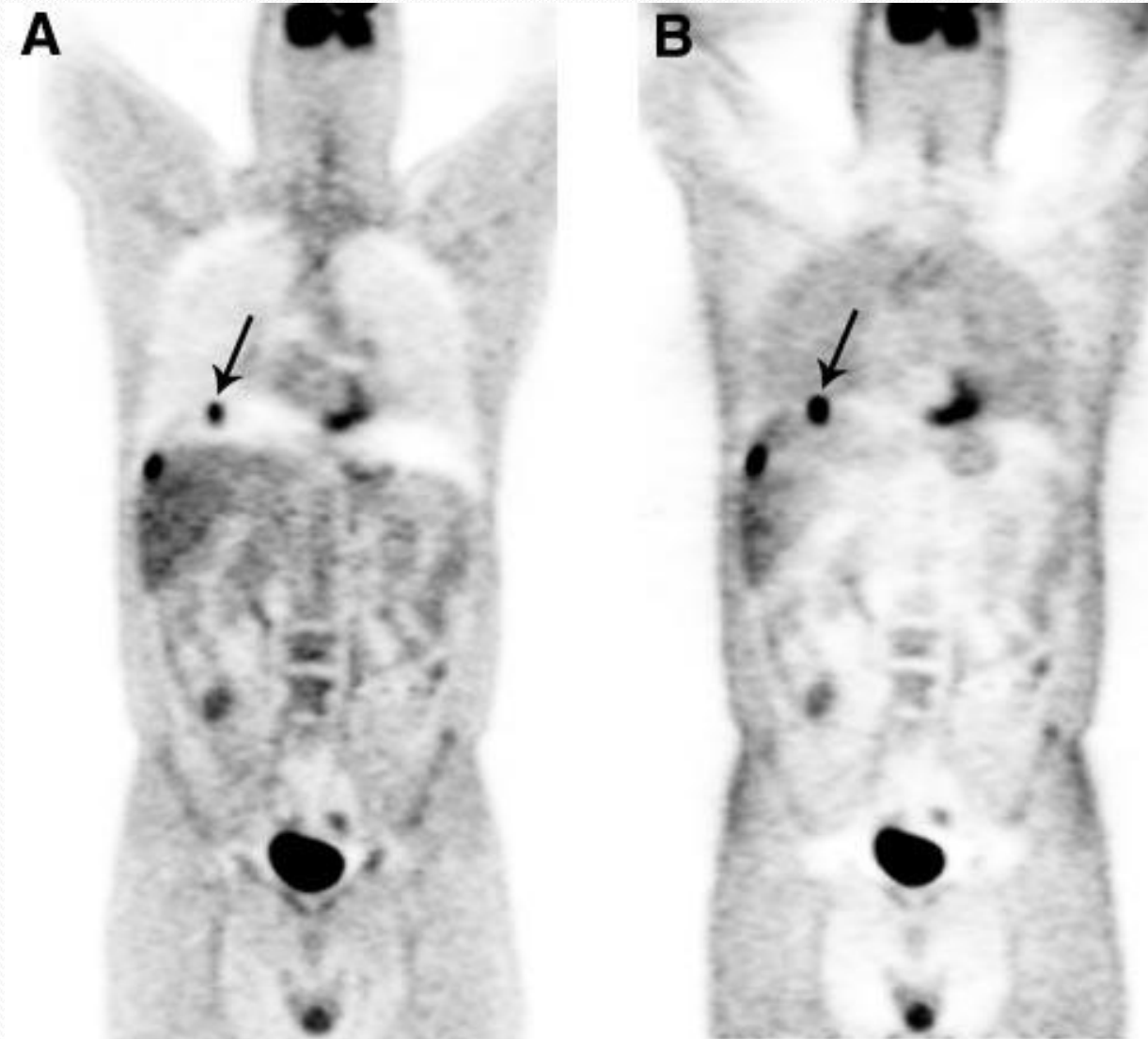


Fused Sagittals



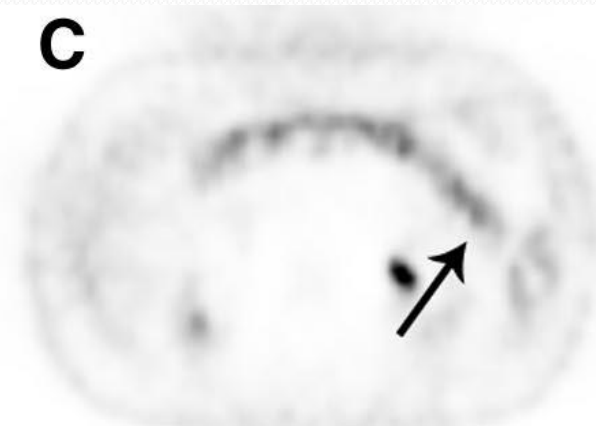
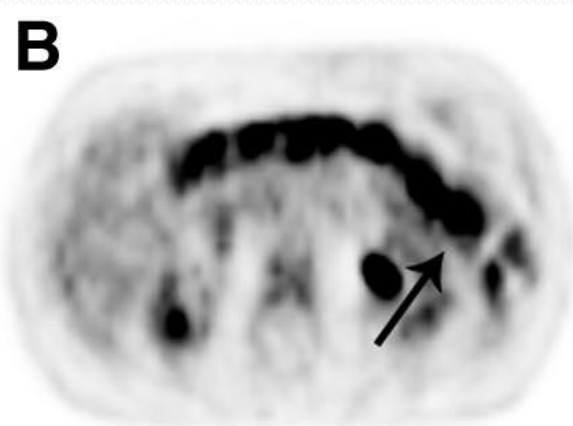
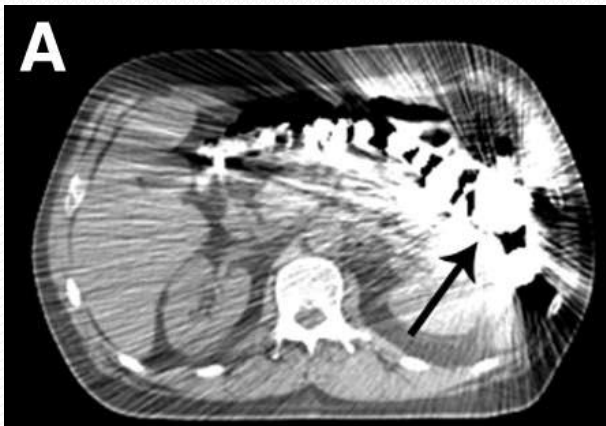
PET NACSagittals

# Motion



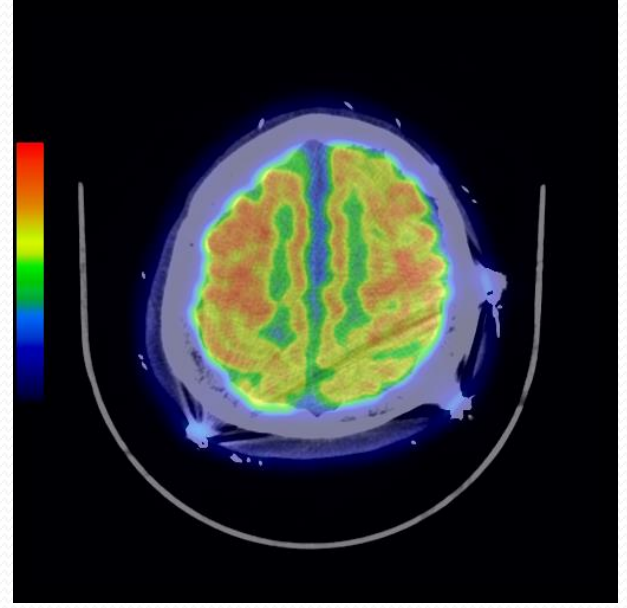
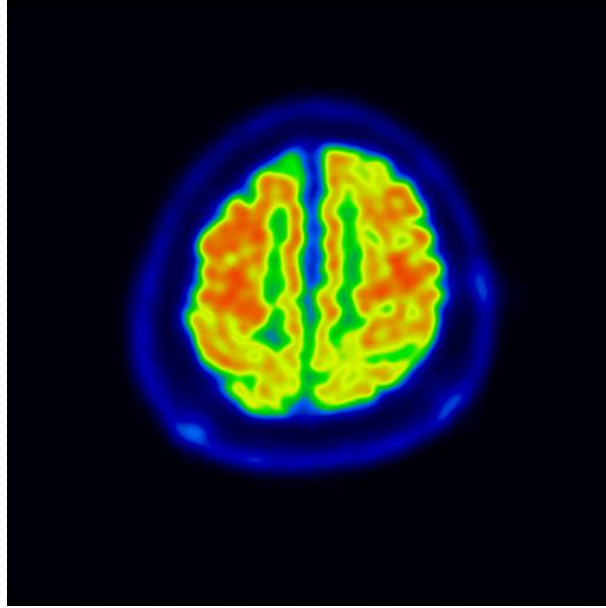
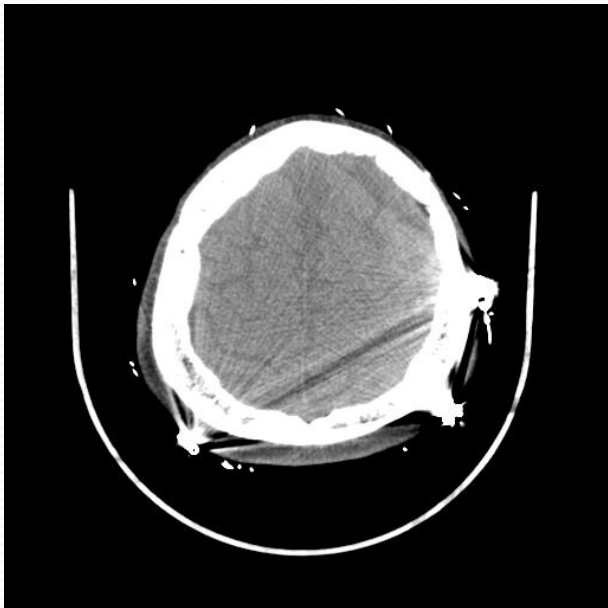


# Barium

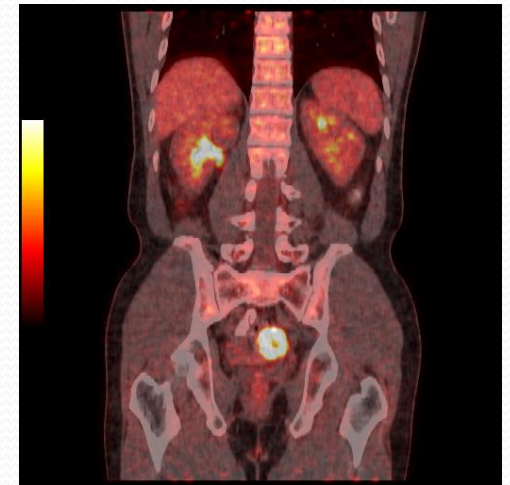
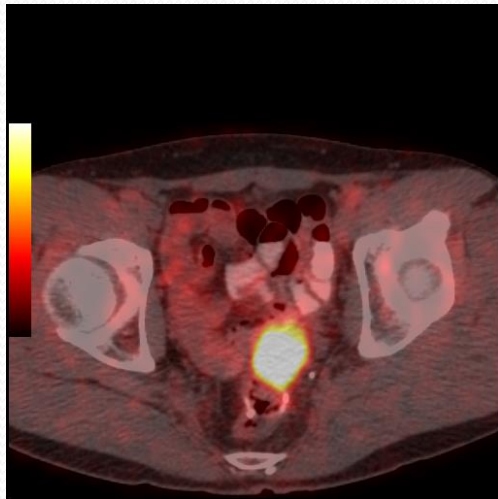
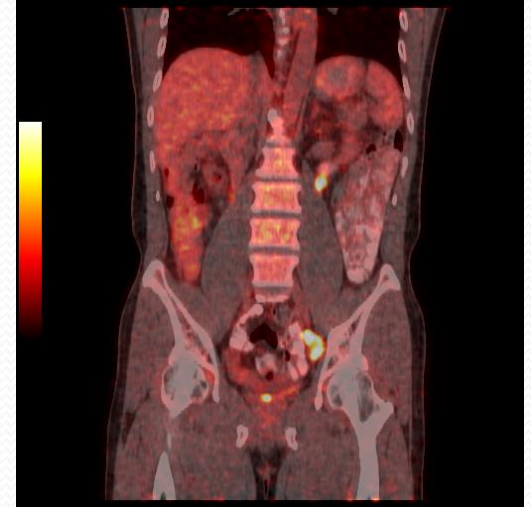
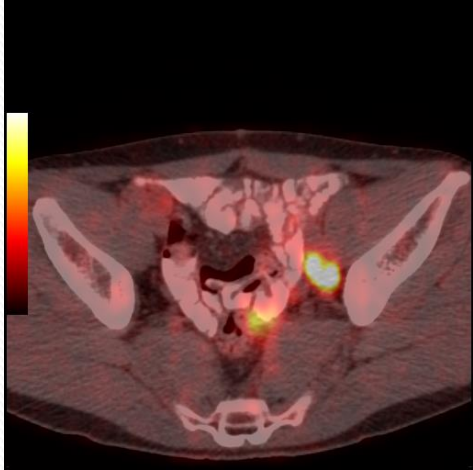


- A 檢查前一天有做鋇劑腸胃造影
- B:PET影像 高AC 的補償
- C:PET 影像 No AC的補償

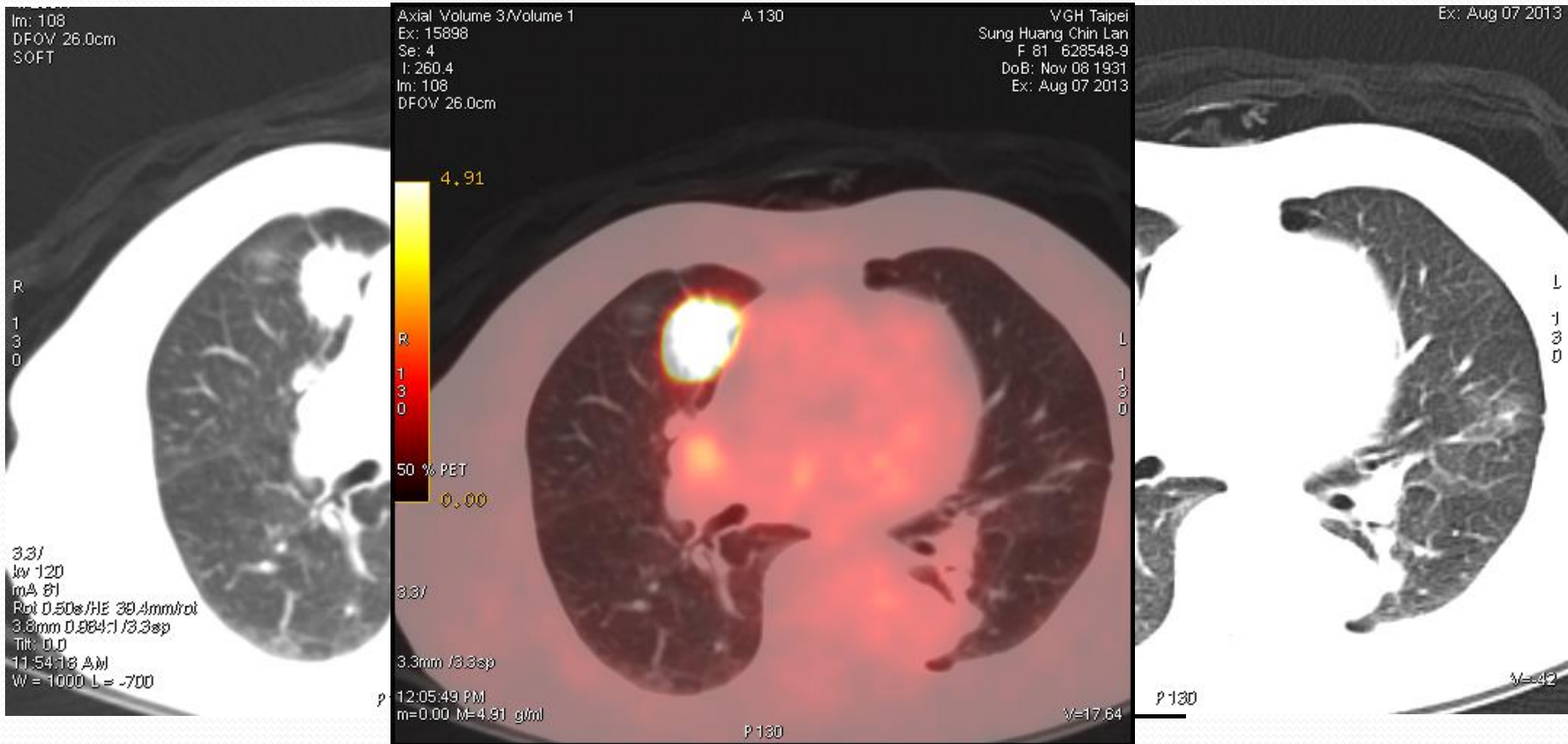
# Epilepsy



# Oral CM



# What's different?



Volume 1

S 138

VGH Taipei  
Hung Chen Fang  
M 41 3676388-9  
DoB: Jul 11 1967

VGH Taipei  
Hung Chen Fang  
M 41 3676388-9

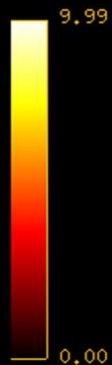
VGH Taipei  
Hung Chen Fang  
M 41 3676388-9  
DoB: Jul 11 1967  
Ex: Jul 02 2009

Axial Volume 2/Volume 1  
Ex: 5810  
Se: 4  
I: 342.8  
Im: 143  
DFOV 50.0cm

A 250



1915



R  
3  
5  
4

50 % PET

3.3/

3.3mm /3.3var.sp

03:48:22 PM  
m=0.00 M=9.99 g/ml



L  
3  
5  
4

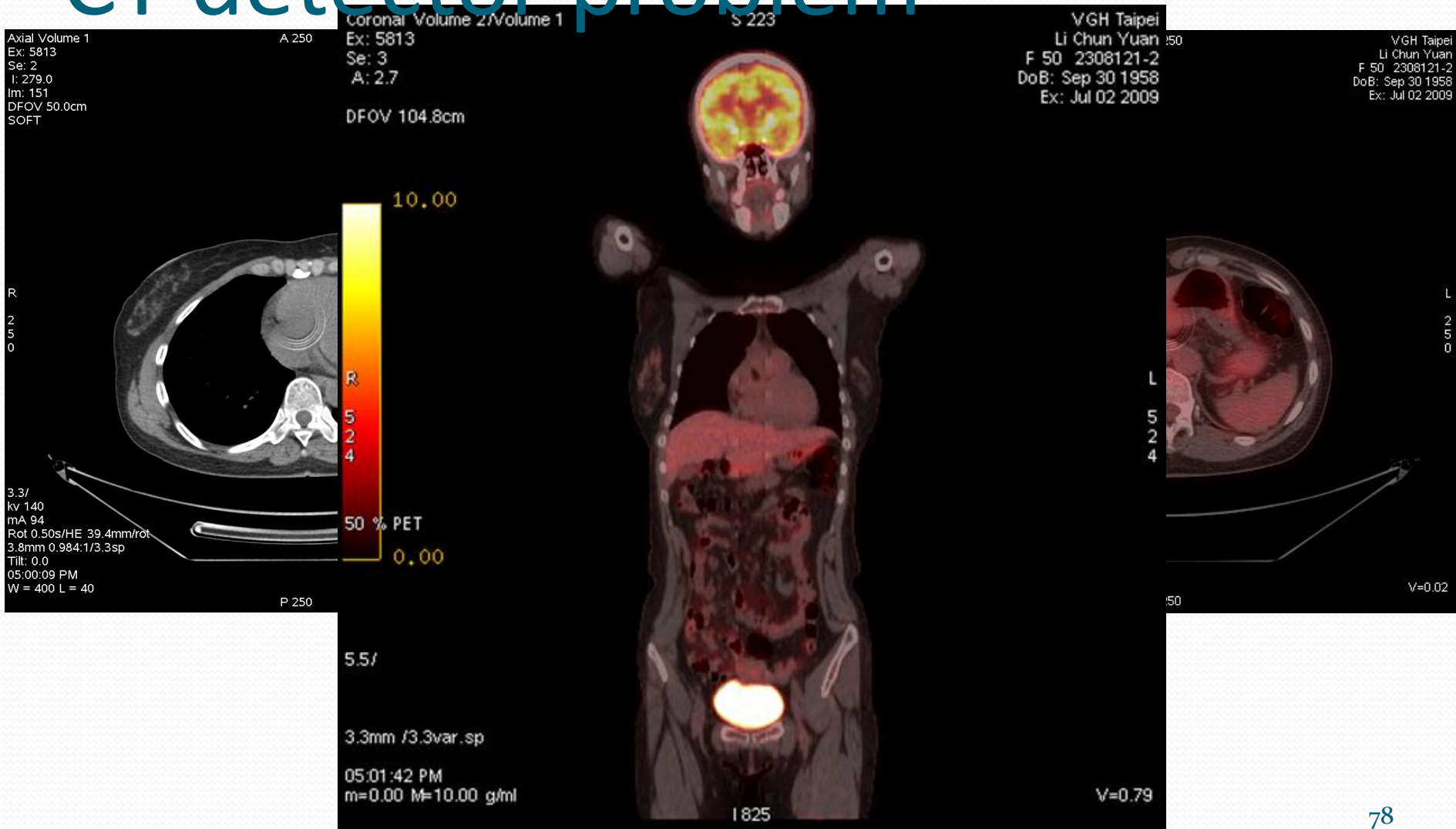
P 250

V=2.45

Y=-1.62

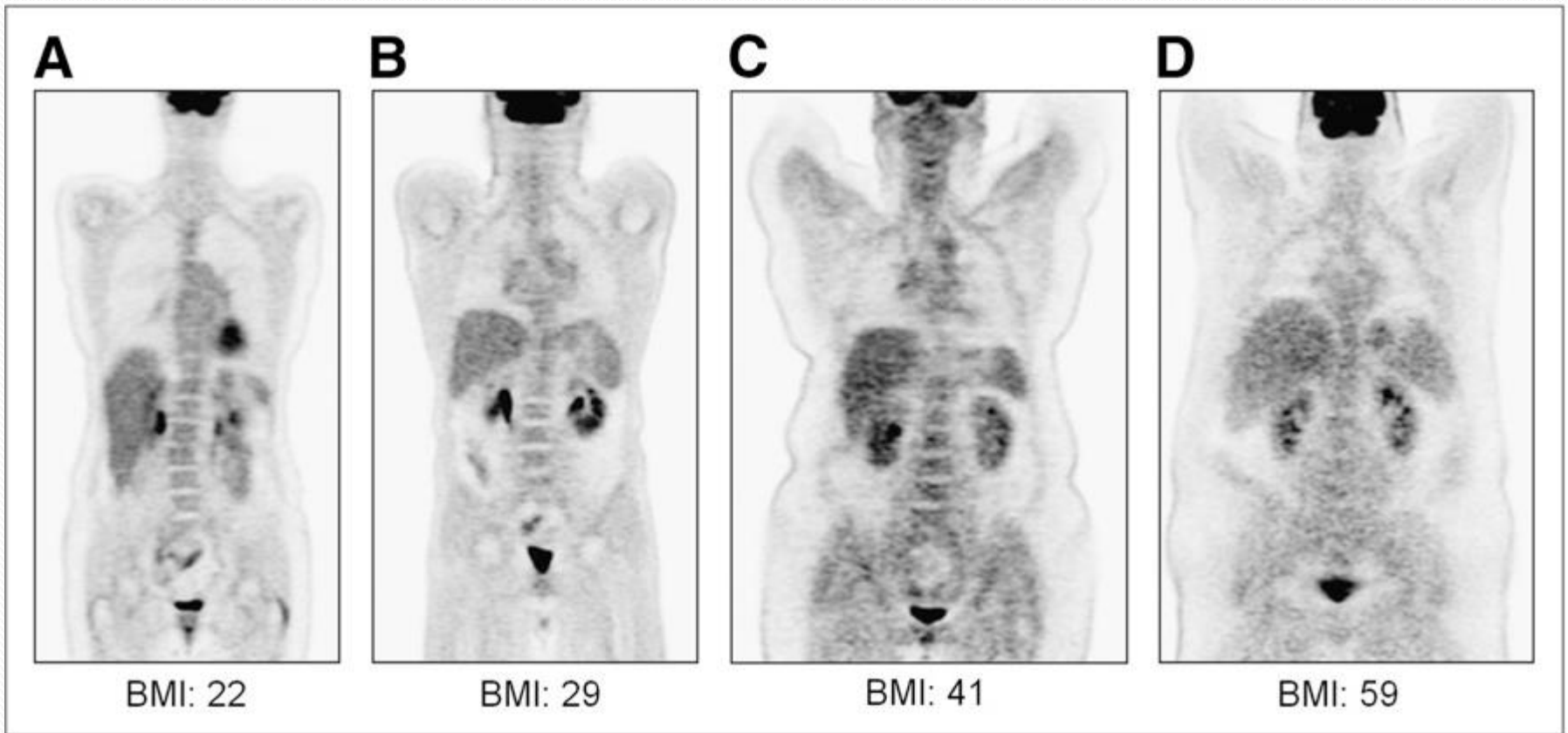
V=2.45

# CT detector problem

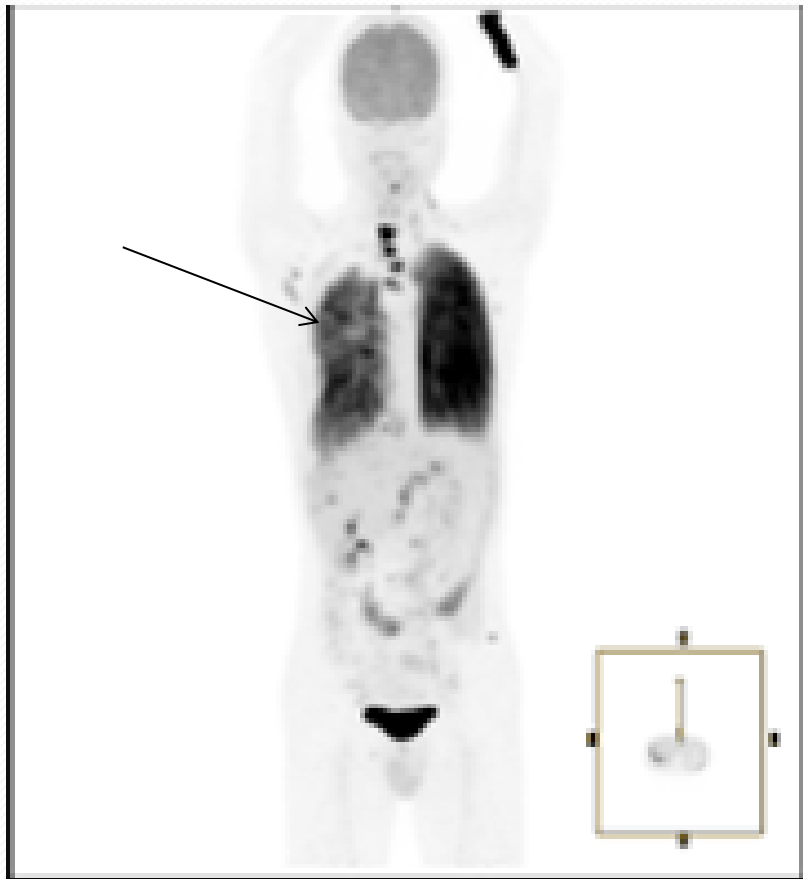


# Imaging Artifacts from physiological function

# Degradation of image quality as function of patient BMI.



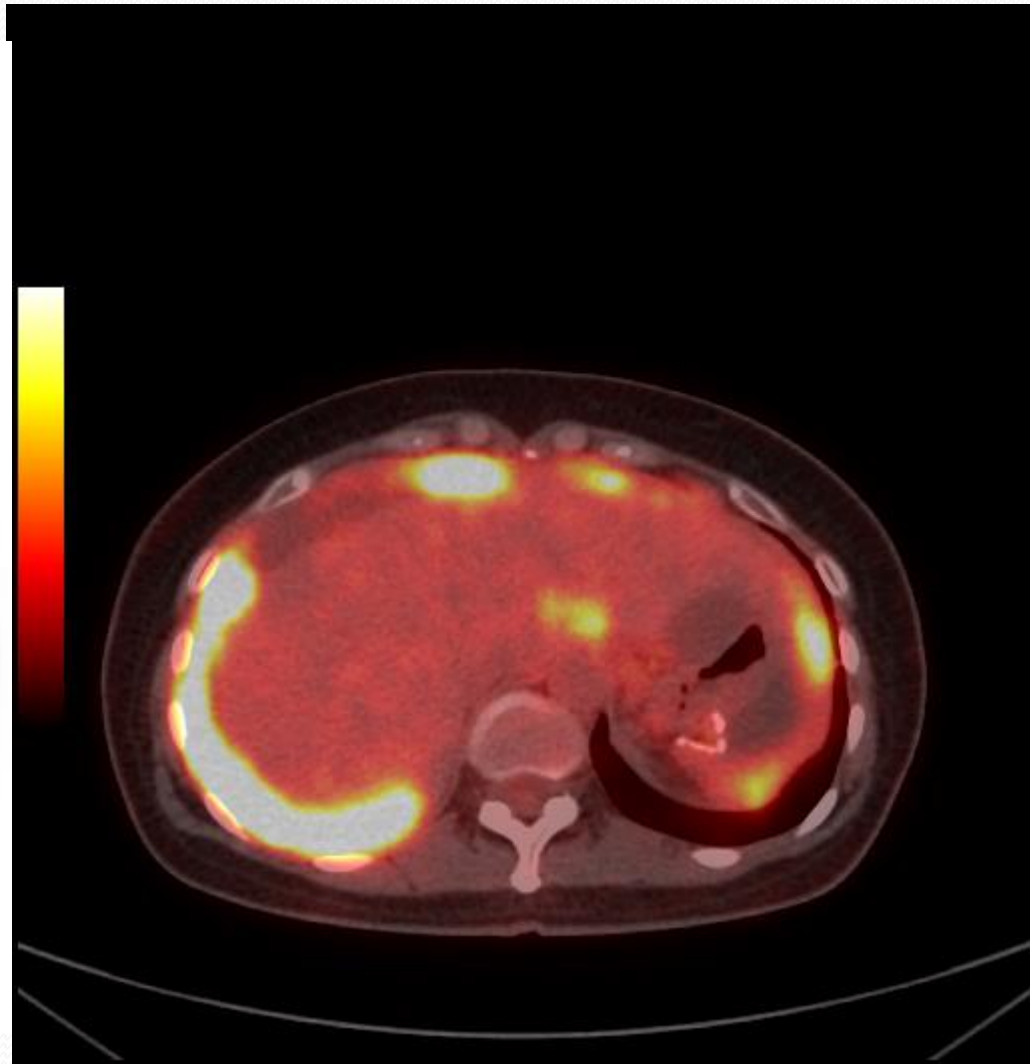
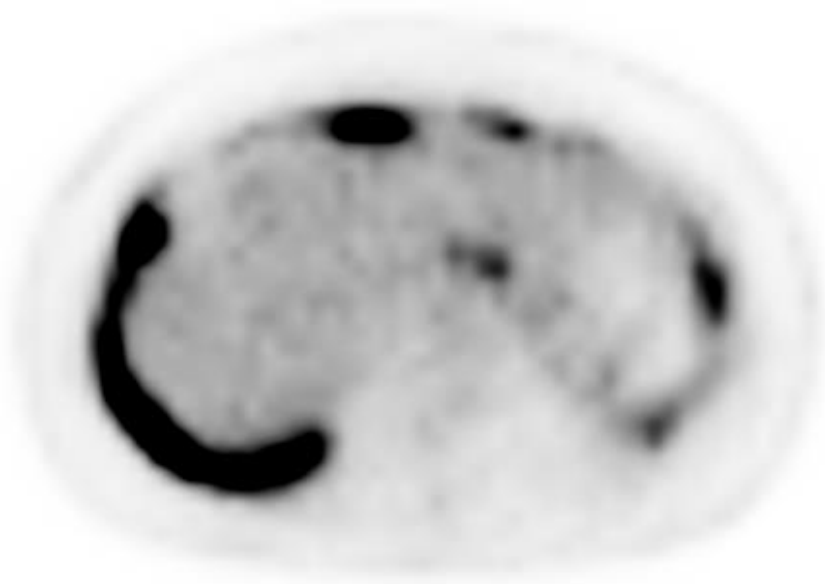




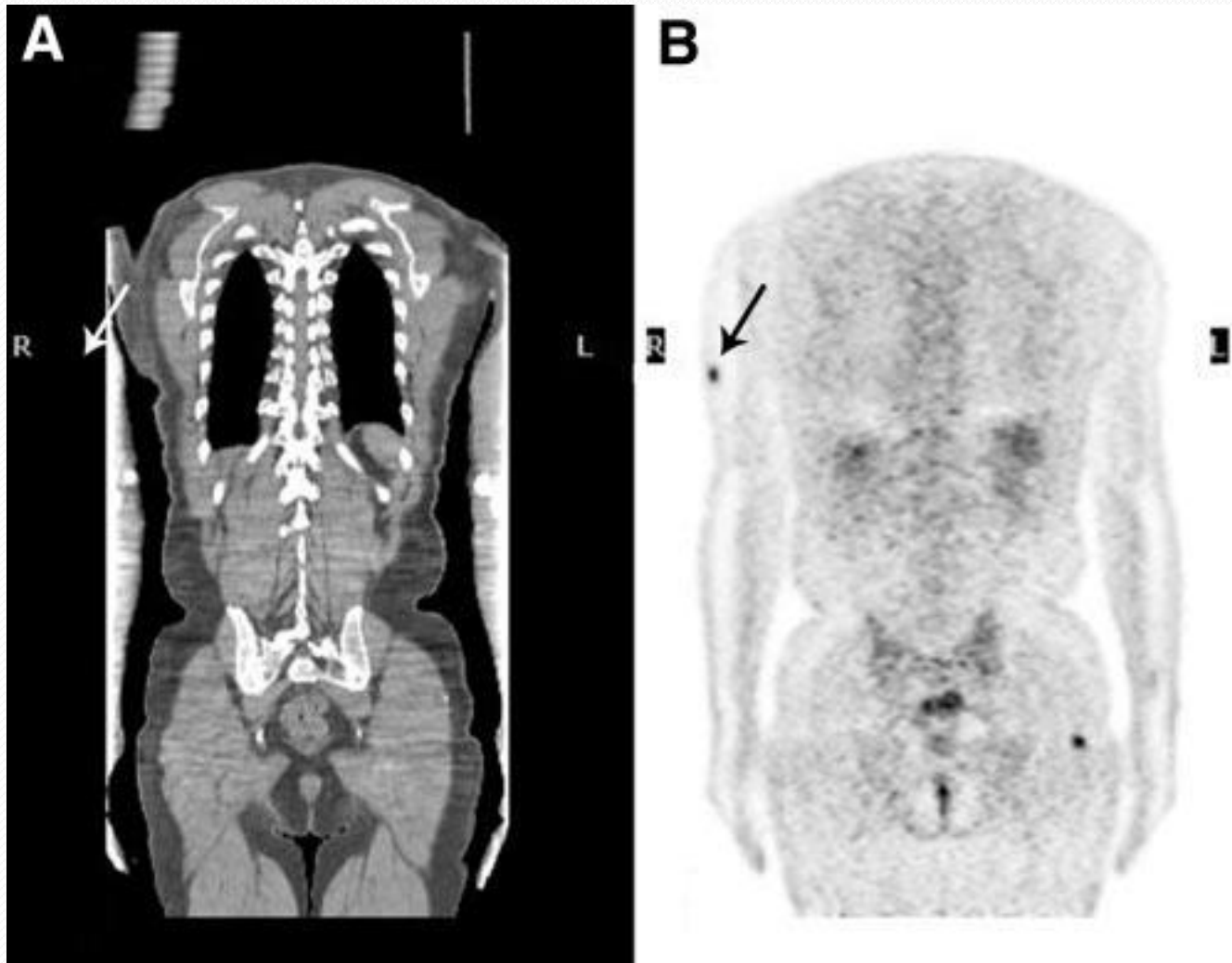
● 化療10天的病人

● 手術3天

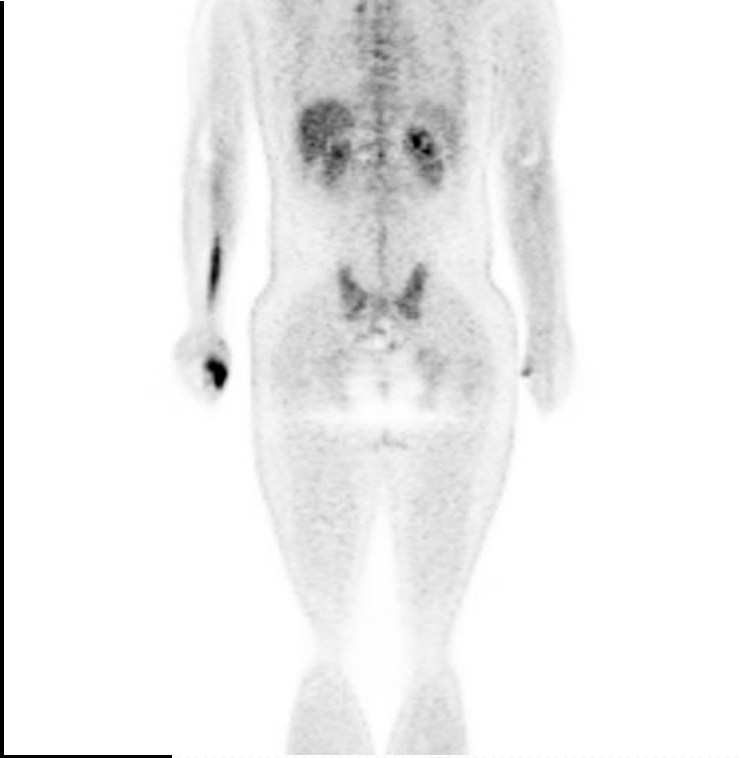
# 腹水



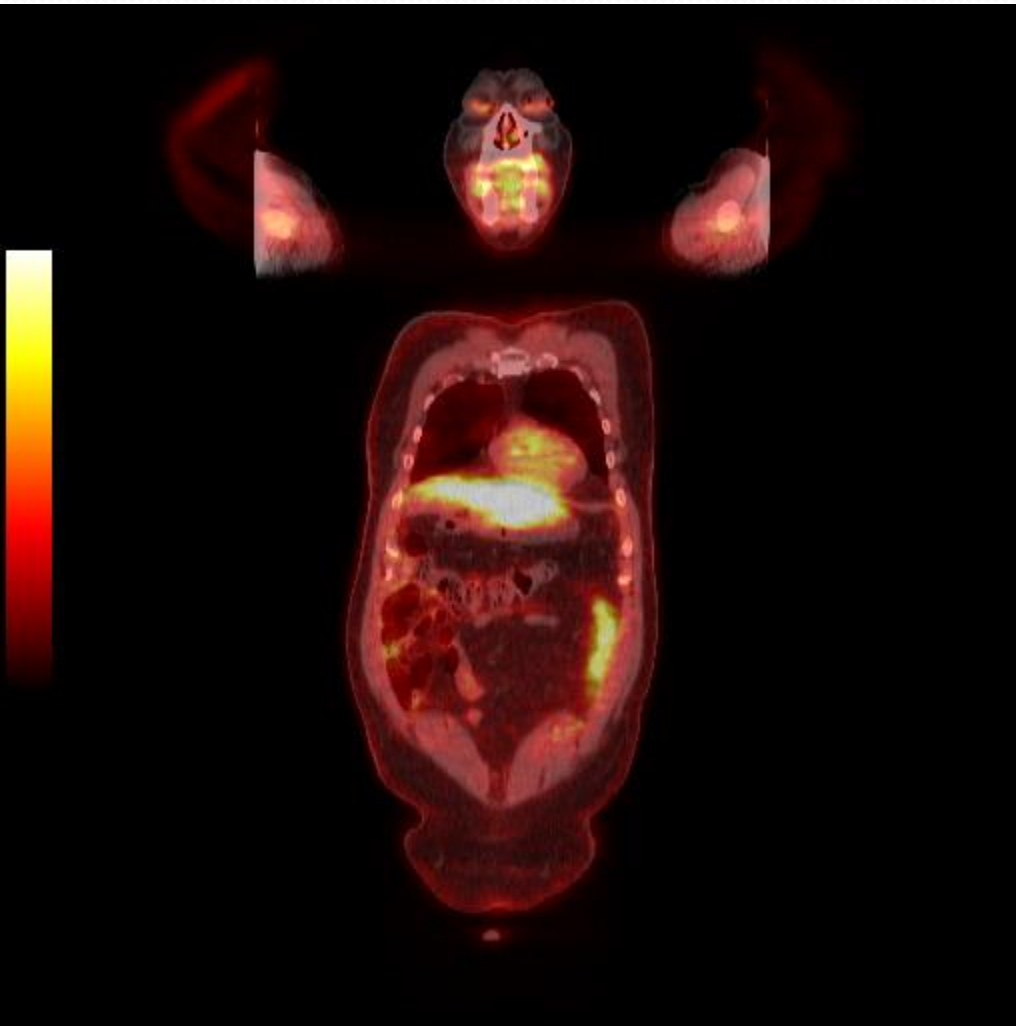
# Truncation



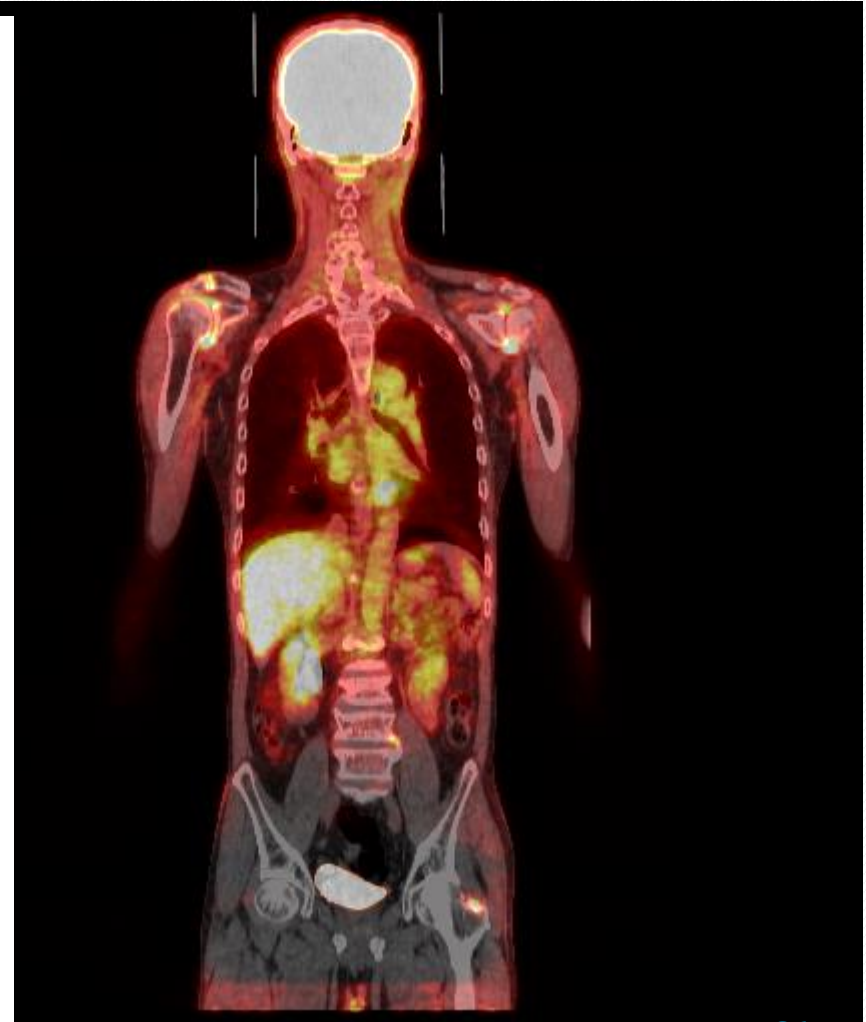
# Truncation



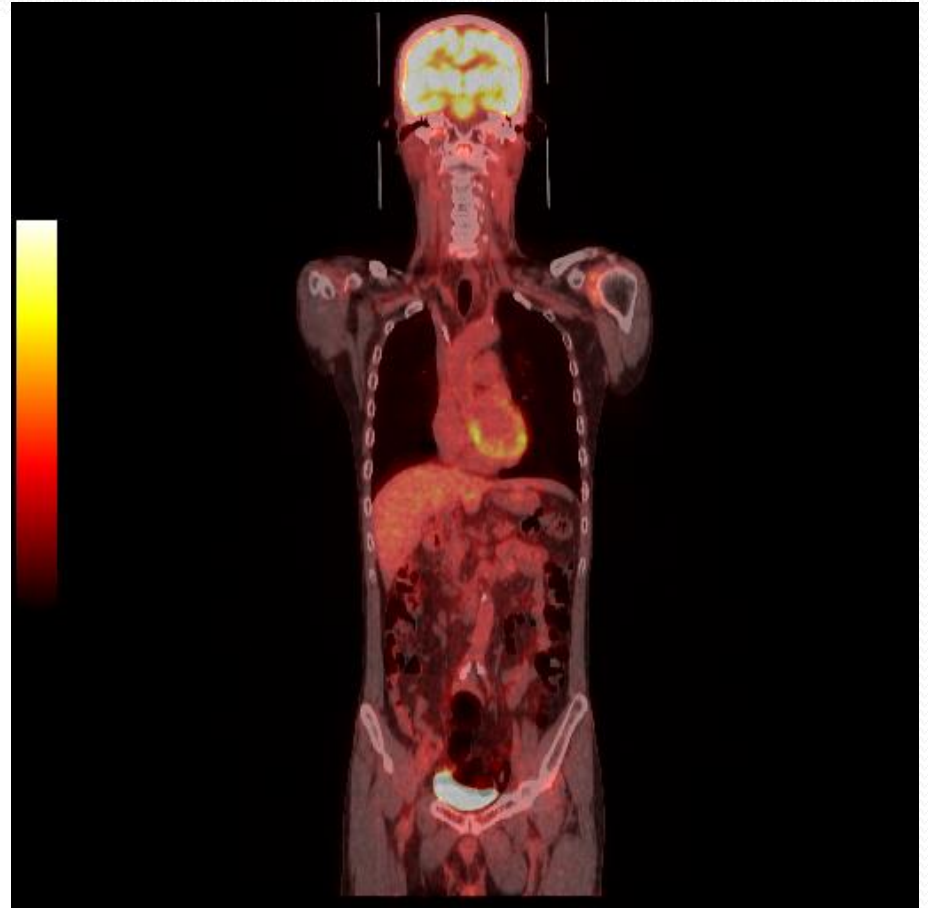
# Truncation



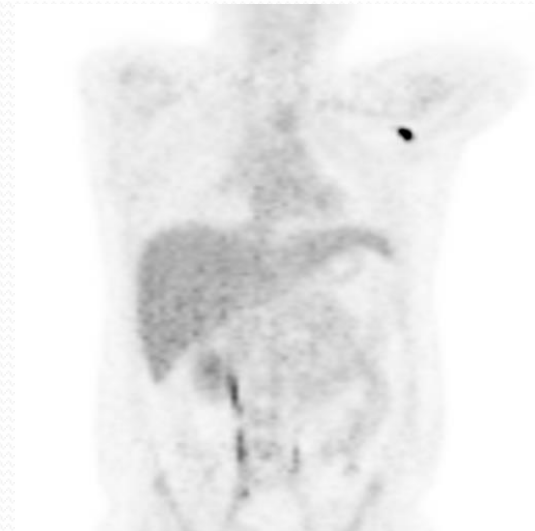
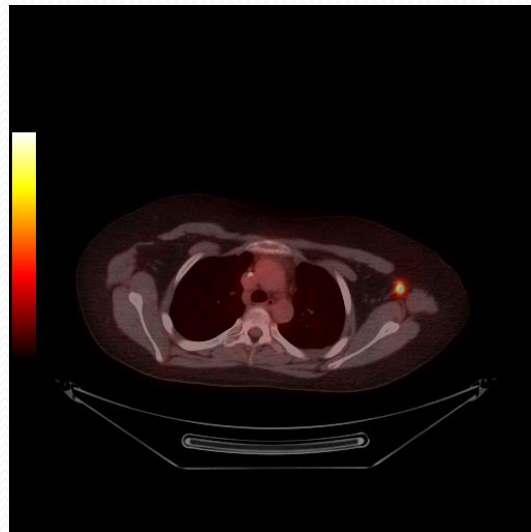
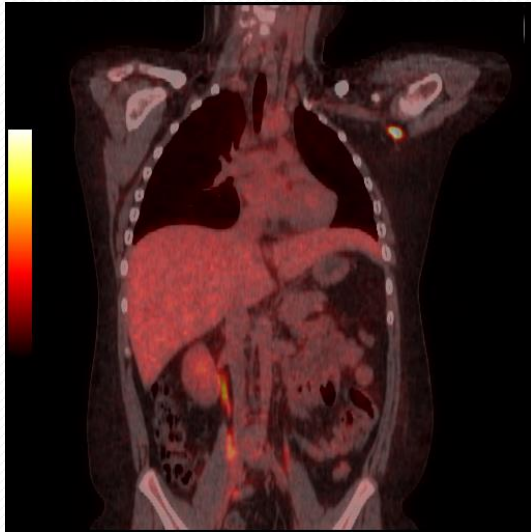
# Overflow



# Overflow Correction



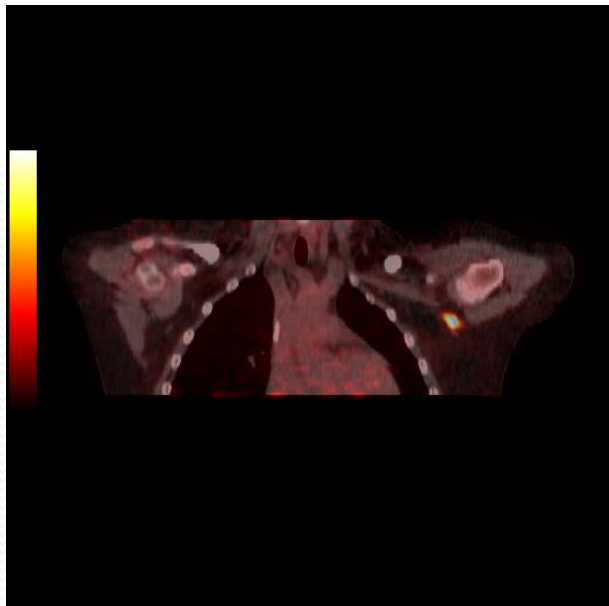
# IV site



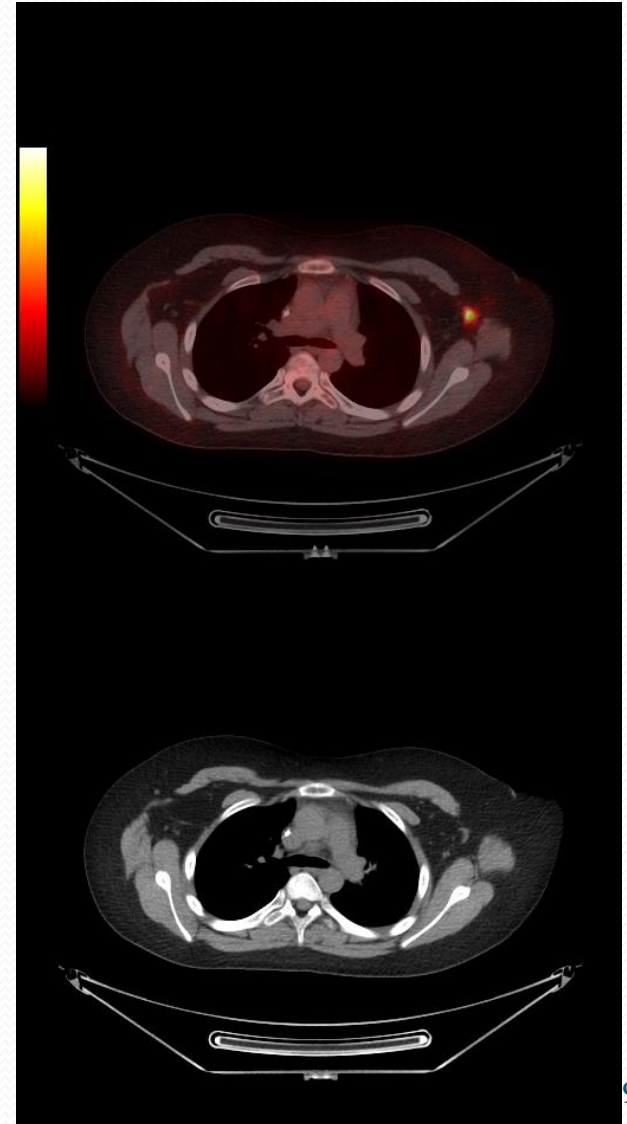
Early phase

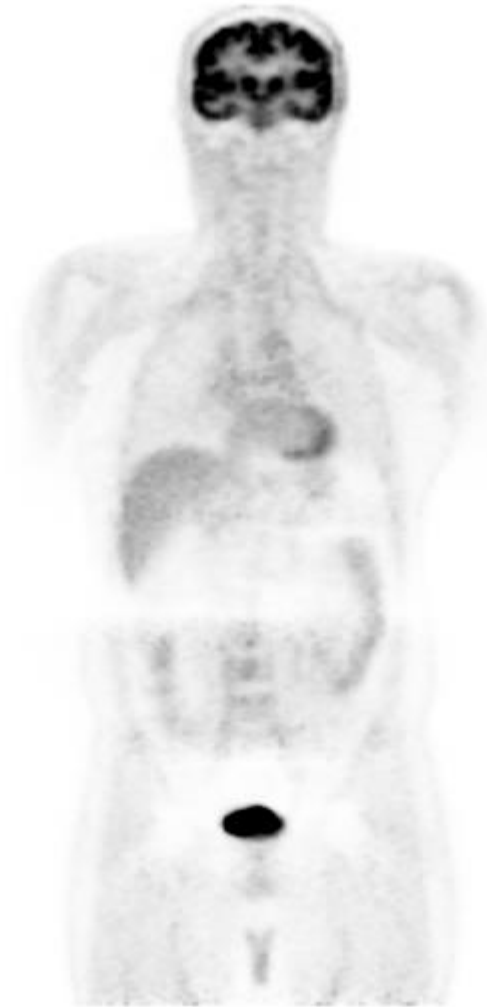
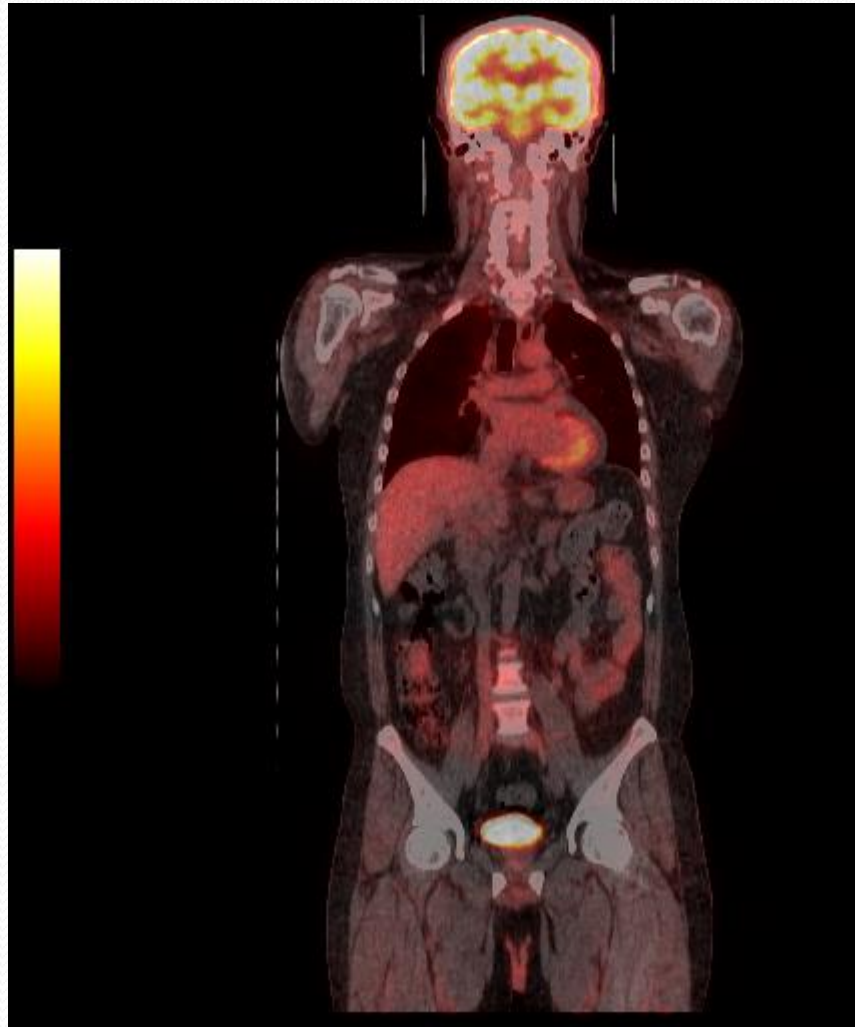


# IV site

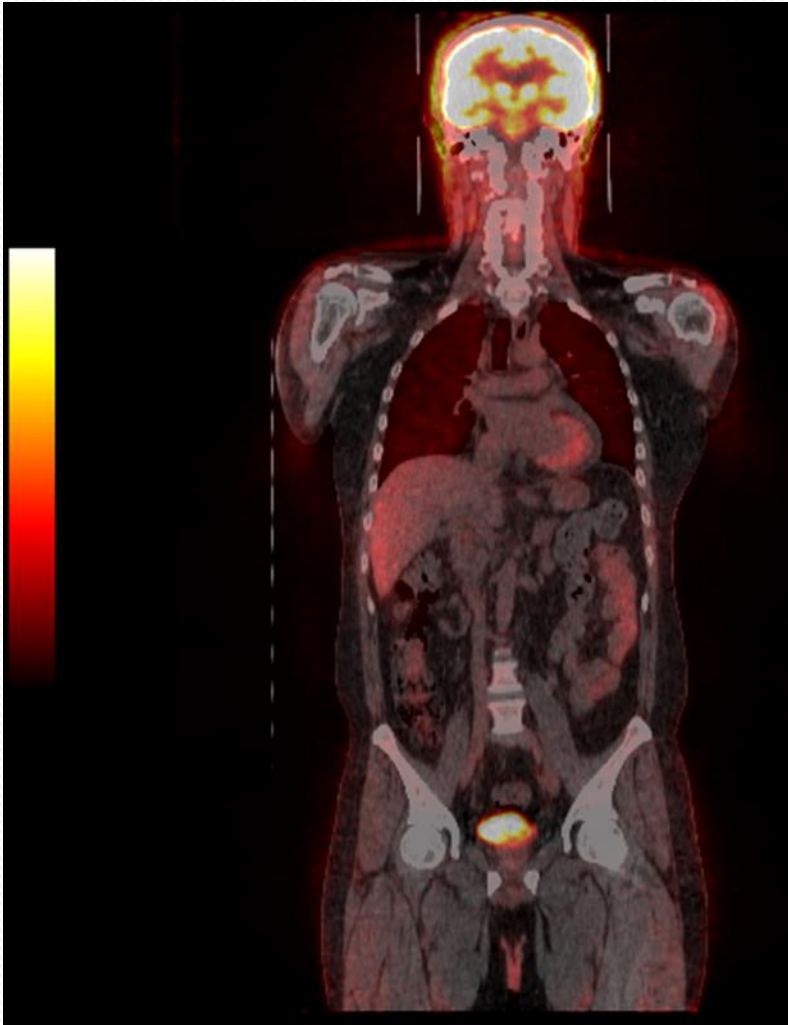


Delay phase

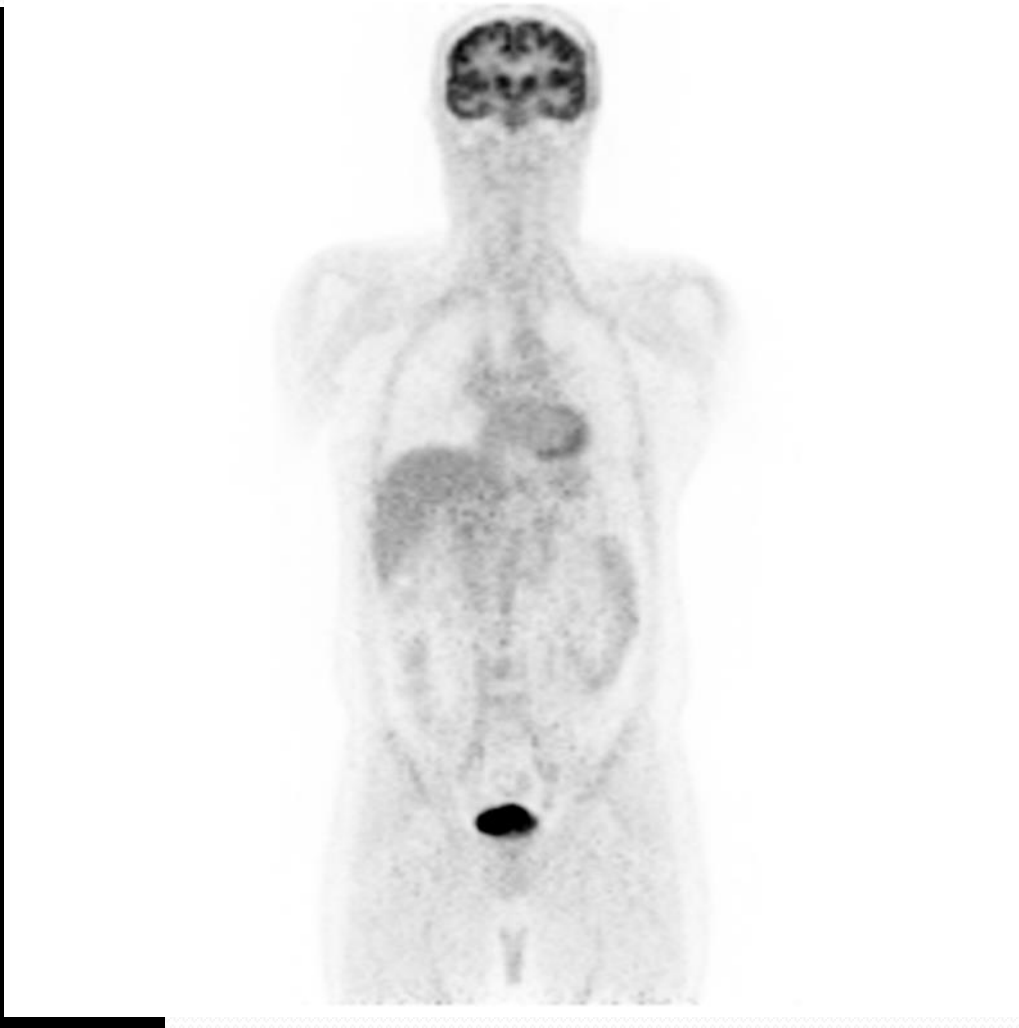
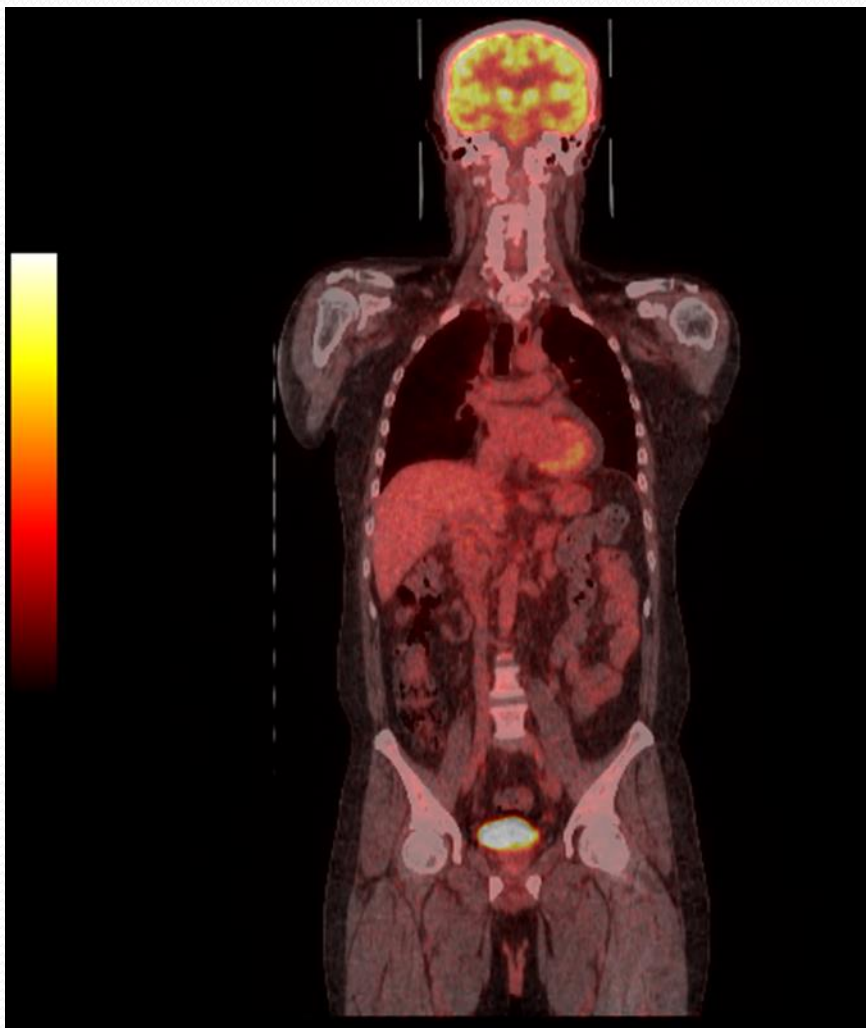




# W/O AC

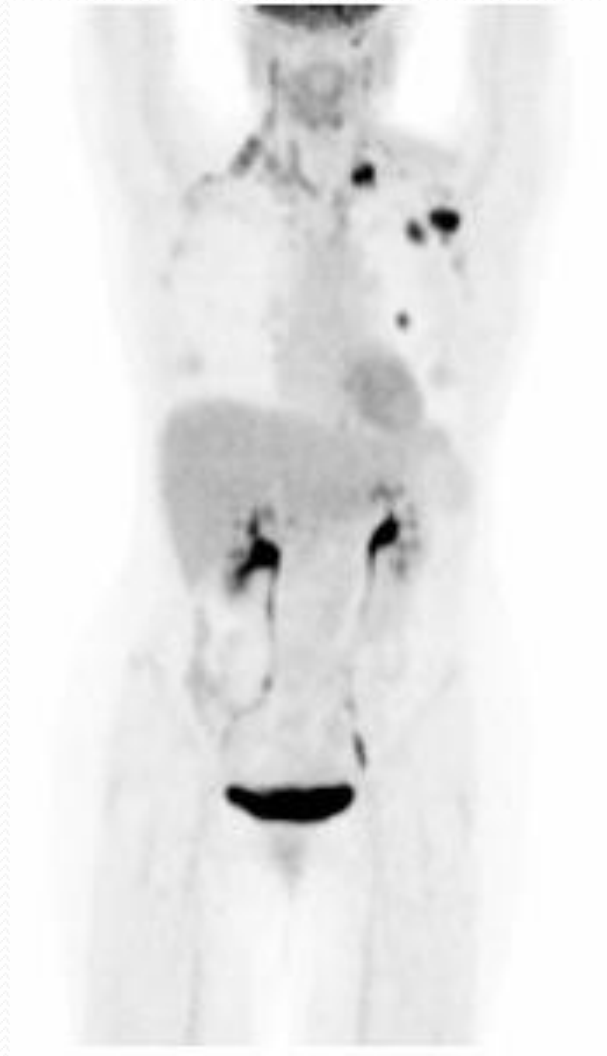


# W/O SC

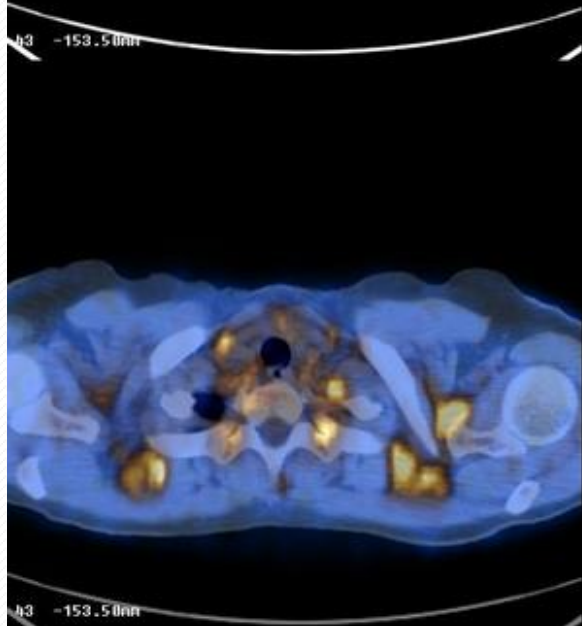




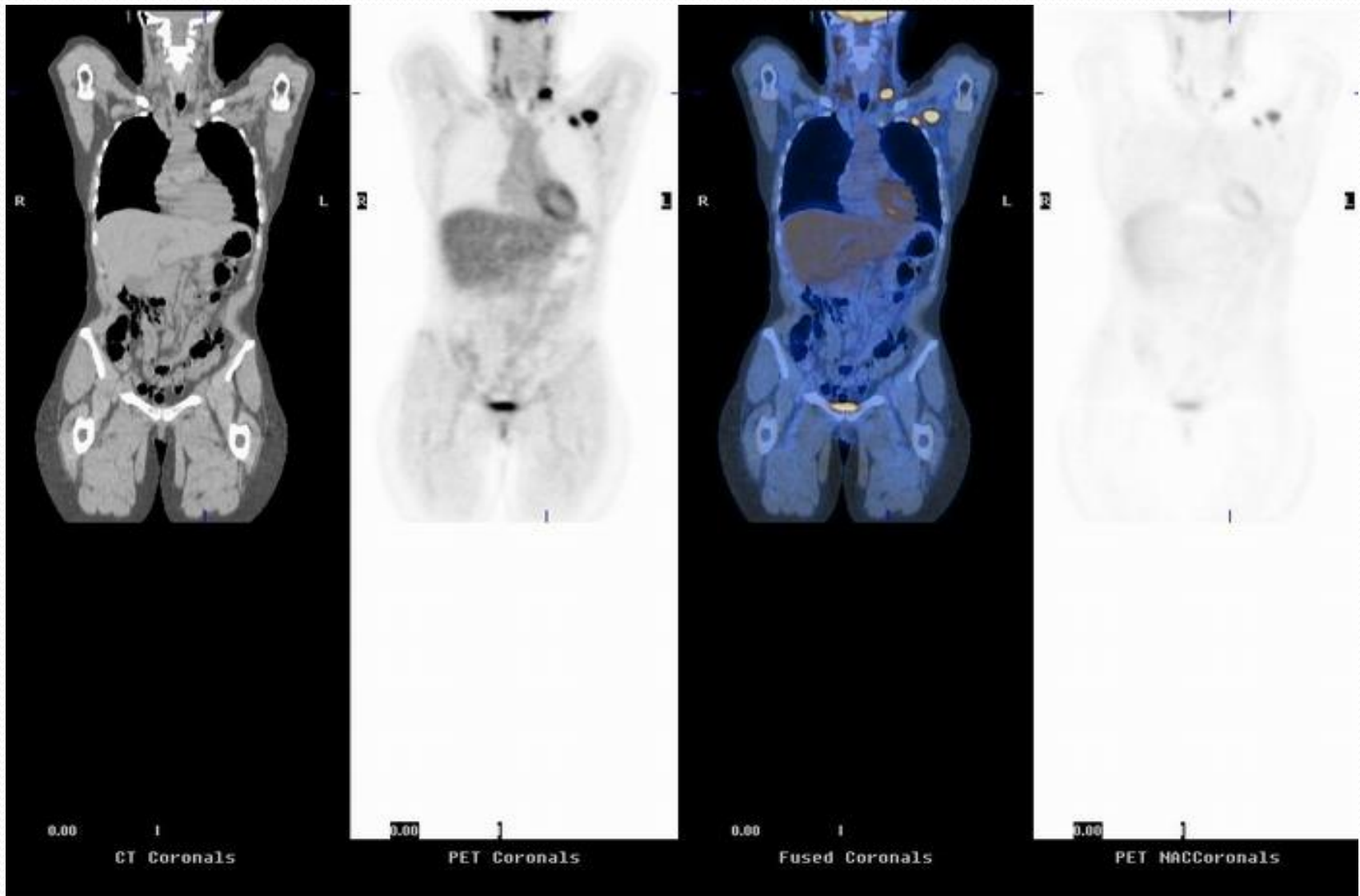
# Brown Fat



# Brown Fat



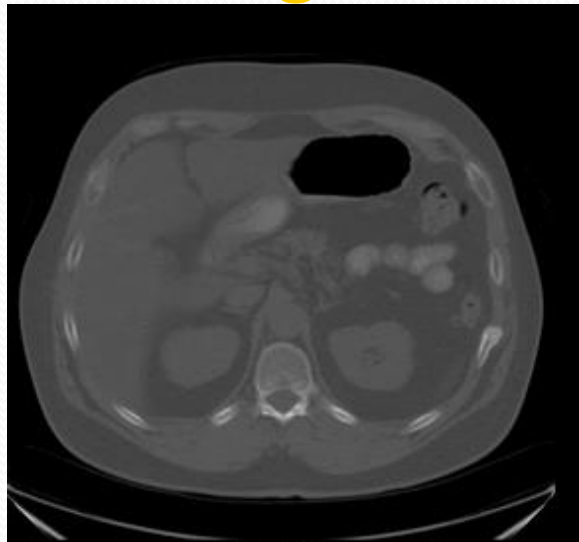
# Brown Fat



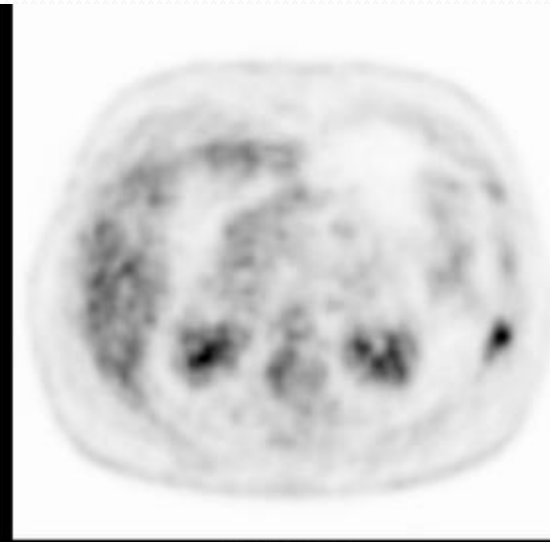


# Fracture

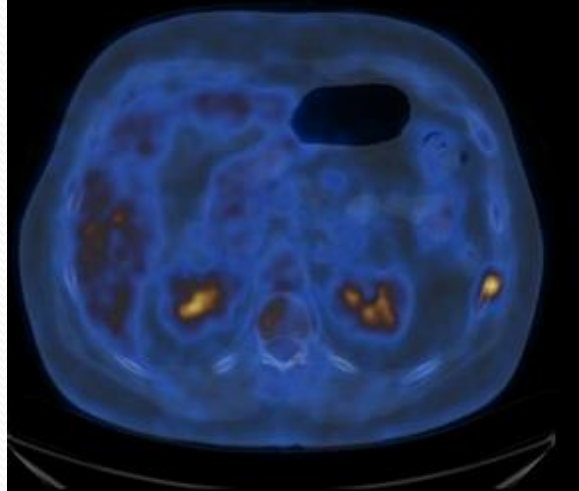
# Benign Pathological Variants: Fractures



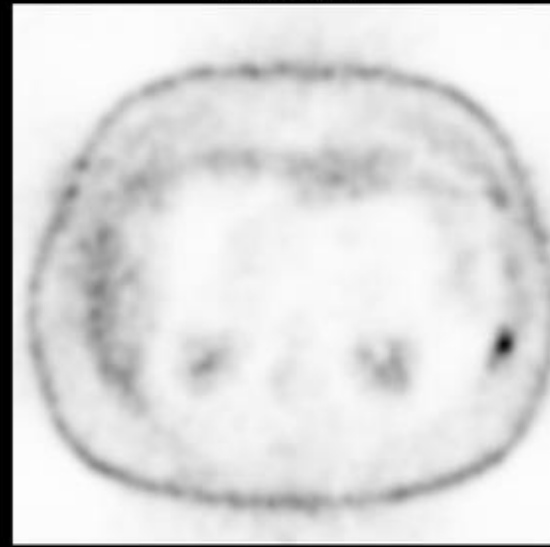
CT Transaxials



PET Transaxials

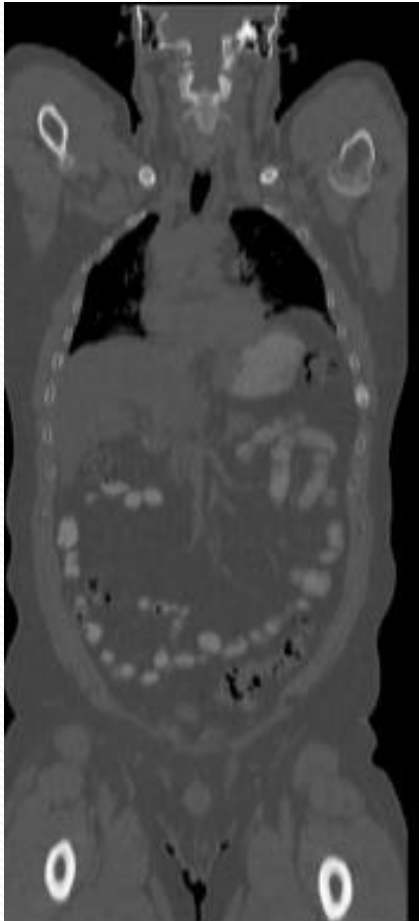


Fused Transaxials

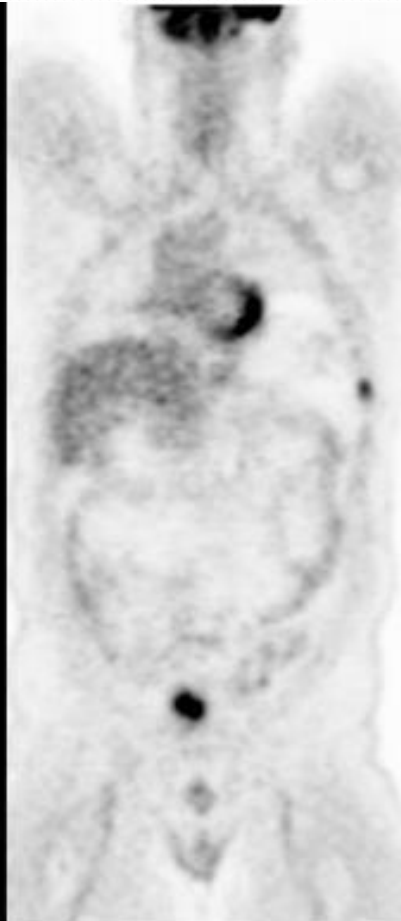


PET MIP Transaxials

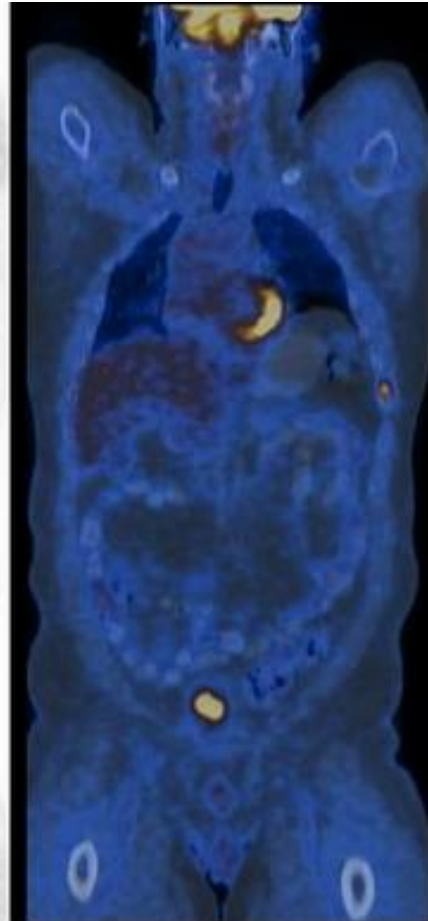
# Benign Pathological Variants: Fractures



CT Coronals



PET Coronals

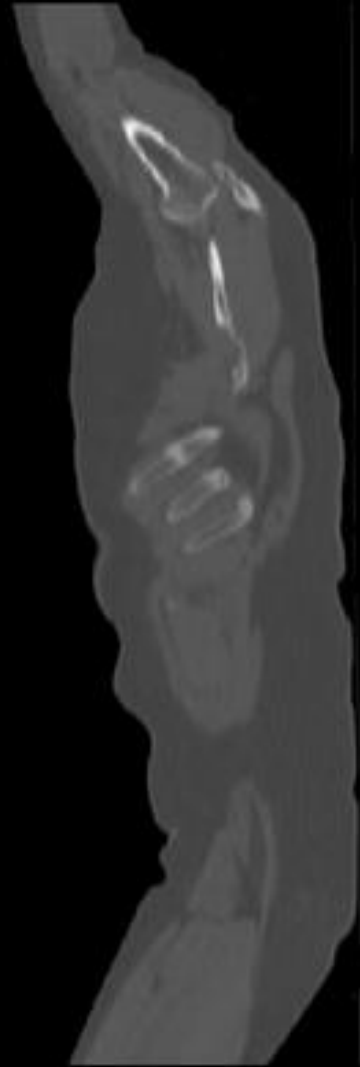


Fused Coronals

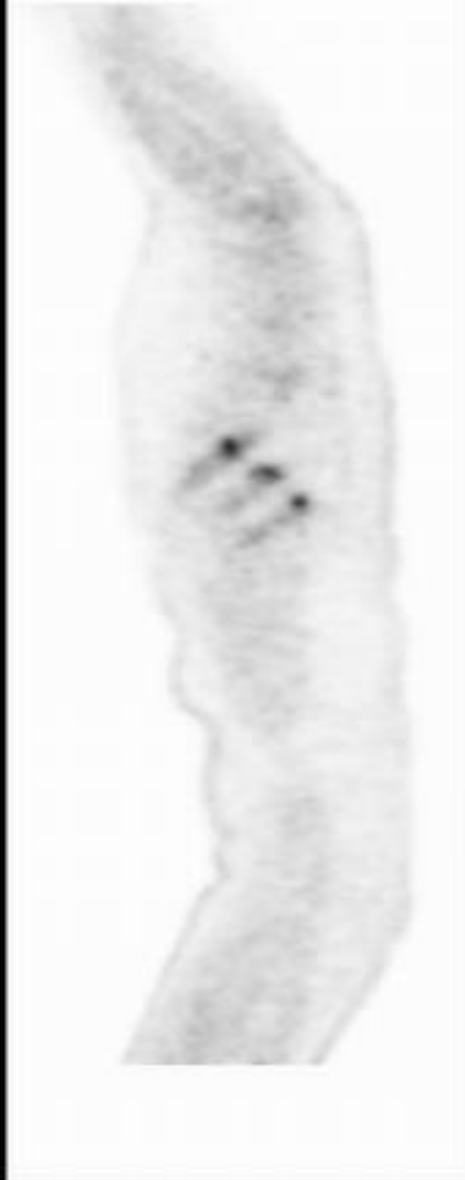


PET NACoronals

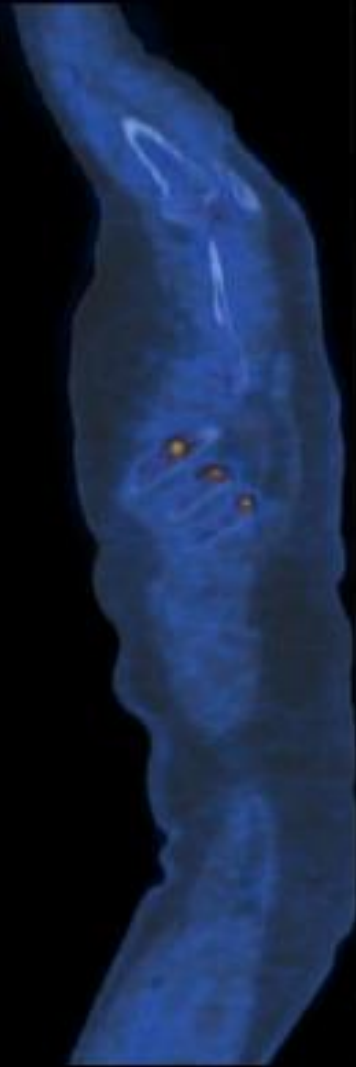
# Benign Pathological Variants: Fractures



CT Sagittals



PET Sagittals



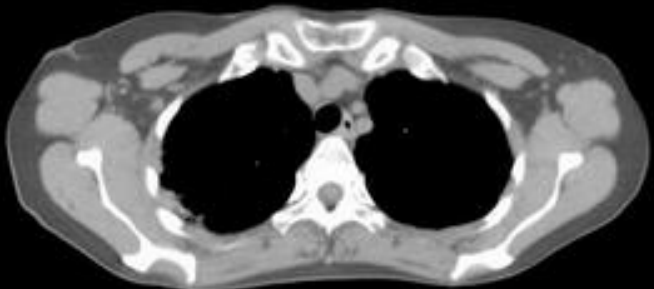
Fused Sagittals



PET NACSagittals

# Common sites of skeletal muscular uptake:

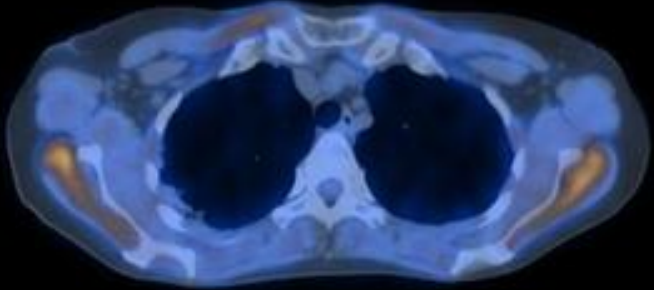
1. Ocular muscles
2. Muscles of mastication
3. Neck strap muscles
4. Tongue - especially the base
5. Larynx
6. Forearms
7. Hands
8. Large muscles of the legs



CT Transaxials



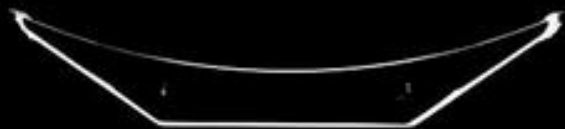
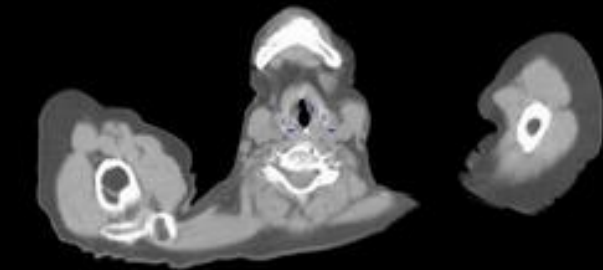
PET Transaxials



Fused Transaxials



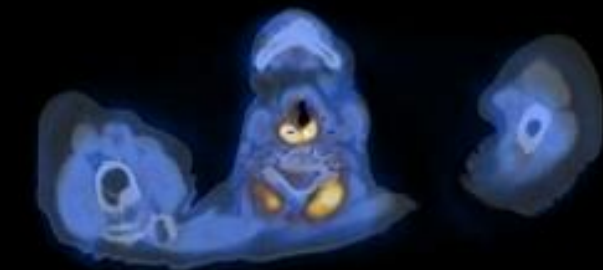
PET NACTransaxials



CT Transaxials



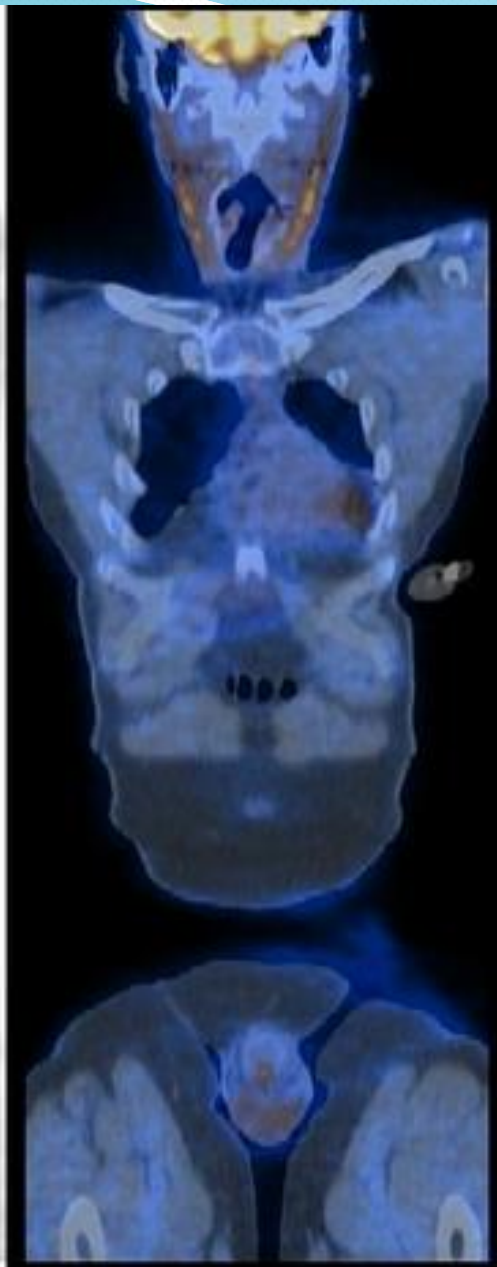
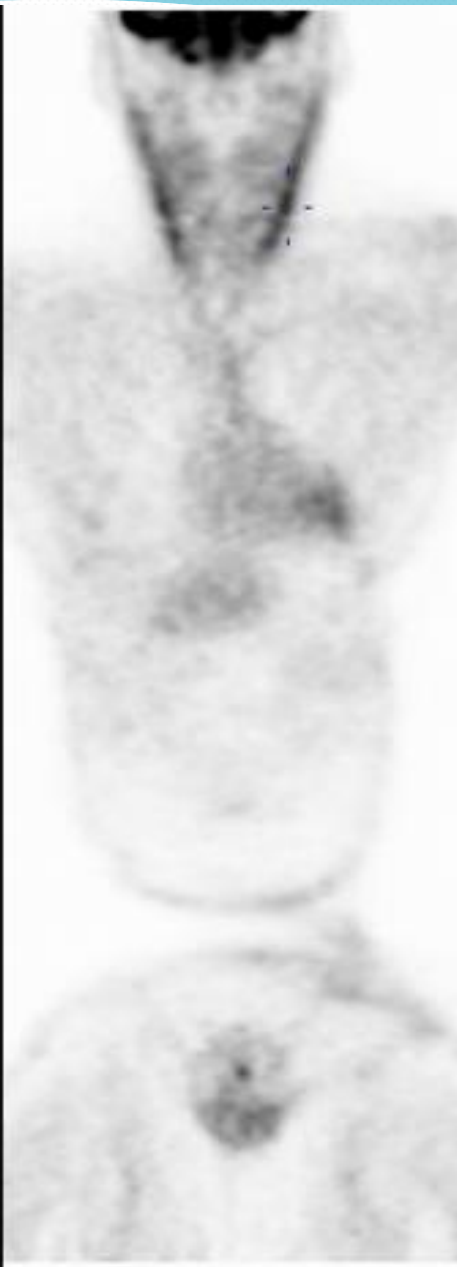
PET Transaxials



Fused Transaxials



PET MACTransaxials





Q&A

感謝凝聽